Neuronal Input Strategies for Functional MRI

Peter A. Bandettini, Ph.D

Unit on Functional Imaging Methods
&
3T Neuroimaging Core Facility

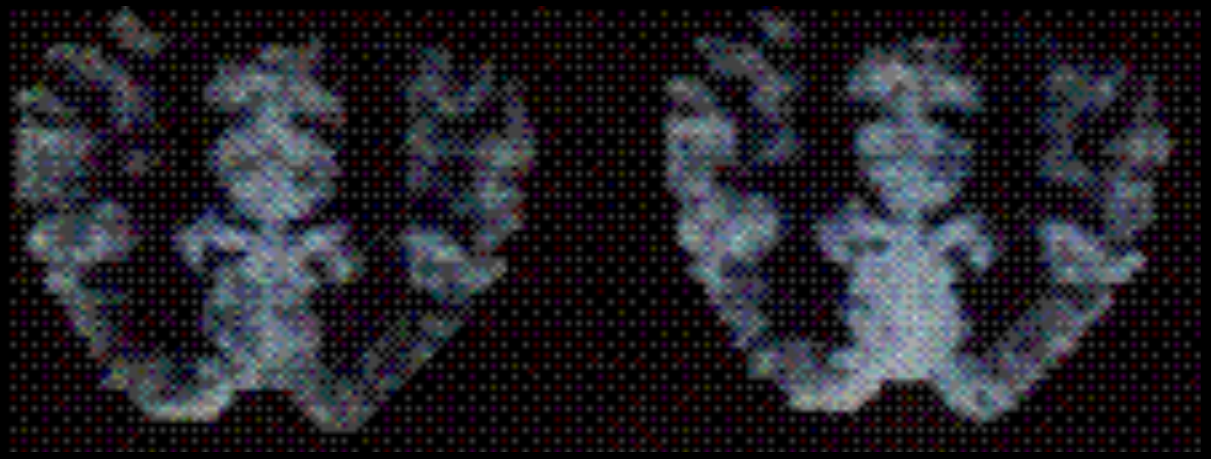
Laboratory of Brain and Cognition
National Institute of Mental Health

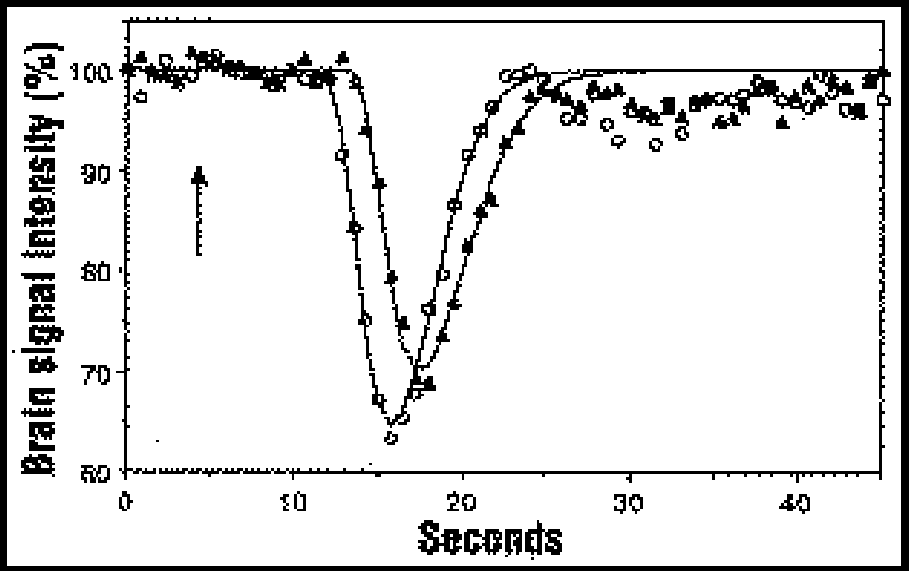
Contrast in Functional MRI

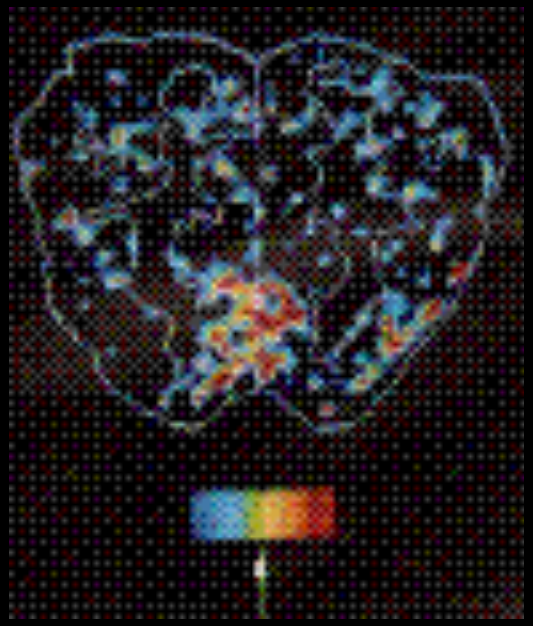
- **Blood Volume**
  - Contrast agent injection and time series collection of T2* or T2 - weighted images
- **BOLD**
  - Time series collection of T2* or T2 - weighted images
- **Perfusion**
  - T1 weighting
  - Arterial spin labeling
- **$CMRO_2$**
  - BOLD and Perfusion w/

  Normalization to Global Perfusion Change

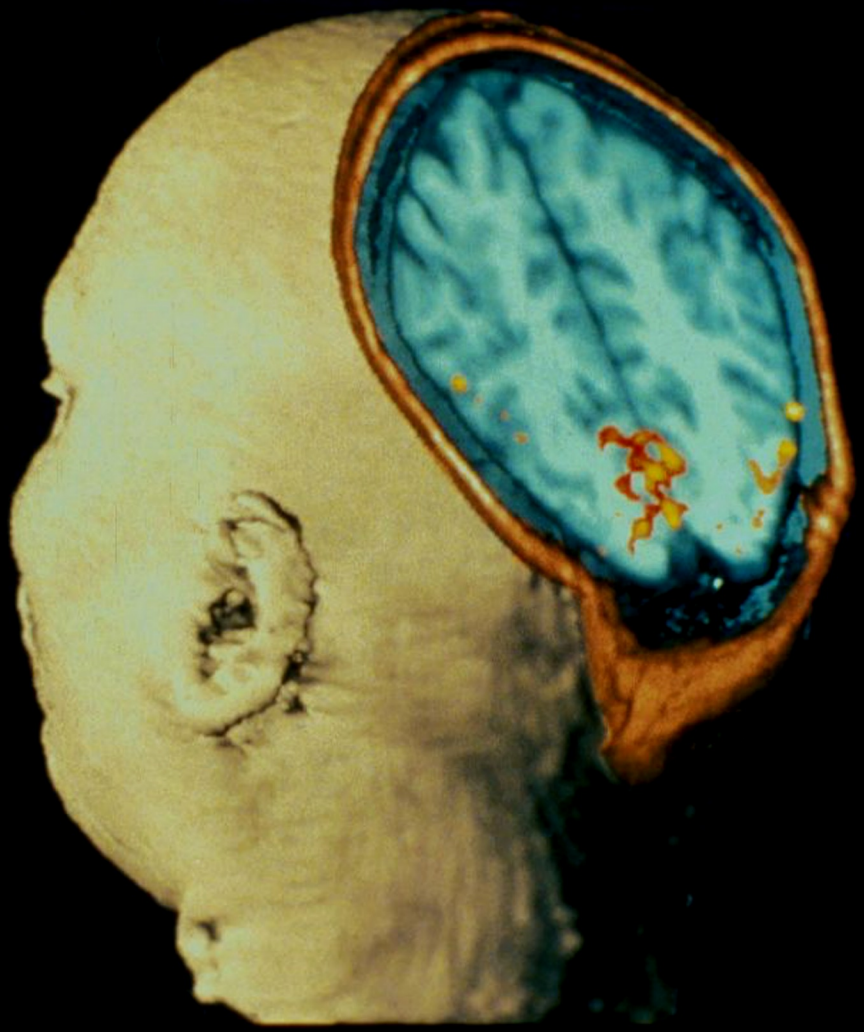
Resting Active







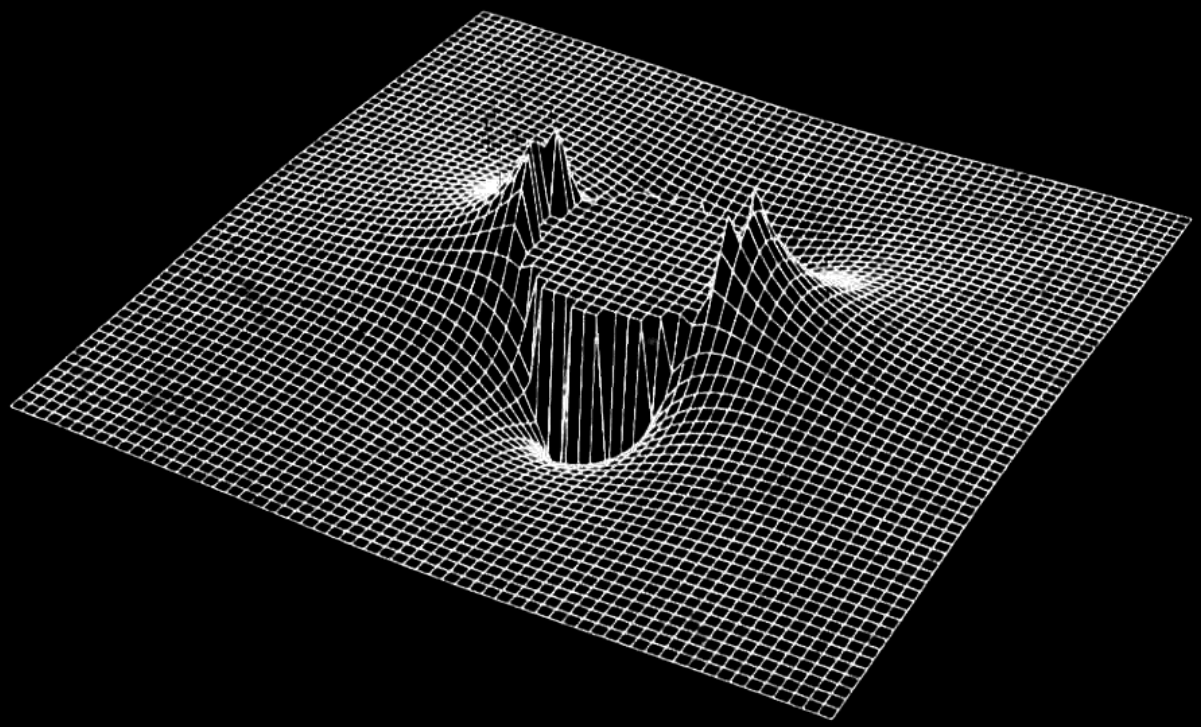
Photic Stimulation



MRI Image showing activation of the Visual Cortex

From Belliveau, et al. Science Nov 1991

Susceptibility-Induced Field Distortion in the Vicinity of a Microvessel $\perp$ to B_o.



BOLD Contrast in the Detection of Neuronal Activity

Cerebral Tissue Activation

↓

Local Vasodilation

↓

Increase in Cerebral Blood Flow and Volume → Oxygen Delivery Exceeds Metabolic Need

↓

Increase in Capillary and Venous Blood Oxygenation

↓

Decrease in Deoxy-hemoglobin

Deoxy-hemoglobin: paramagnetic
Oxy-hemoglobin: diamagnetic

↓

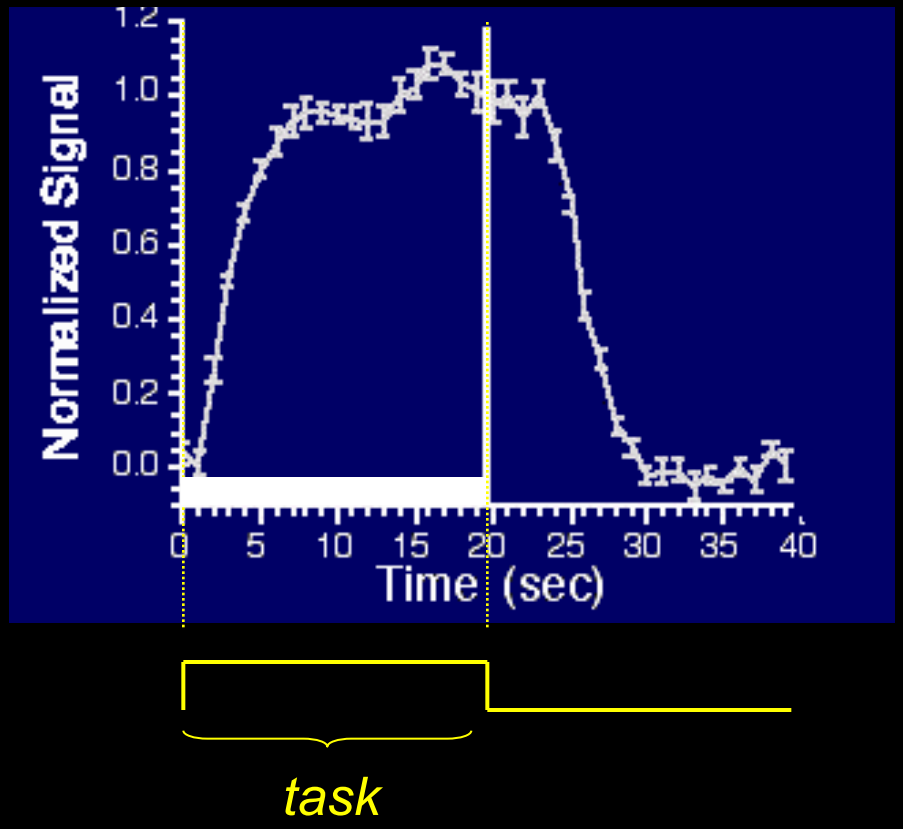
Decrease in susceptibility-related intravoxel dephasing → Increase in T2 and T2*

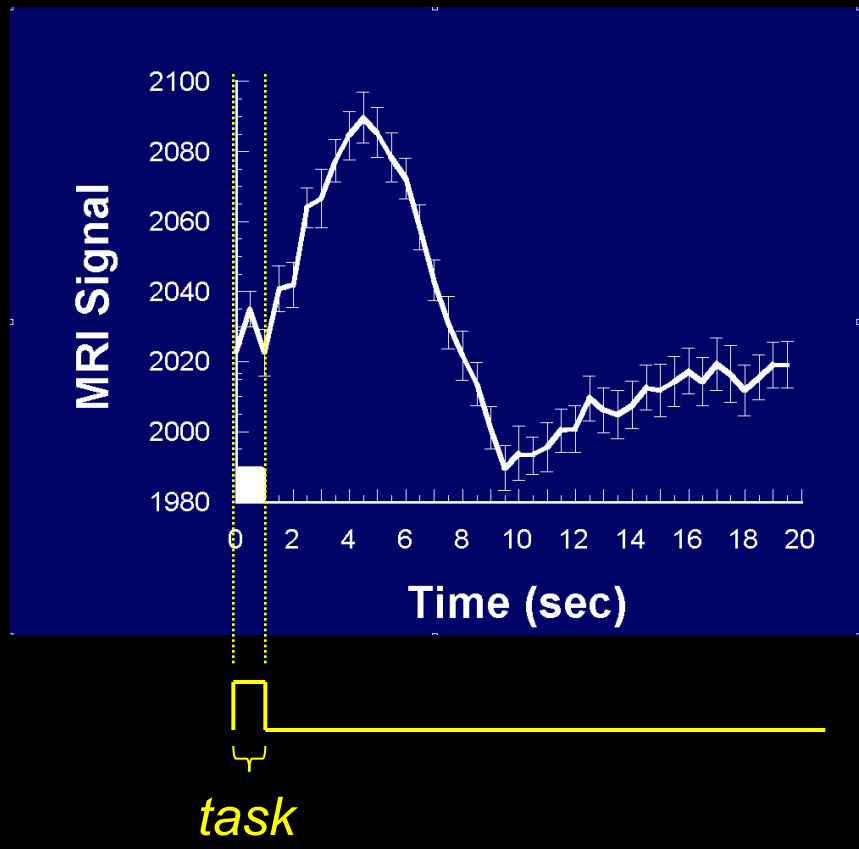
↓

Local Signal Increase in T2 and T2* - weighted sequences

The BOLD Signal

Blood Oxygenation Level Dependent (BOLD) signal changes

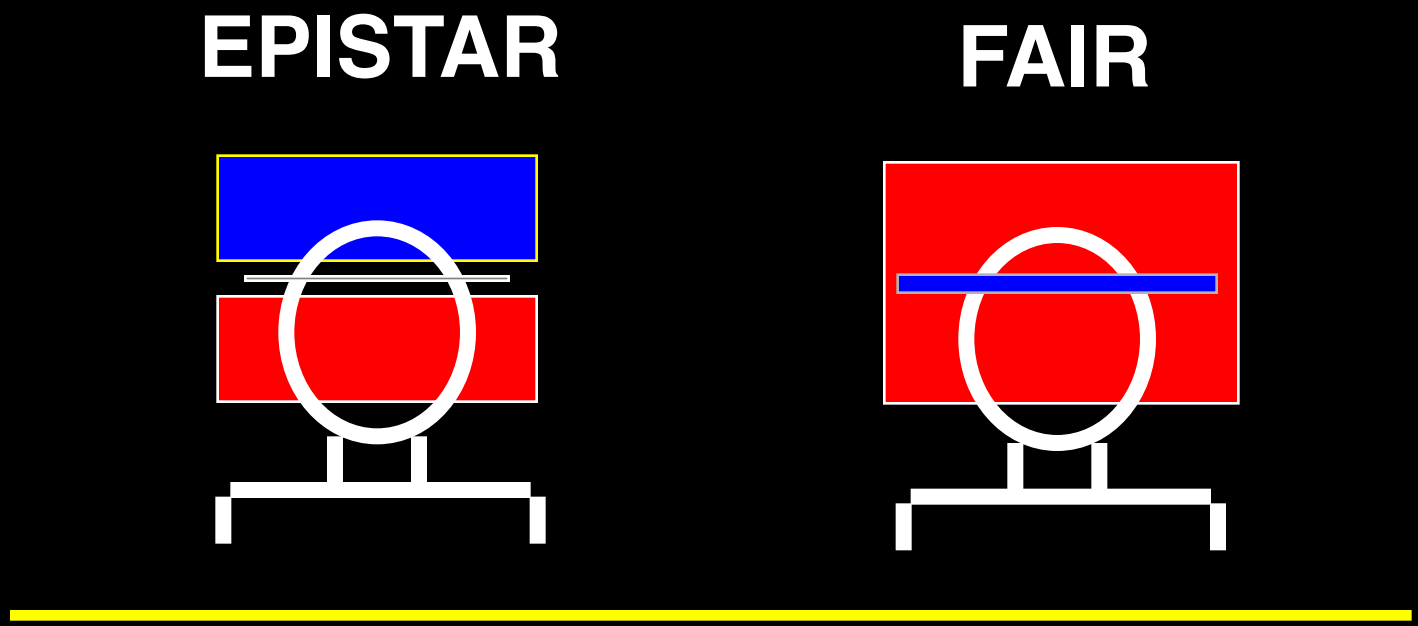


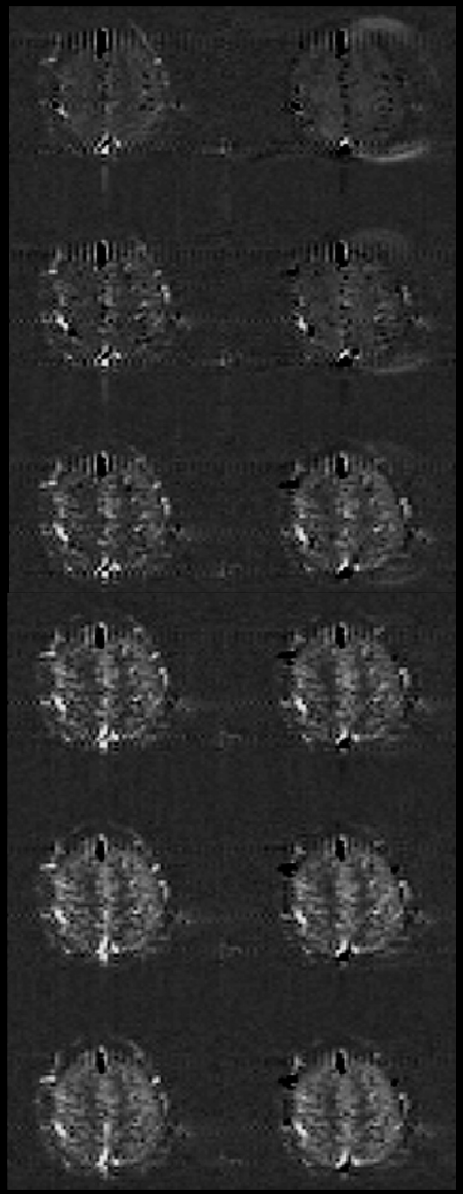


Alternating Left and Right Finger Tapping

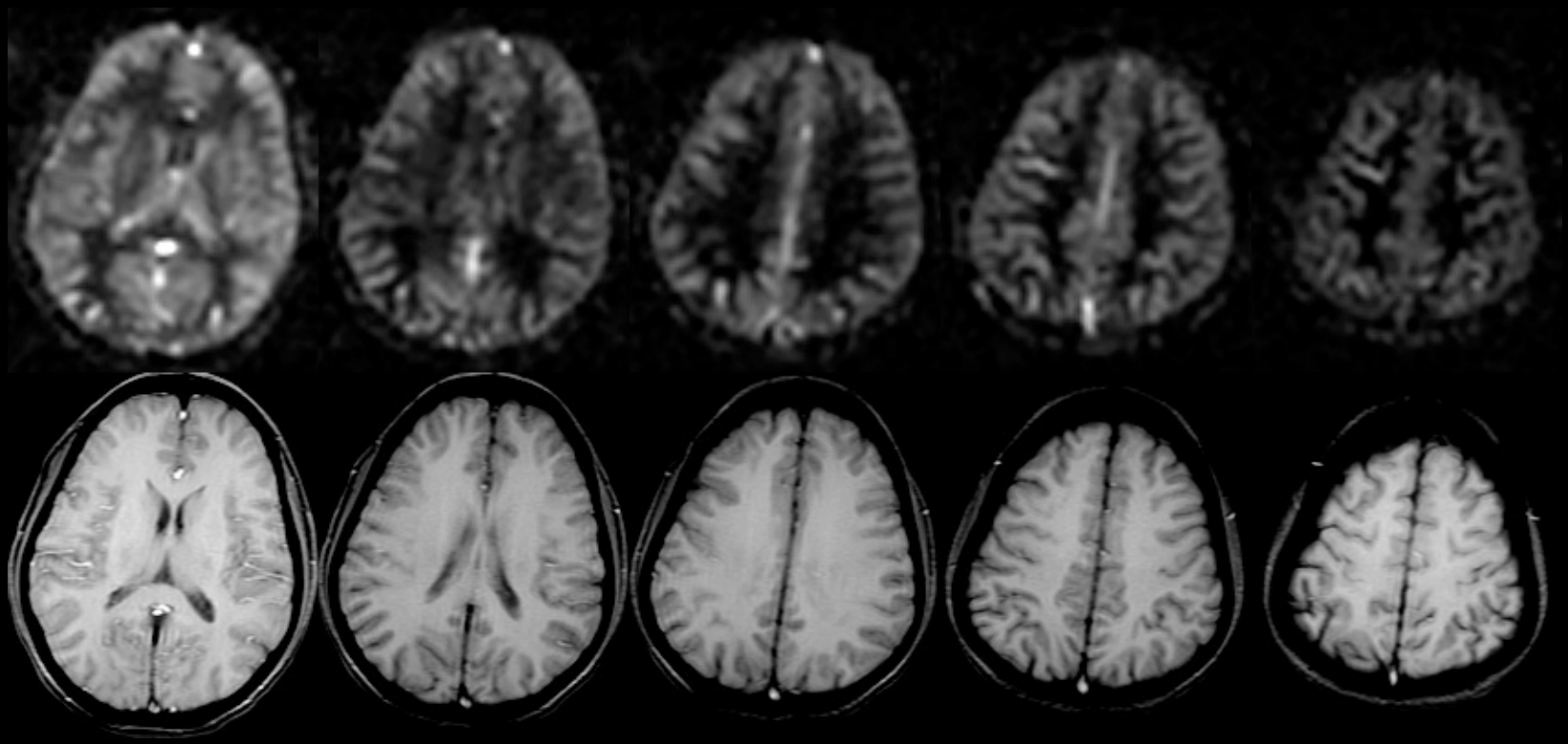
~ 1992

Perfusion / Flow Imaging

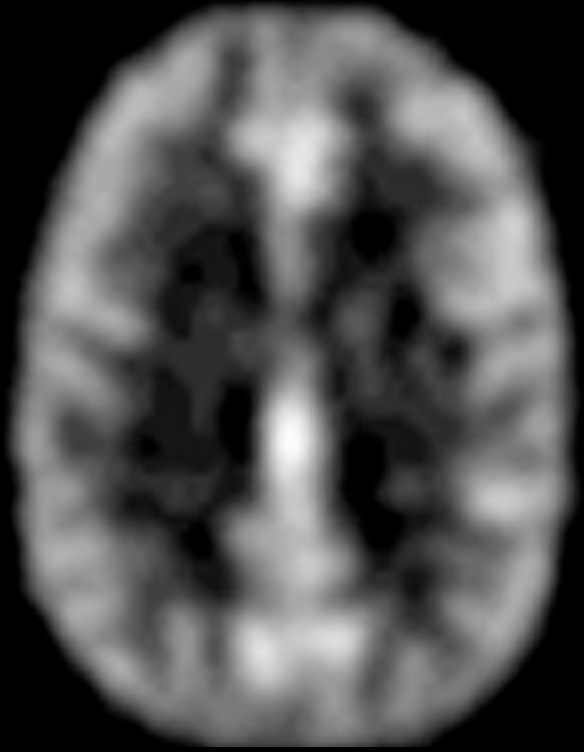


TI (ms)	FAIR	EPISTAR
200		
400		
600		
800		
1000		
1200		

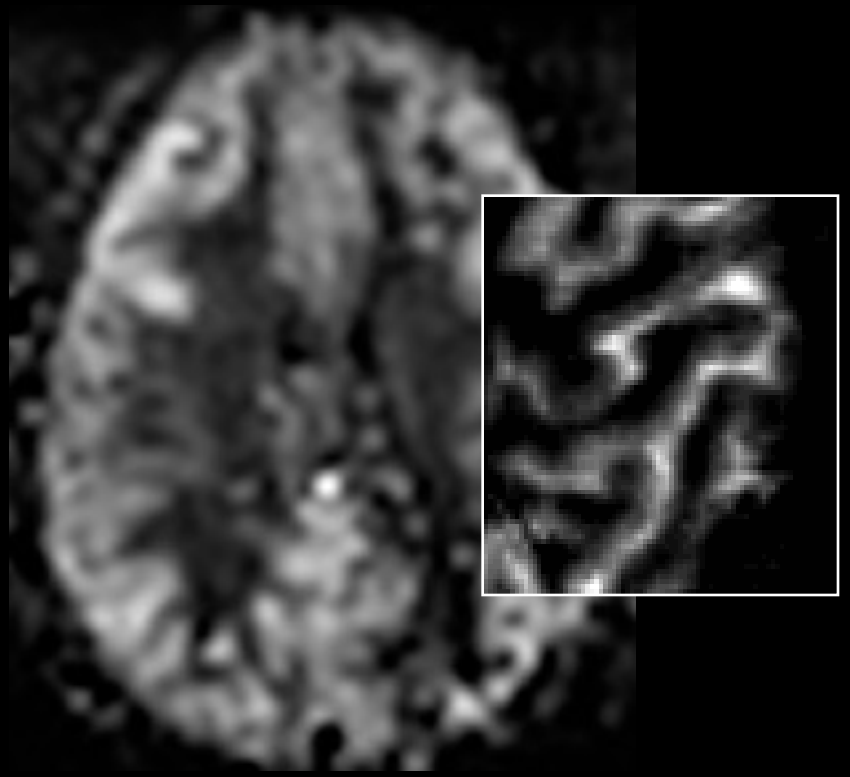
Resting ASL Signal



Comparison with Positron Emission Tomography



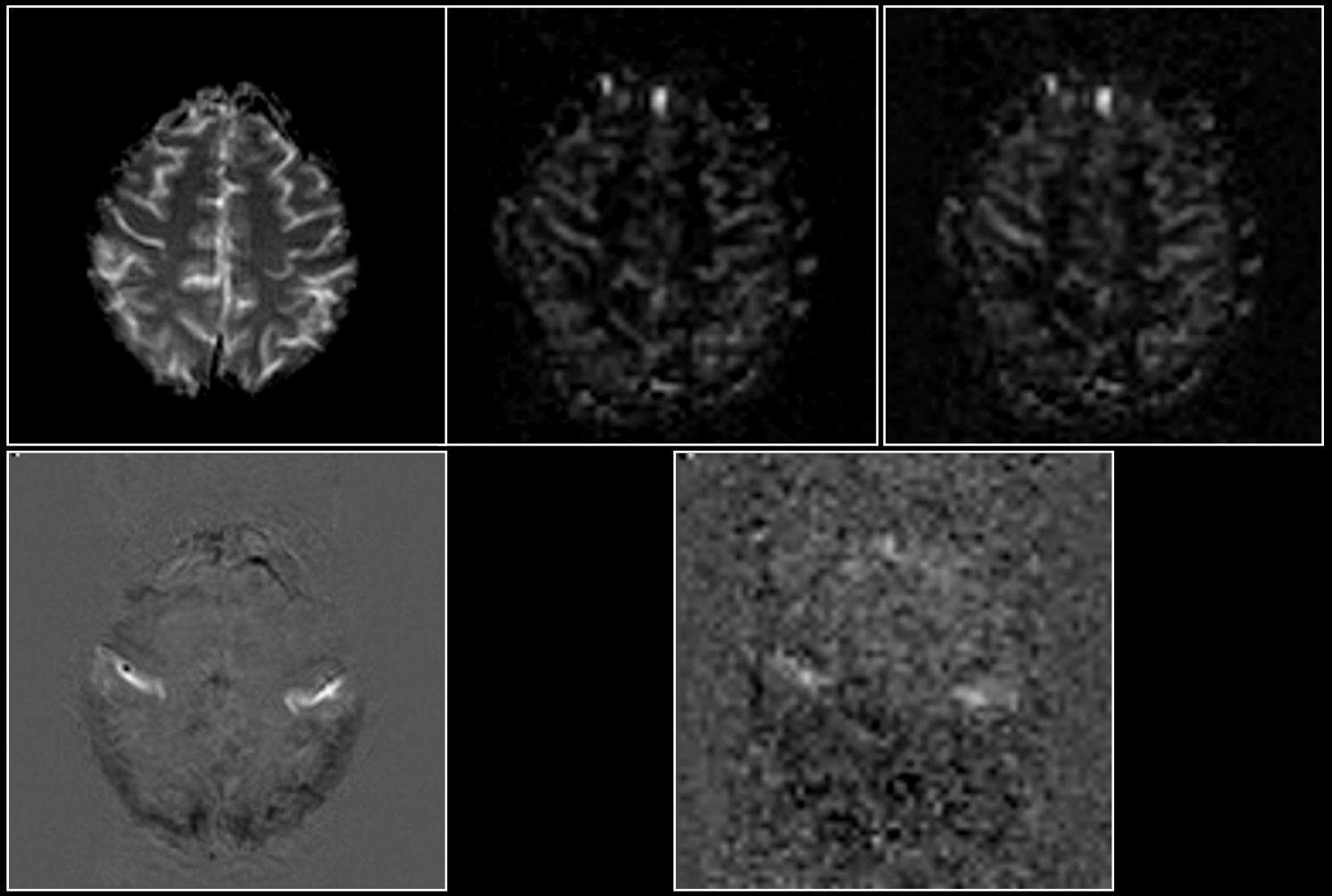
PET: $H_2{}^{15}O$



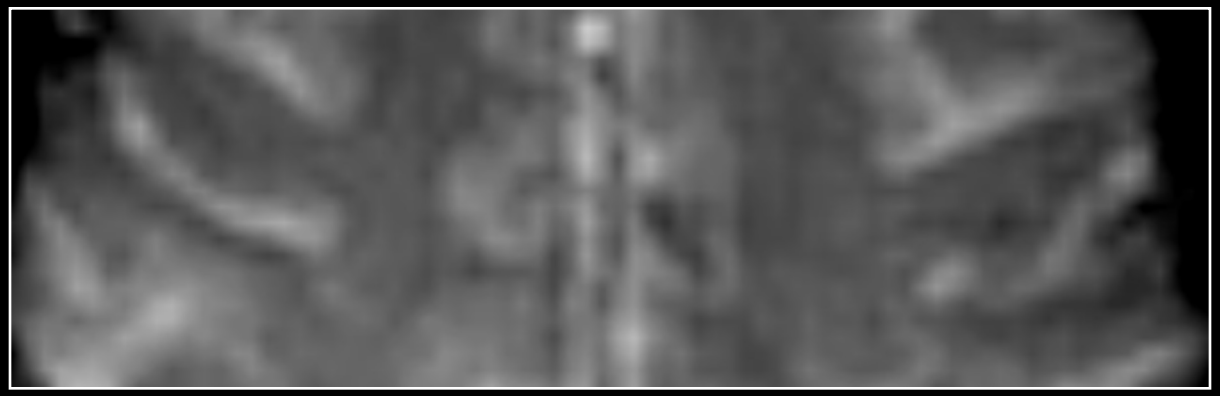
MRI: ASL

Perfusion

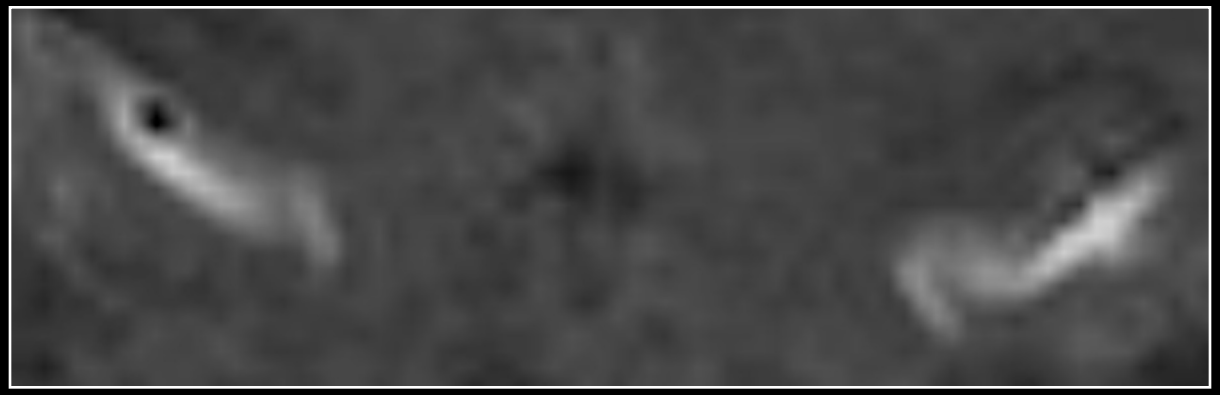
BOLD *Rest* *Activation*



Anatomy



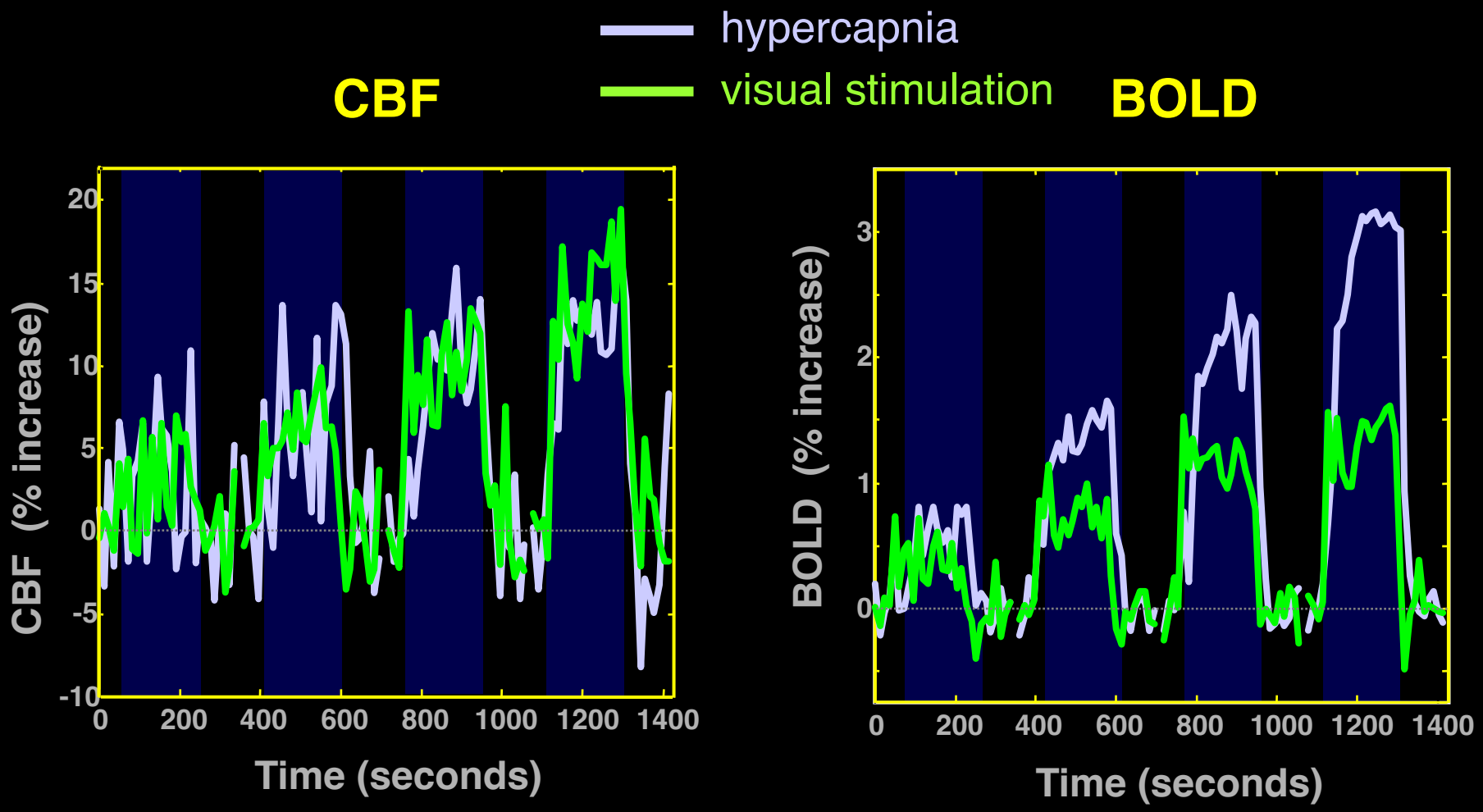
BOLD



Perfusion

$CMRO_2$-related BOLD signal deficit:

Hoge, et al.

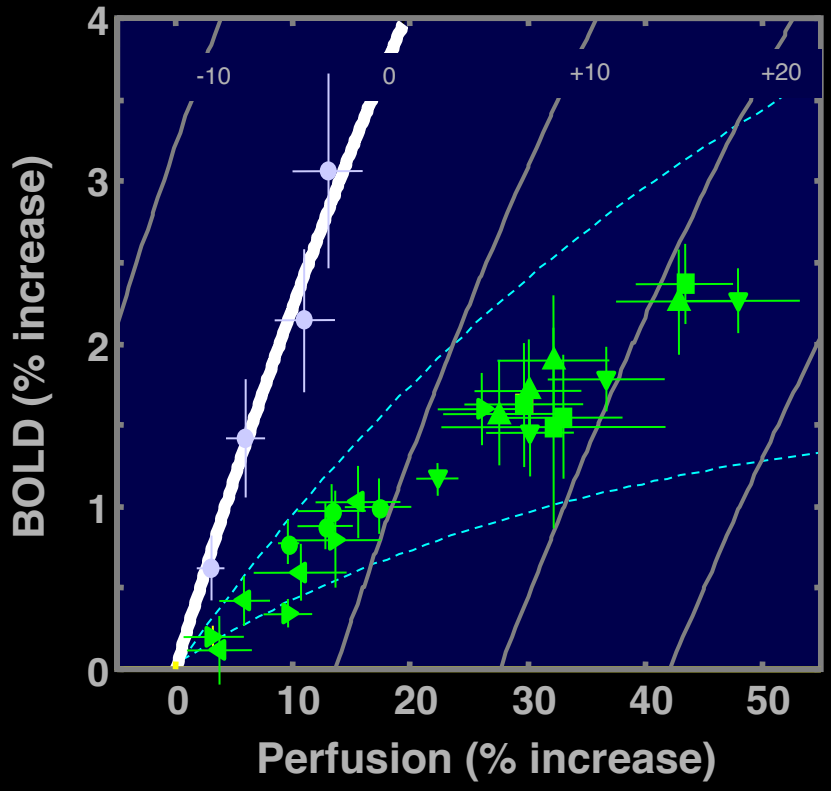


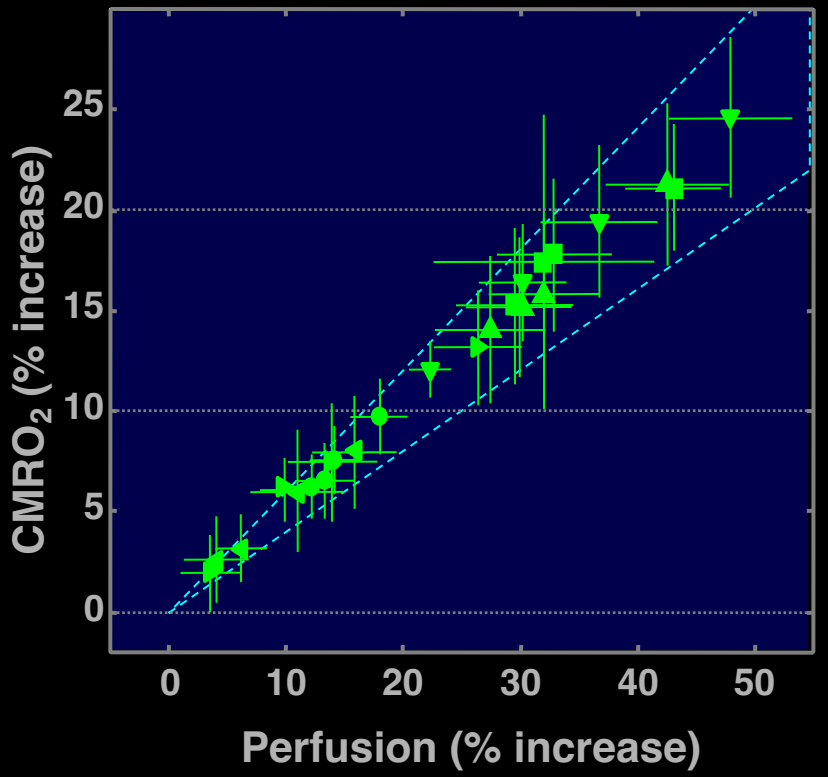
Simultaneous Perfusion and BOLD imaging during graded visual activation and hypercapnia

N=12

CBF-$CMRO_2$ coupling

Hoge, et al.

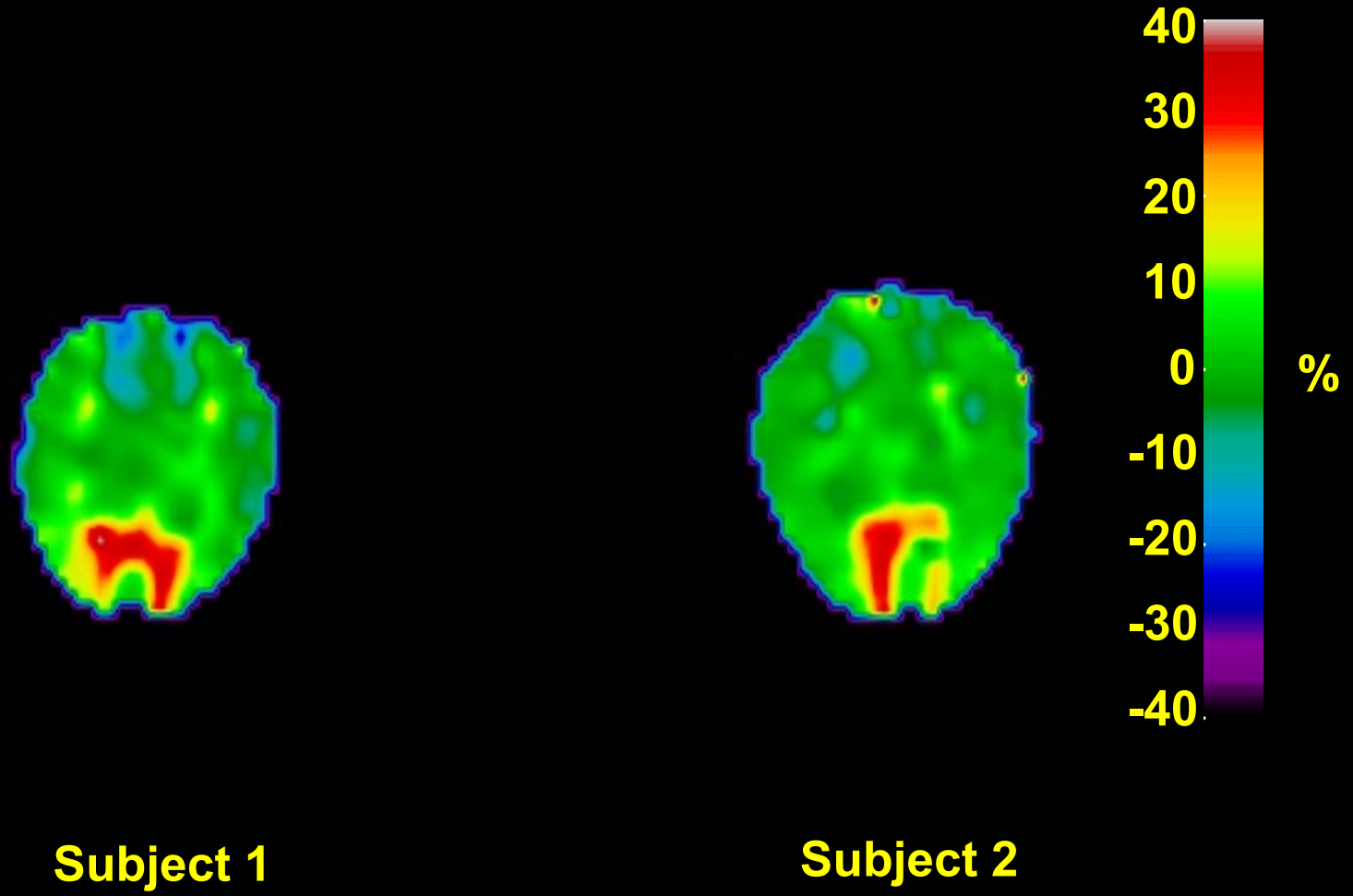




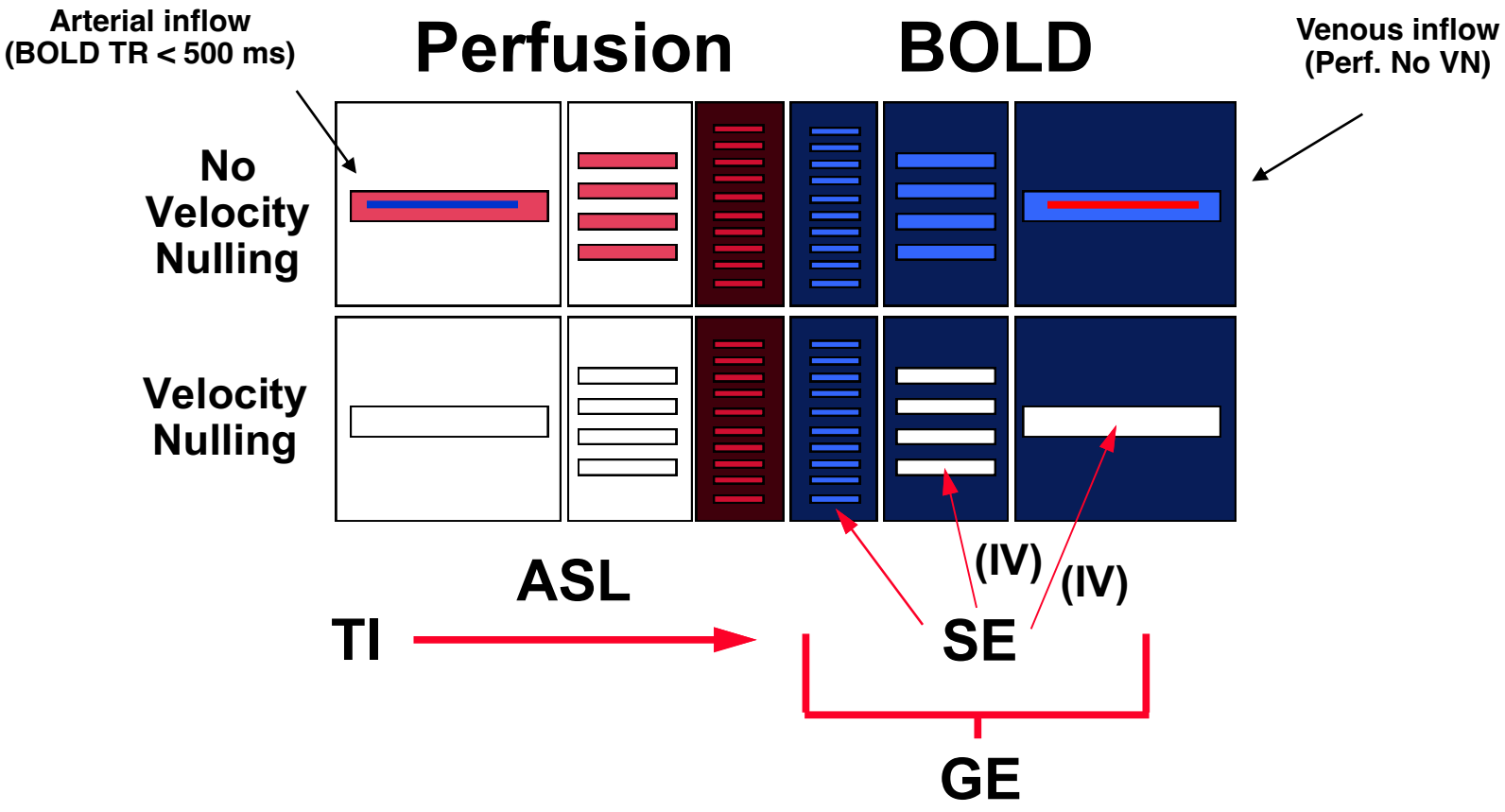
Characterizing Activation-induced $CMRO_2$ changes using calibration with hypercapnia

Hoge, et al.

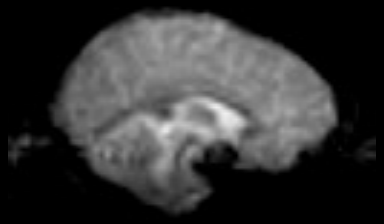
Computed $CMRO_2$ changes

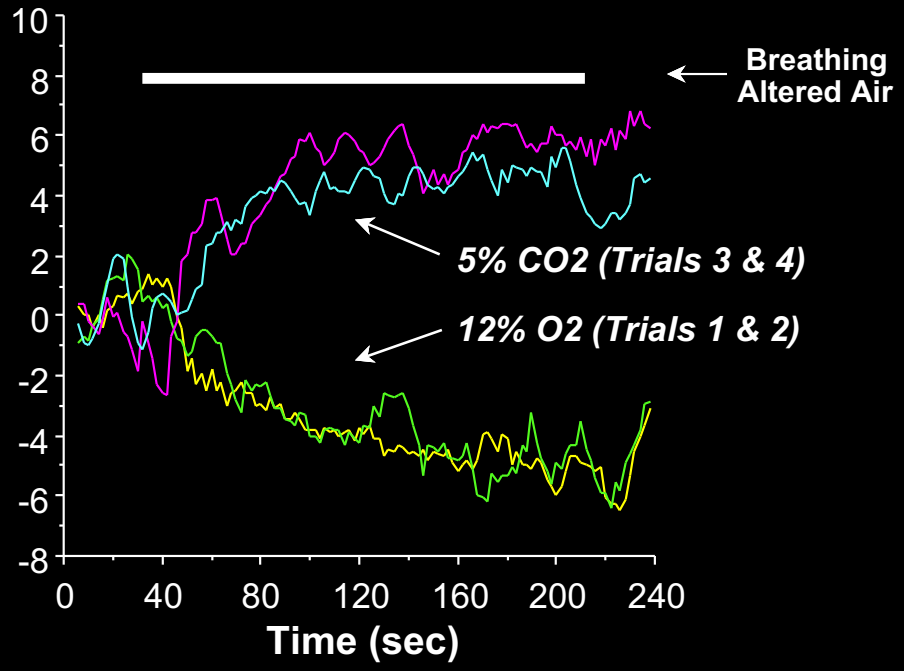


Hemodynamic Specificity

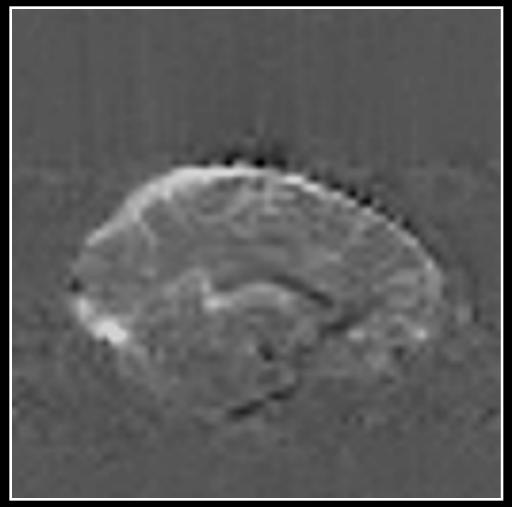


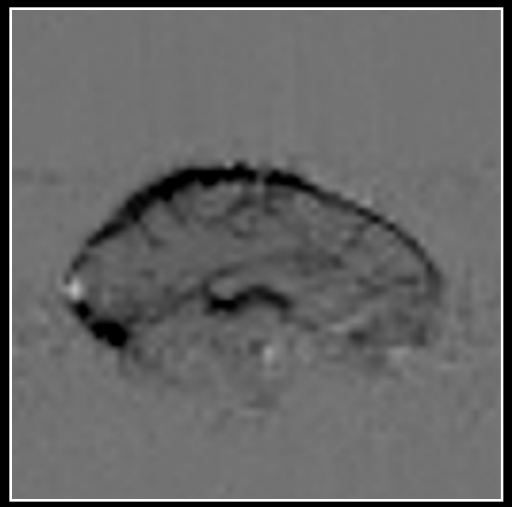
Hemdodynamic Stress Calibration





5% CO2

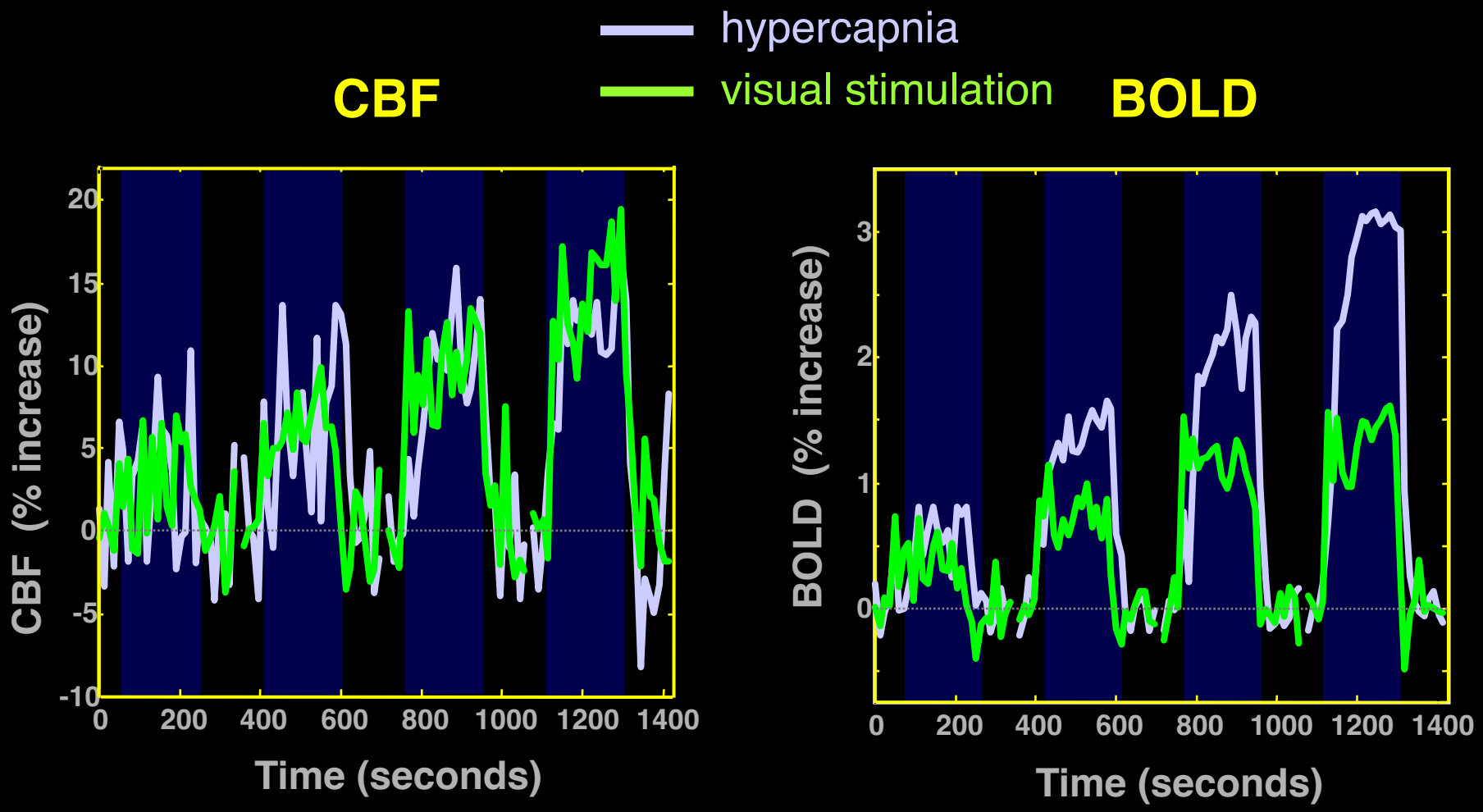




12% O2

$CMRO_2$-related BOLD signal deficit:

Hoge, et al.

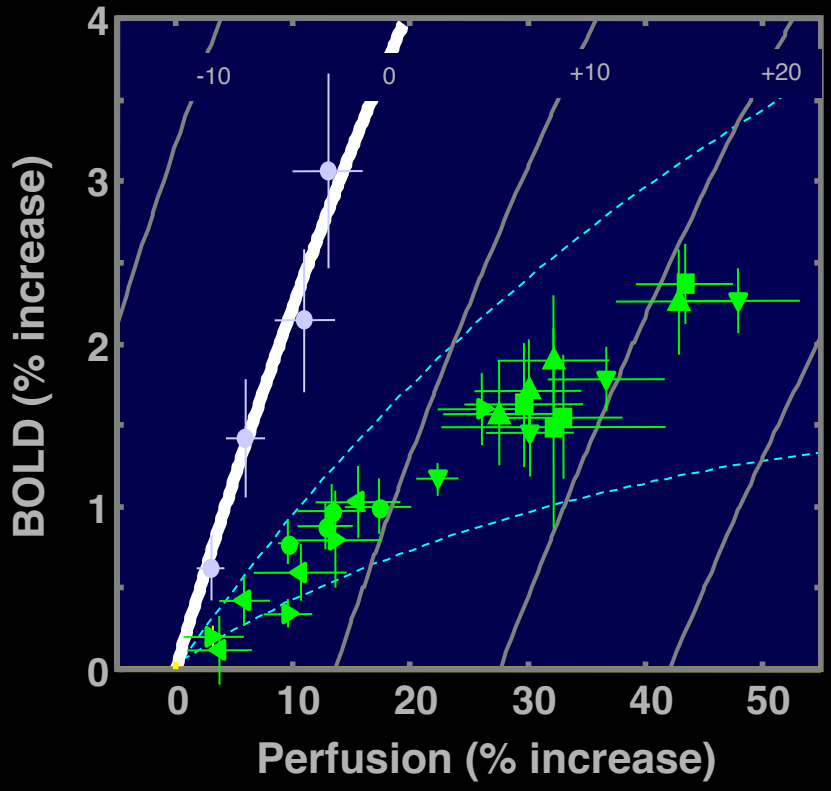


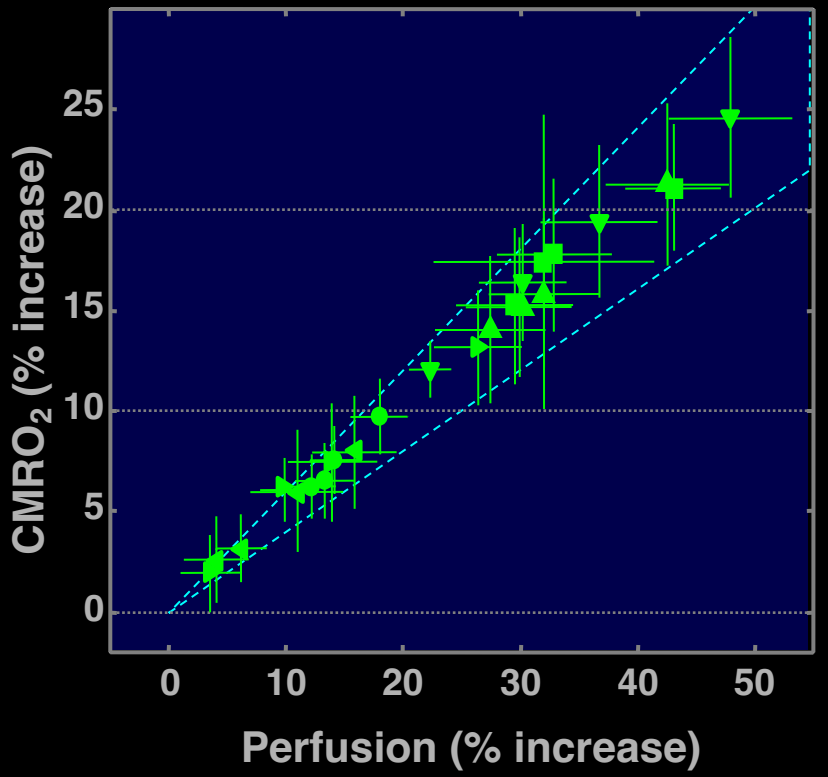
Simultaneous Perfusion and BOLD imaging during graded visual activation and hypercapnia

N=12

CBF-$CMRO_2$ coupling

Hoge, et al.

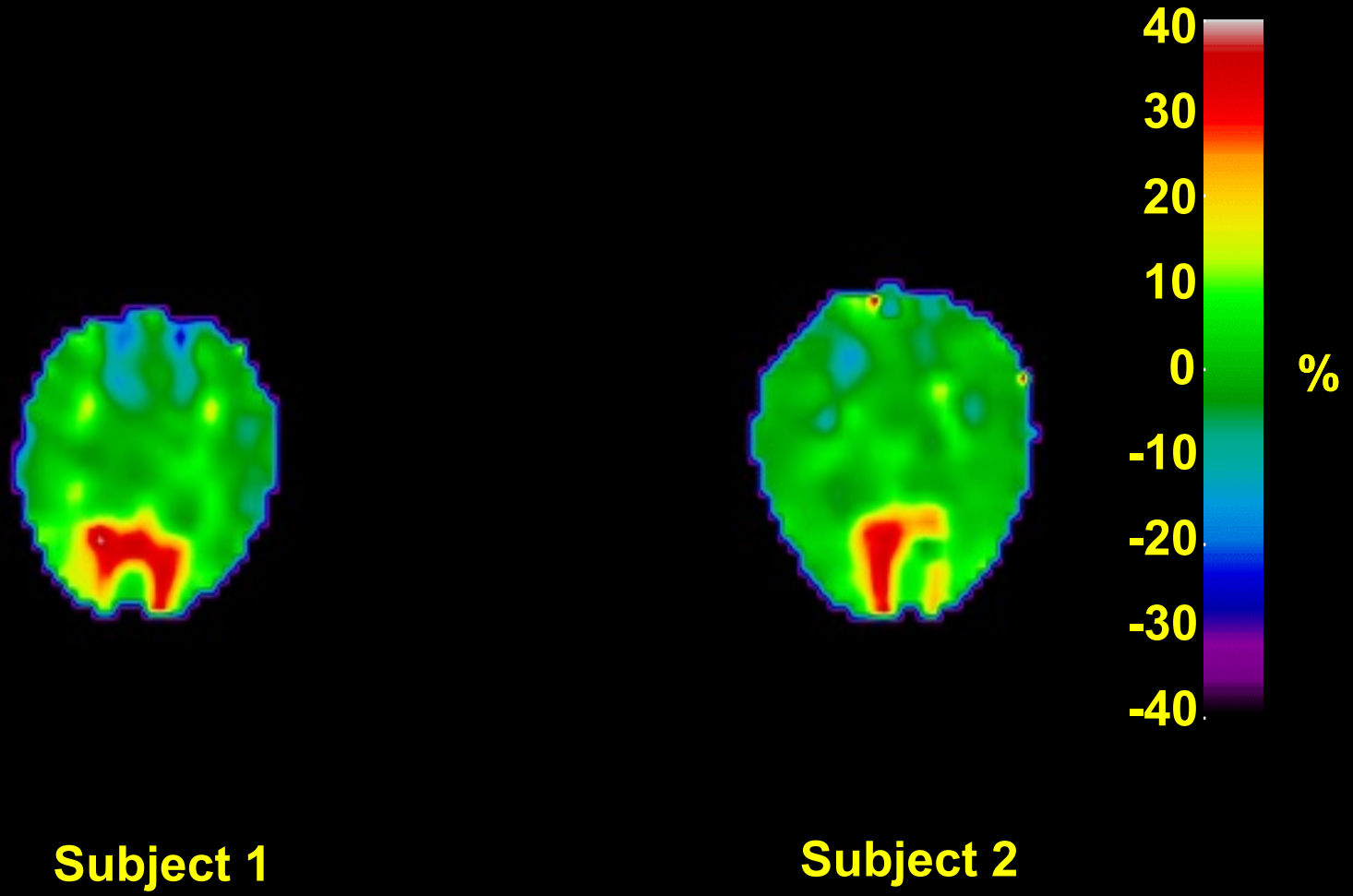




Characterizing Activation-induced $CMRO_2$ changes using calibration with hypercapnia

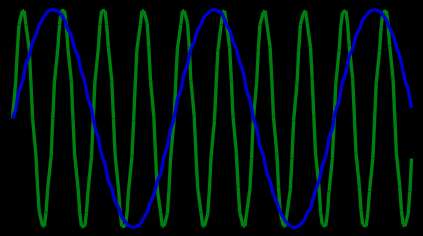
Hoge, et al.

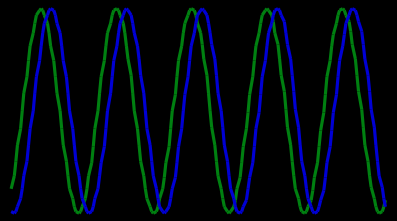
Computed $CMRO_2$ changes

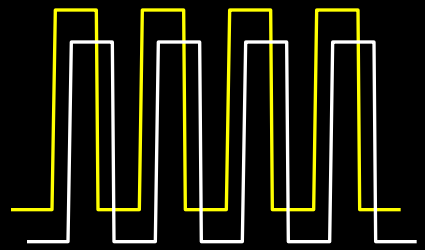


Neuronal Activation Input Strategies

1. Block Design
2. Frequency Encoding
3. Phase Encoding
4. Single Event
5. Orthogonal Block Design
6. Free Behavior Design.



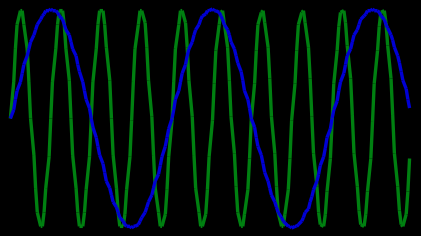




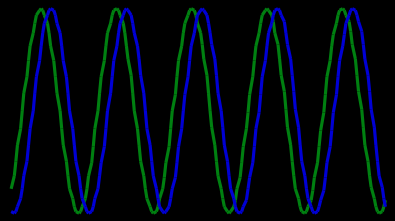
Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

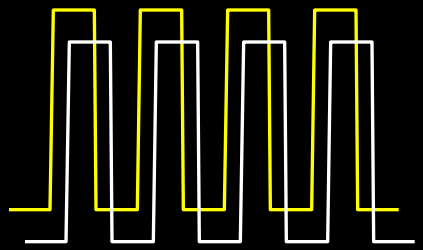


3. Phase Encoding

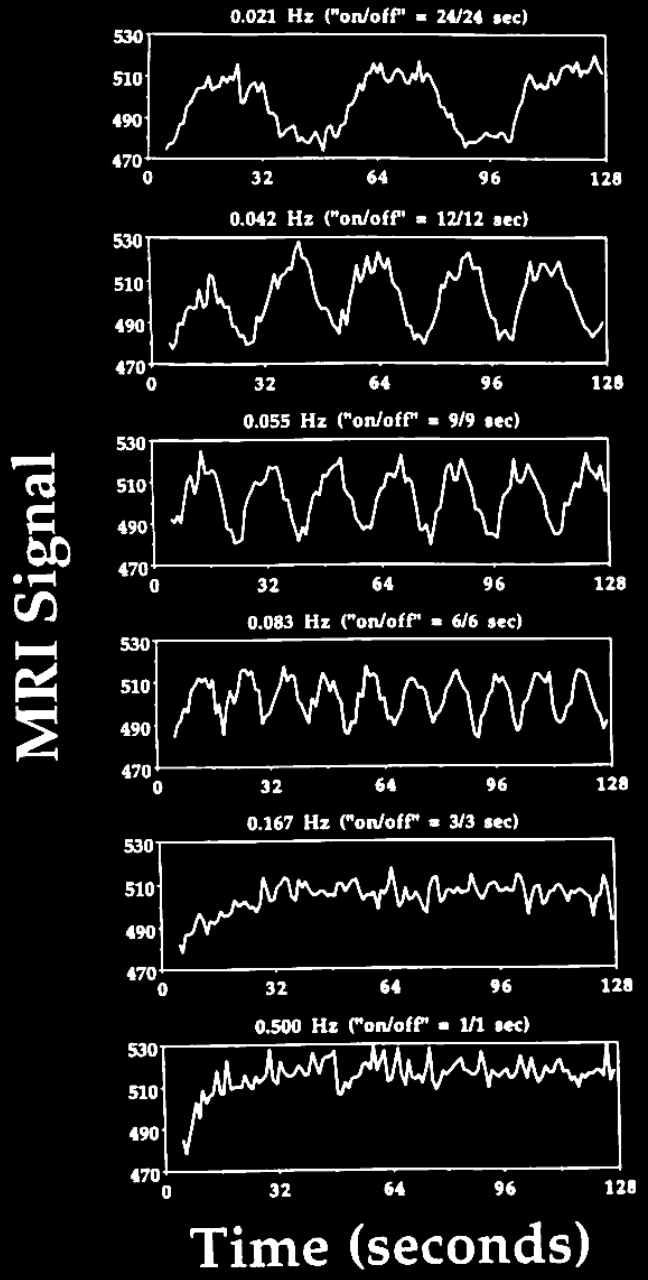


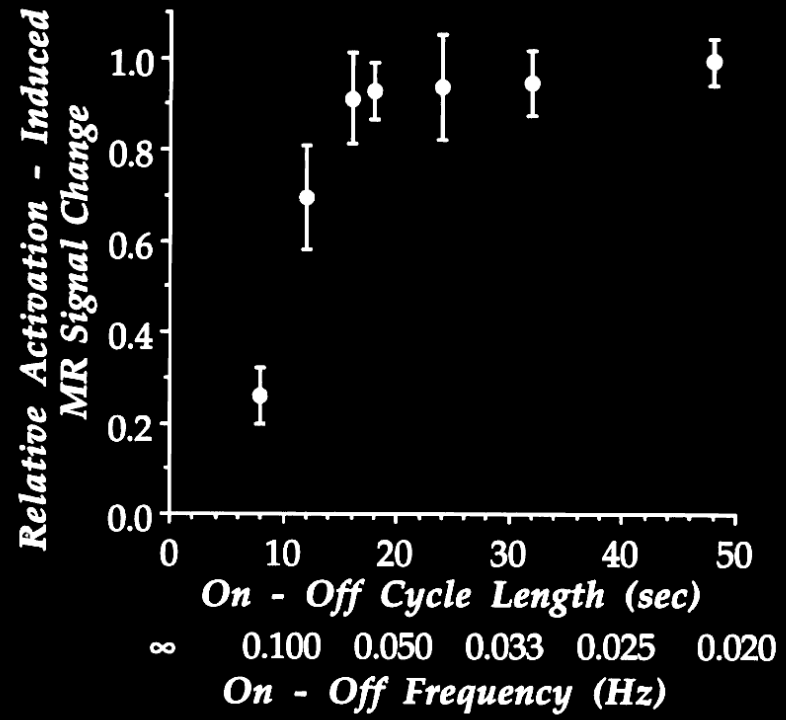
4. Single Event

5. Orthogonal Block Design

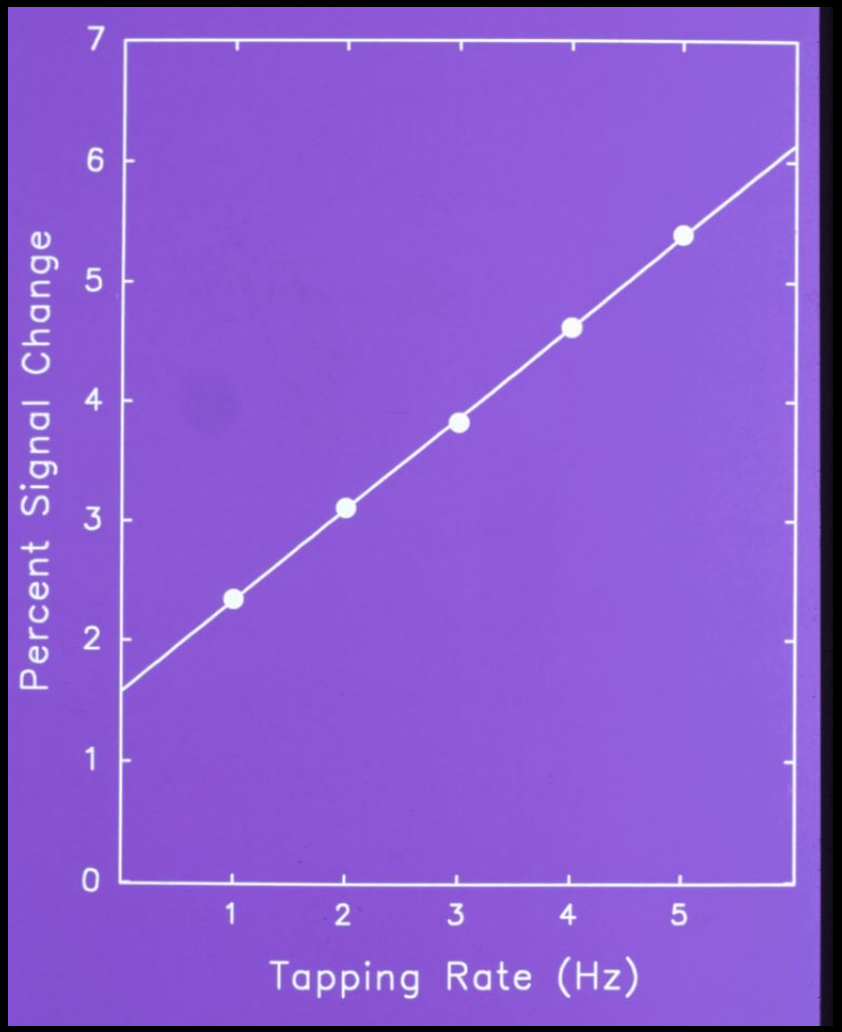


6. Free Behavior Design.

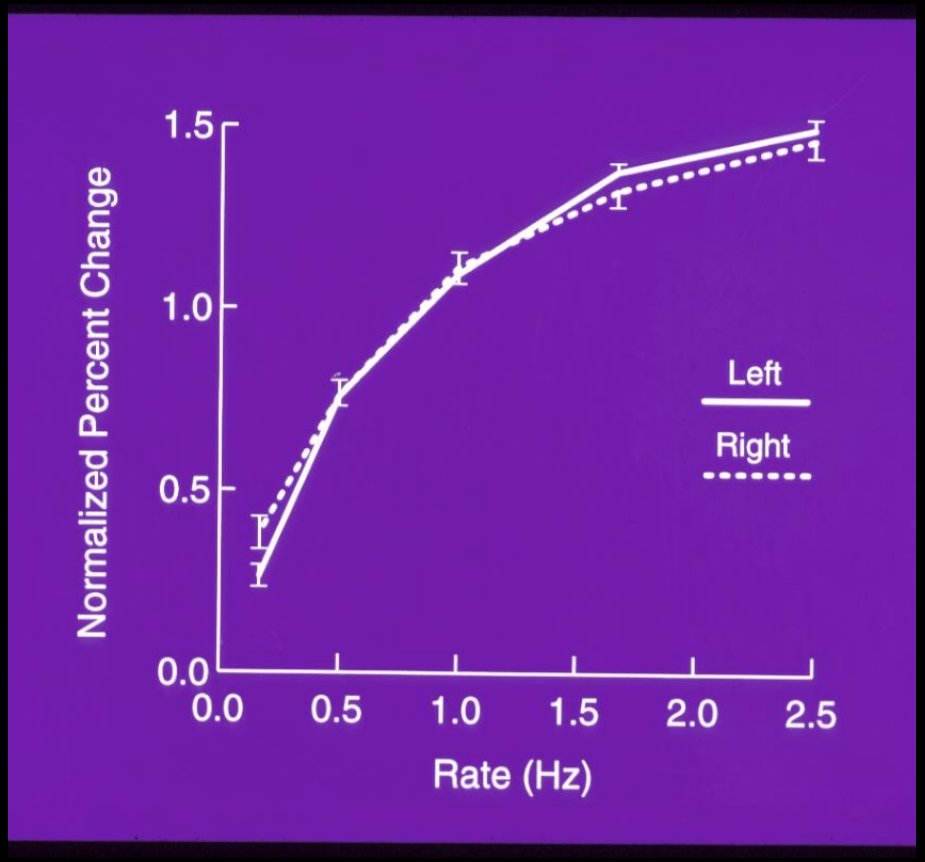

0.021 Hz ("on/off" = 24/24 sec)
0.042 Hz ("on/off" = 12/12 sec)
0.055 Hz ("on/off" = 9/9 sec)
0.083 Hz ("on/off" = 6/6 sec)
0.167 Hz ("on/off" = 3/3 sec)
0.500 Hz ("on/off" = 1/1 sec)
530
510
490
470
0
32
64
96
128
MRI Signal
Time (seconds)

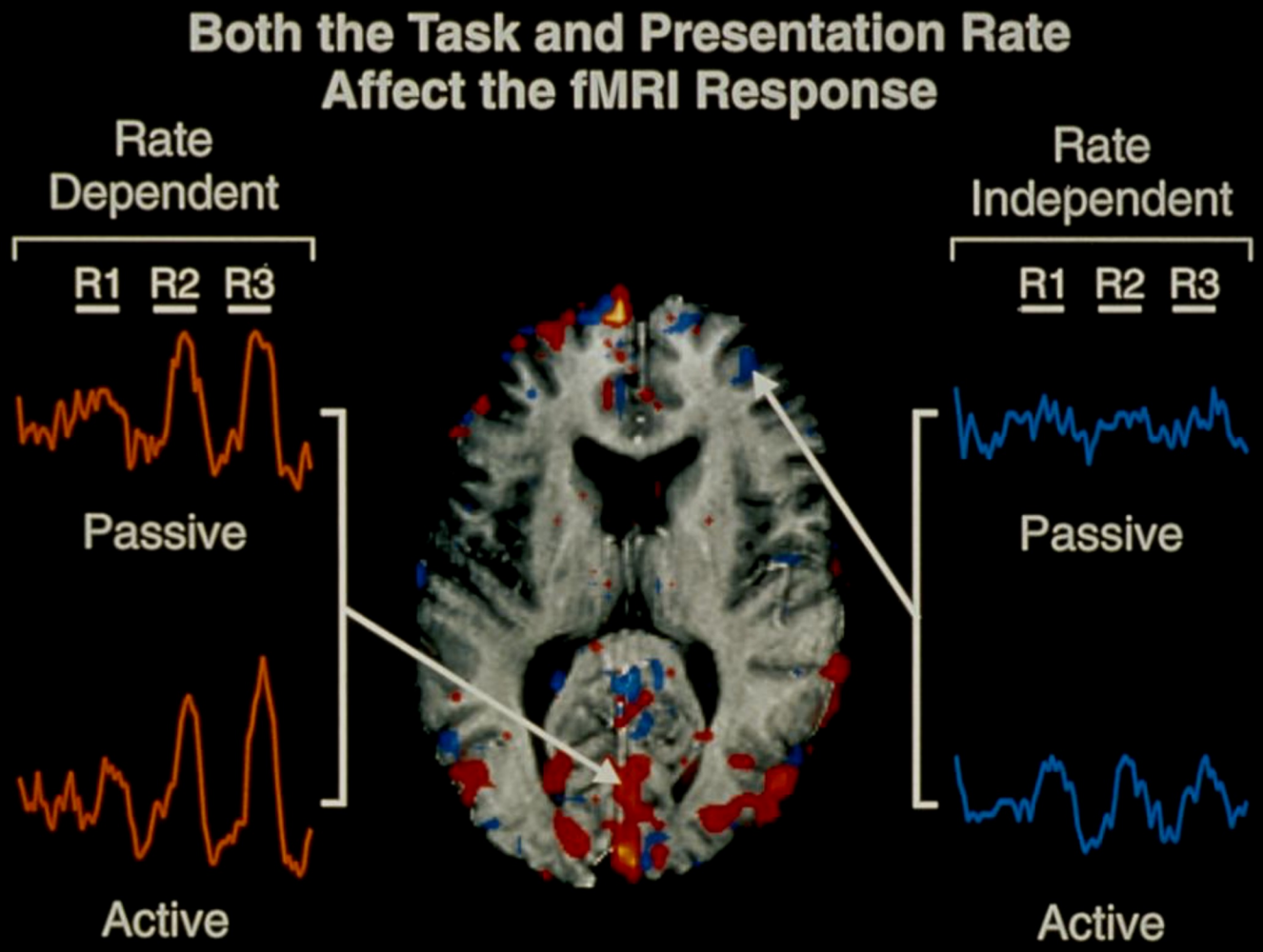

Relative Activation - Induced MR Signal Change
1.0
0.8
0.6
0.4
0.2
0.0
0
10
20
30
40
50
On - Off Cycle Length (sec)
∞
0.100
0.050
0.033
0.025
0.020
On - Off Frequency (Hz)

Motor Cortex

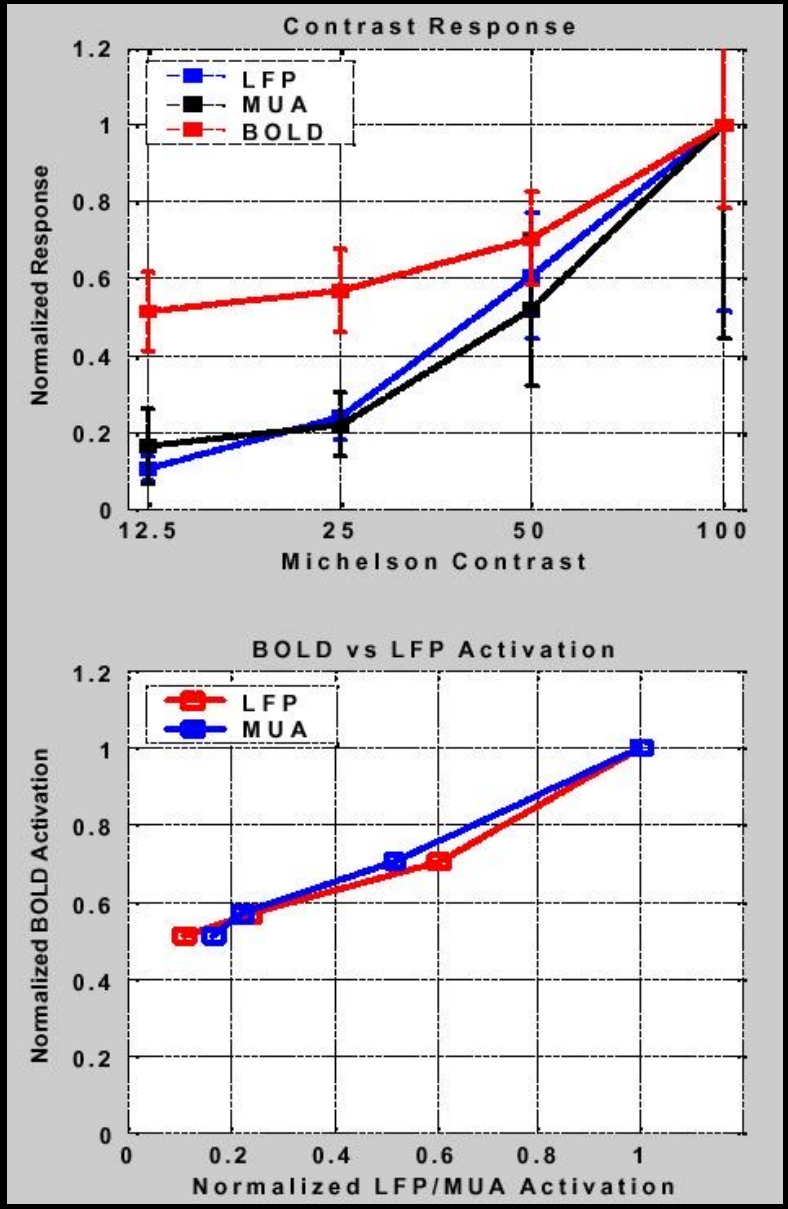


Auditory Cortex




Both the Task and Presentation Rate
Affect the fMRI Response
Rate
Dependent
R1 R2 R3
Passive
Active
Rate
Independent
R1 R2 R3
Passive
Active

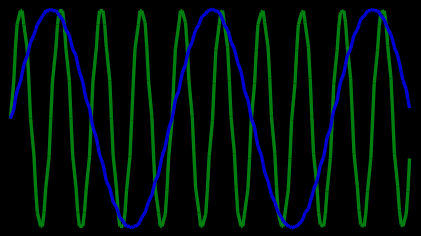
DeYoe et al.



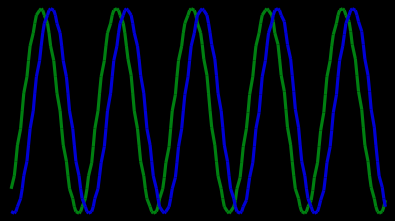
Logothetis et al. Nature, 412, 150-157

Neuronal Activation Input Strategies

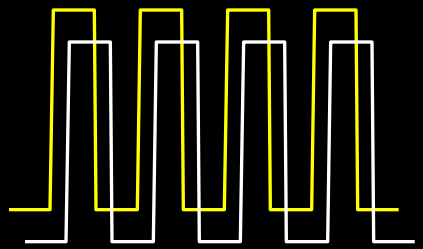
1. Block Design
2. Frequency Encoding



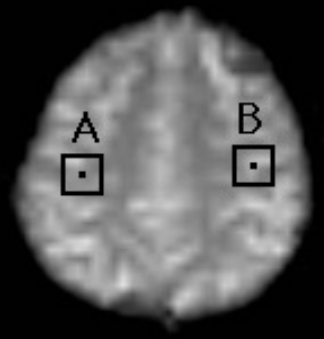
3. Phase Encoding

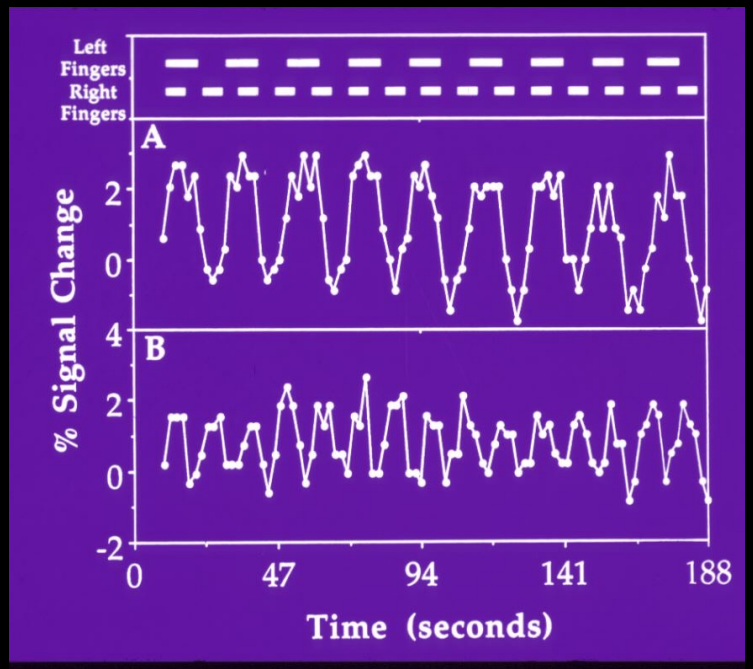


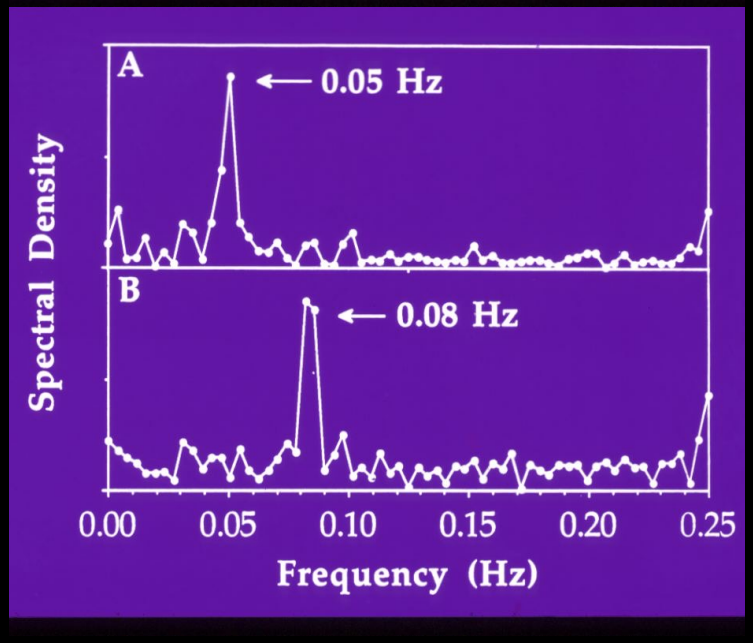
4. Single Event
5. Orthogonal Block Design

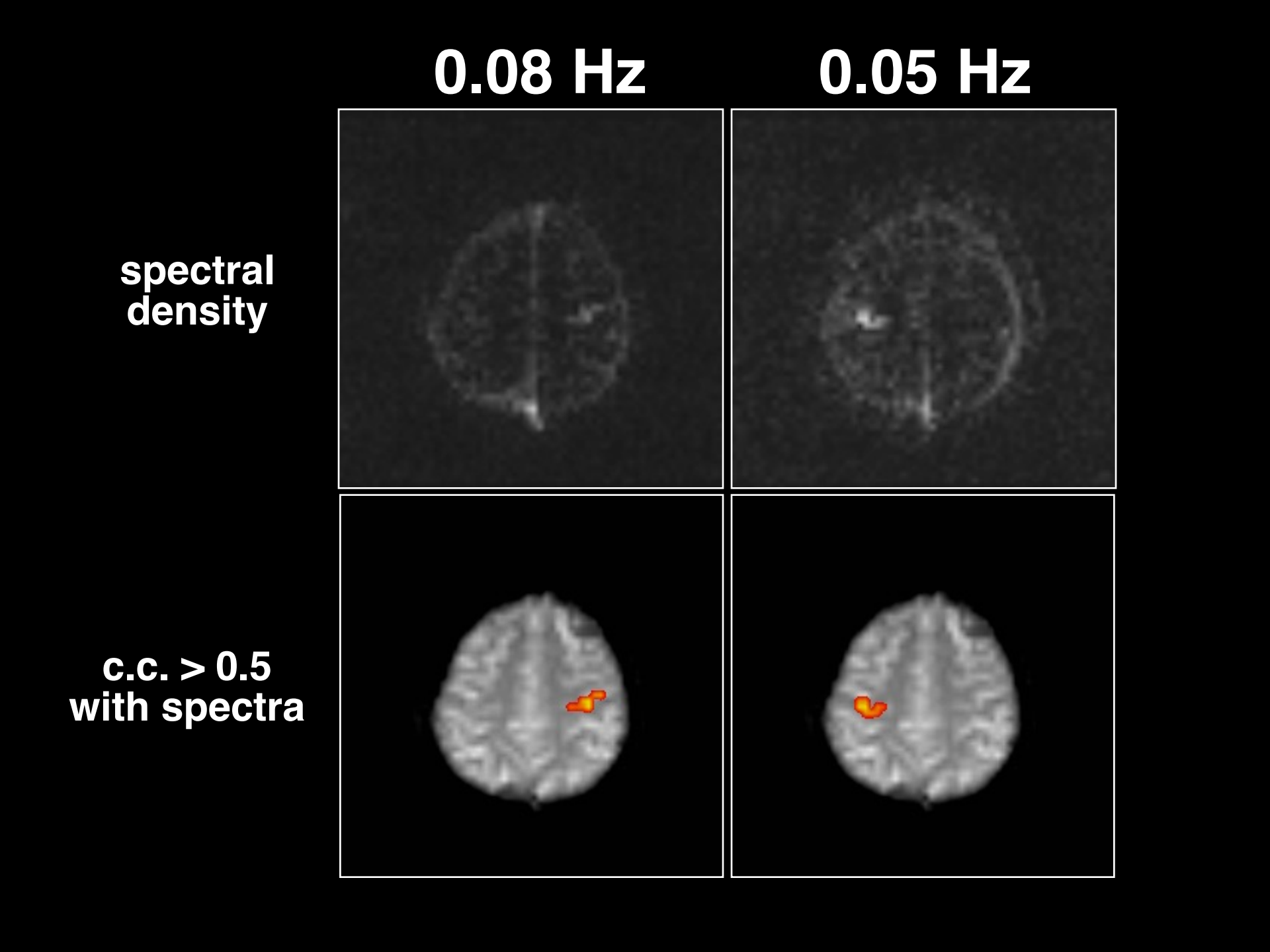


6. Free Behavior Design.


A
B


Left Fingers
Right Fingers
A
B
% Signal Change
2
0
4
2
0
-2
0
47
94
141
188
Time (seconds)

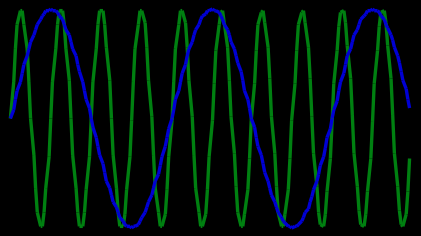

A
0.05 Hz
B
0.08 Hz
Spectral Density
0.00
0.05
0.10
0.15
0.20
0.25
Frequency (Hz)


0.08 Hz
0.05 Hz
spectral density
c.c. > 0.5 with spectra

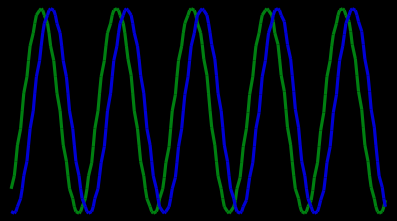
Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

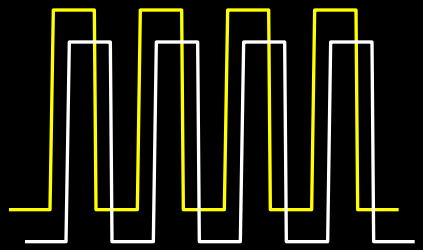


3. Phase Encoding

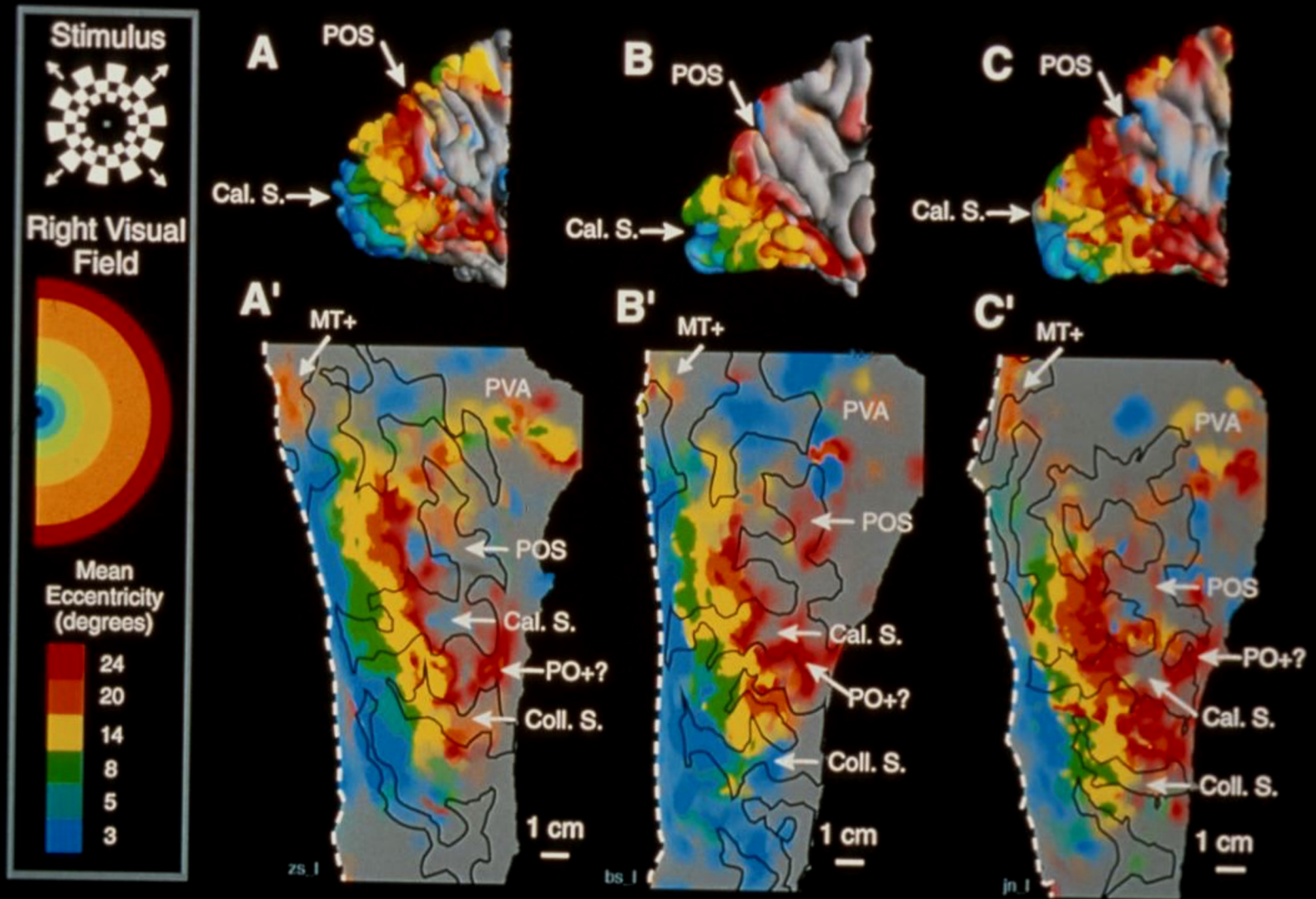


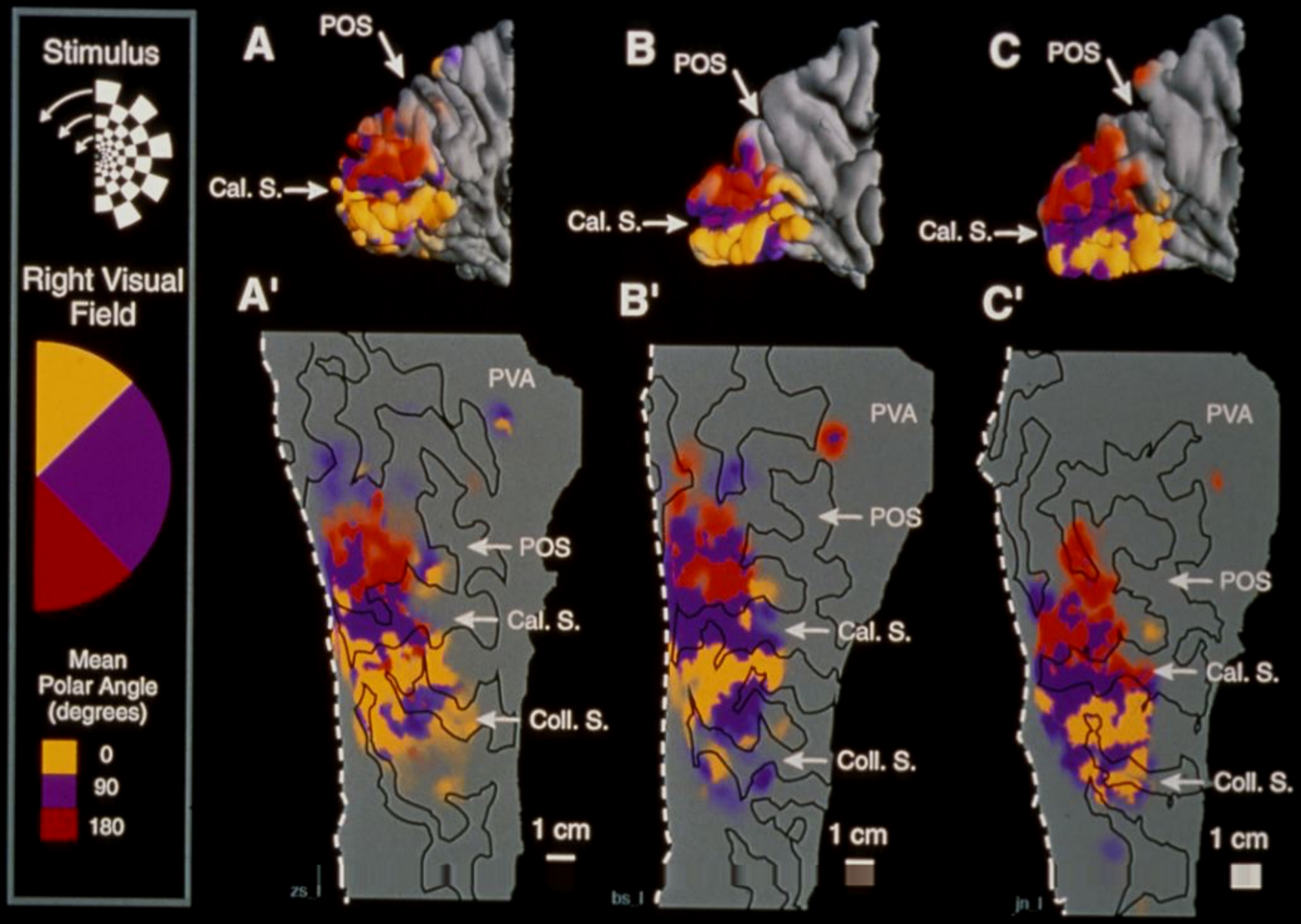
4. Single Event

5. Orthogonal Block Design



6. Free Behavior Design.

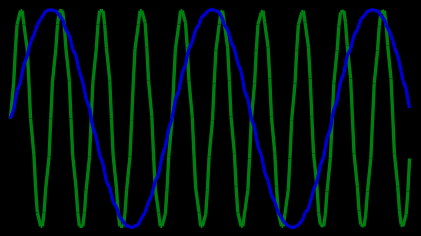

Stimulus
Right Visual Field
Mean Eccentricity (degrees)
24
20
14
8
5
3
A
POS
Cal. S.
B
POS
Cal. S.
C
POS
Cal. S.
A'
MT+
PVA
POS
Cal. S.
PO+?
Coll. S.
1 cm
zs_l
B'
MT+
PVA
POS
Cal. S.
PO+?
Coll. S.
1 cm
bs_l
C'
MT+
PVA
POS
PO+?
Cal. S.
Coll. S.
1 cm
jn_l


Stimulus
Right Visual Field
Mean Polar Angle (degrees)
0
90
180
A
POS
Cal. S.
B
POS
Cal. S.
C
POS
Cal. S.
A'
PVA
POS
Cal. S.
Coll. S.
1 cm
zs_l
B'
PVA
POS
Cal. S.
Coll. S.
1 cm
bs_l
C'
PVA
POS
Cal. S.
Coll. S.
1 cm
jn_l

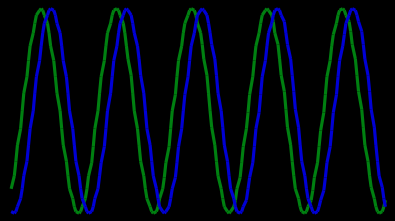
Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

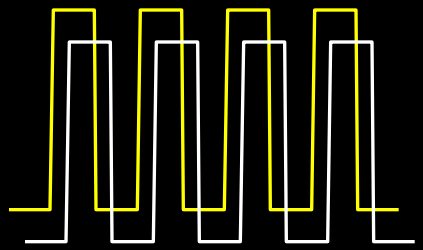


3. Phase Encoding

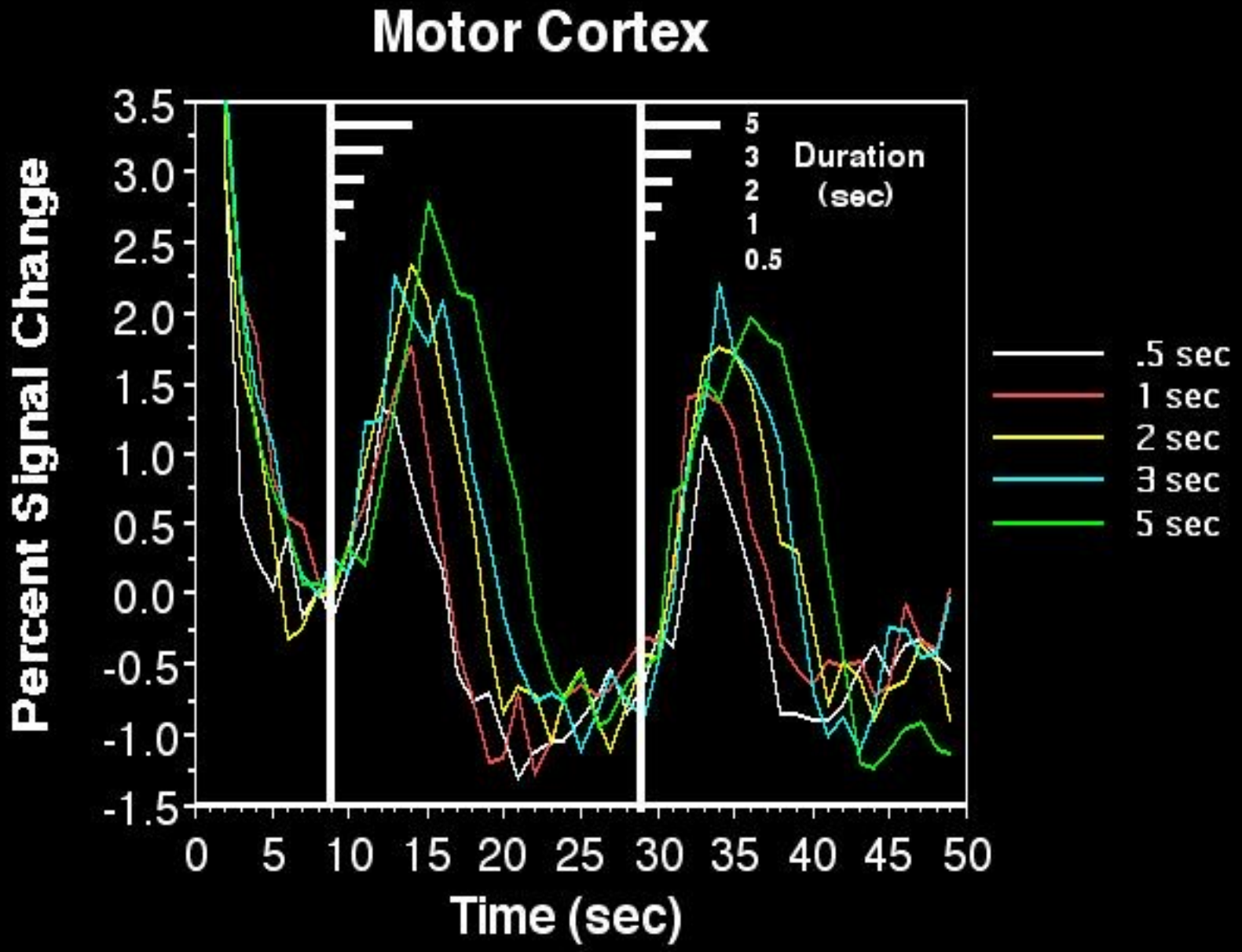


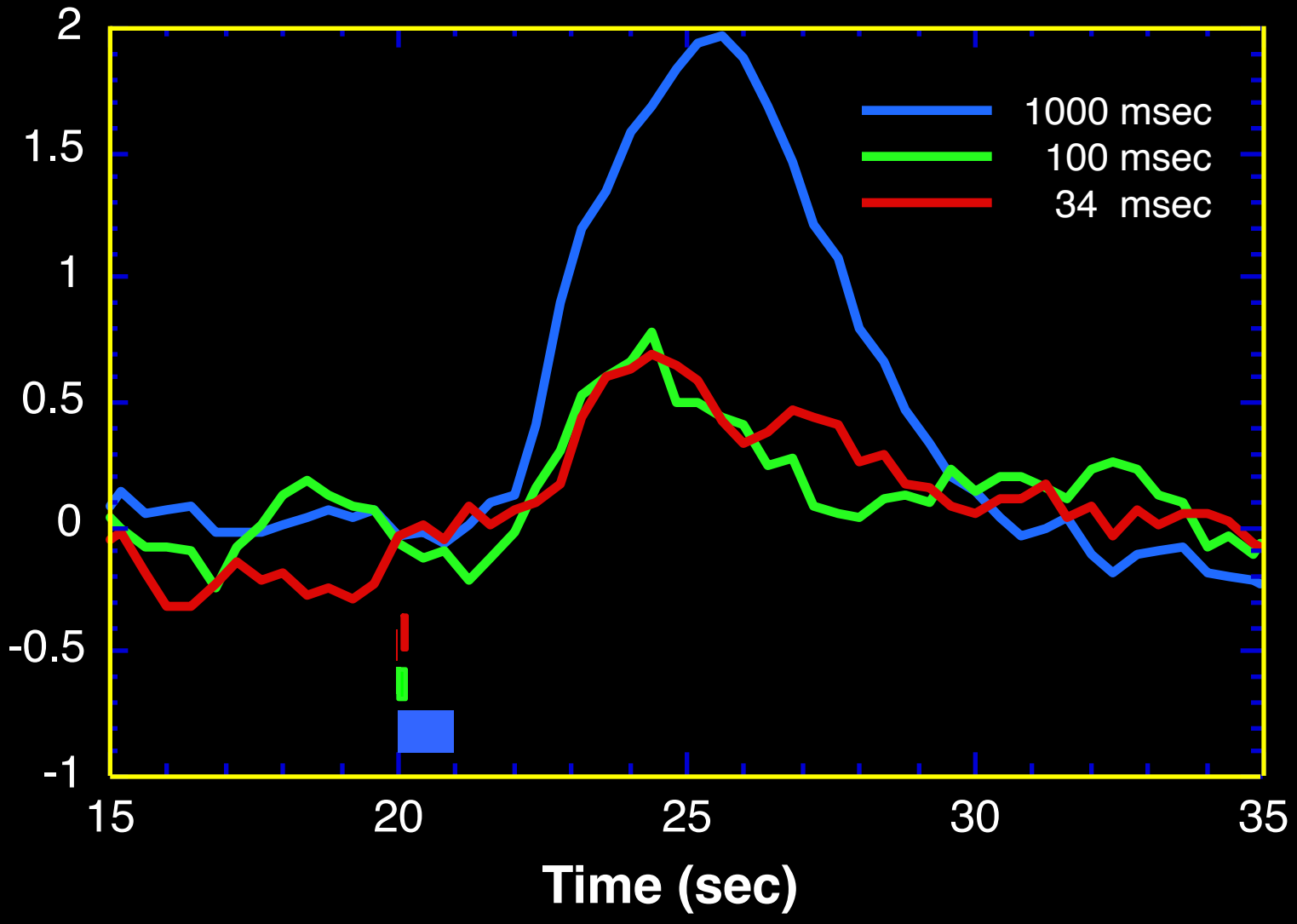
4. Single Event

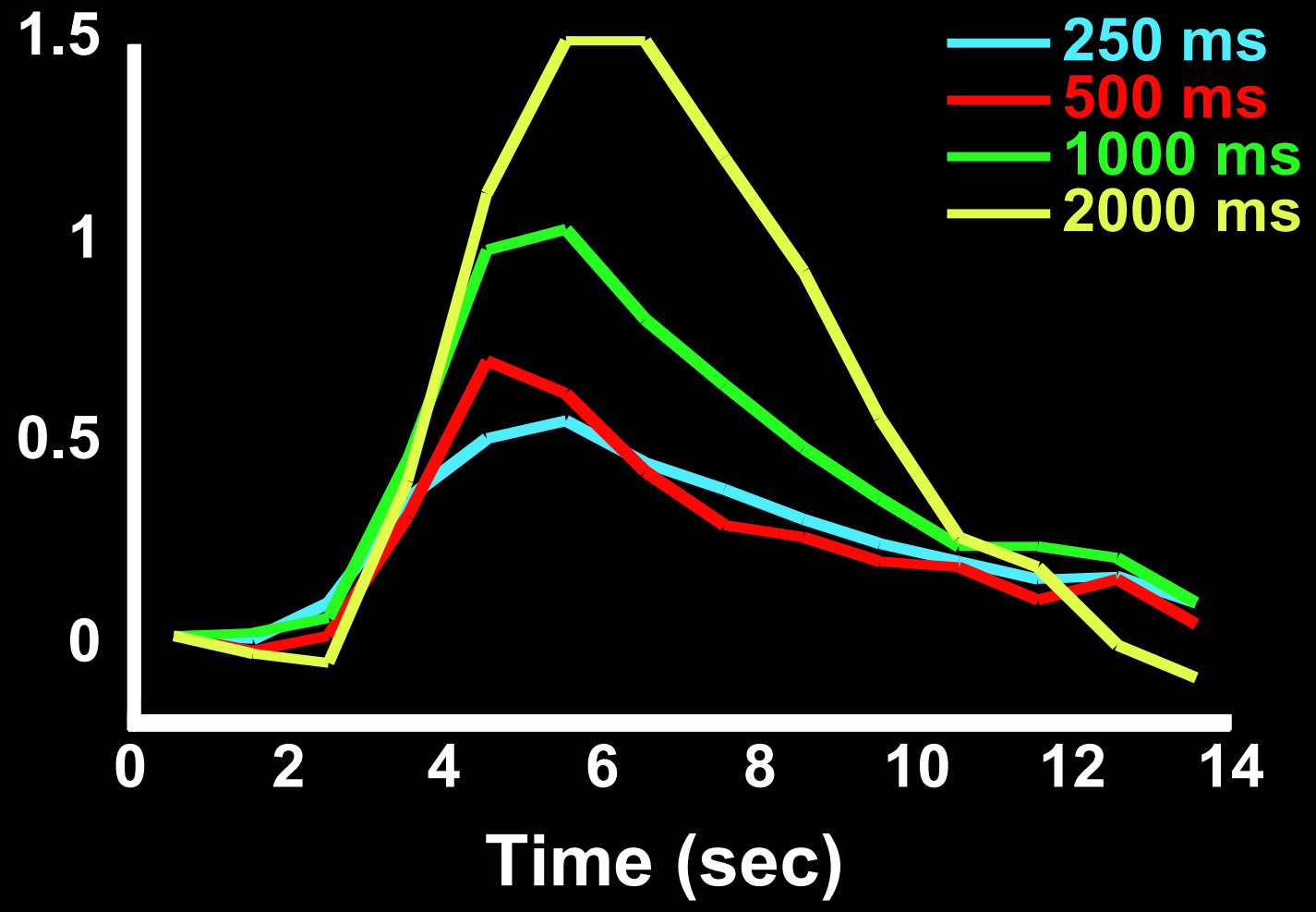
5. Orthogonal Block Design

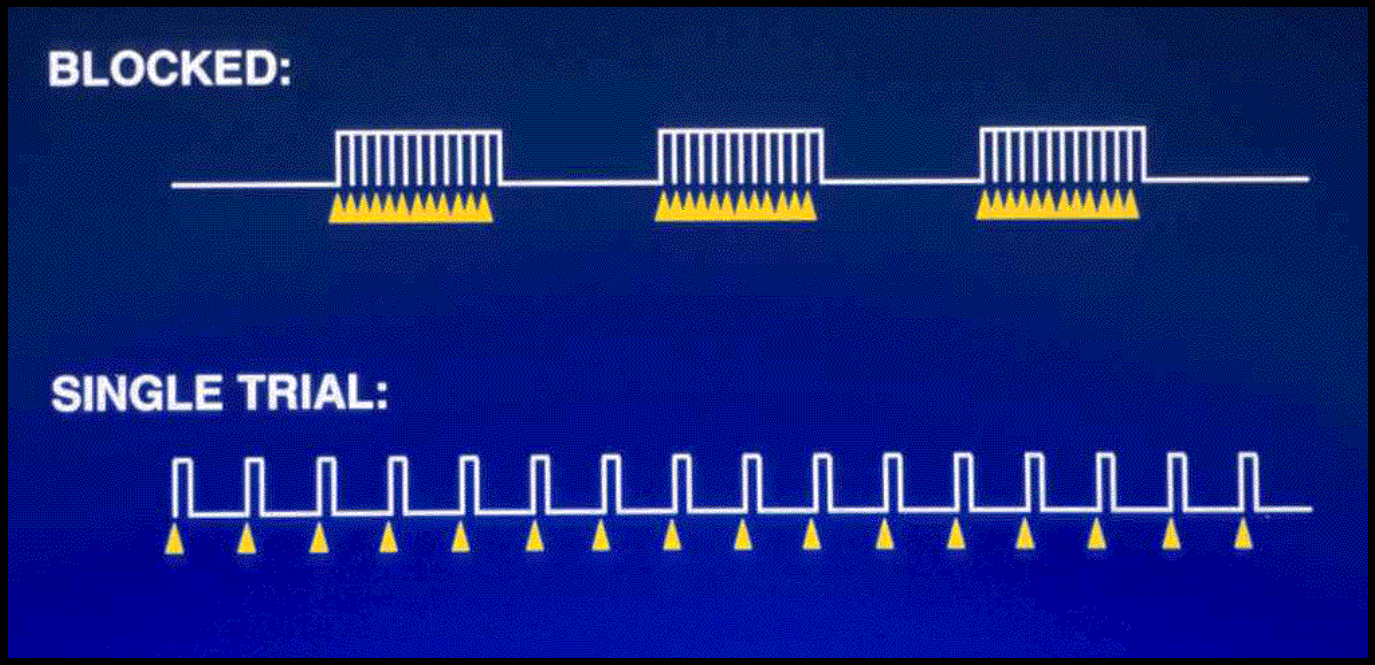


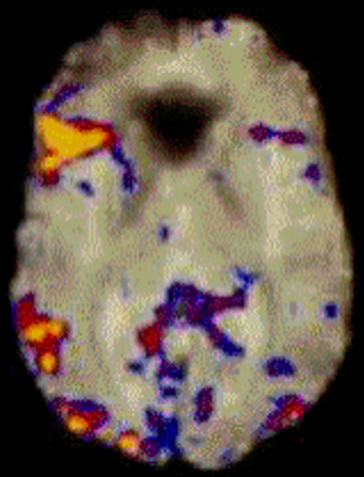
6. Free Behavior Design.

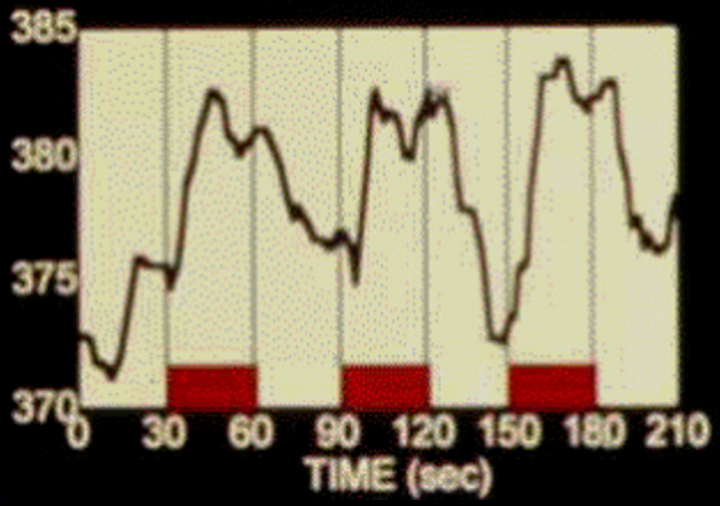

Motor Cortex
Percent Signal Change
3.5
3.0
2.5
2.0
1.5
1.0
0.5
0.0
-0.5
-1.0
-1.5
0
5
10
15
20
25
30
35
40
45
50
Time (sec)
5
3
2
1
0.5
Duration
(sec)
.5 sec
1 sec
2 sec
3 sec
5 sec

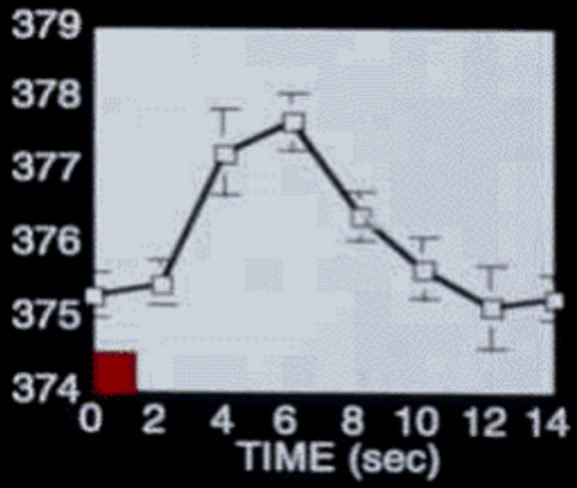

2
1.5
1
0.5
0
-0.5
-1
15
20
25
30
35
1000 msec
100 msec
34 msec
Time (sec)


1.5
1
0.5
0
0
2
4
6
8
10
12
14
Time (sec)
250 ms
500 ms
1000 ms
2000 ms

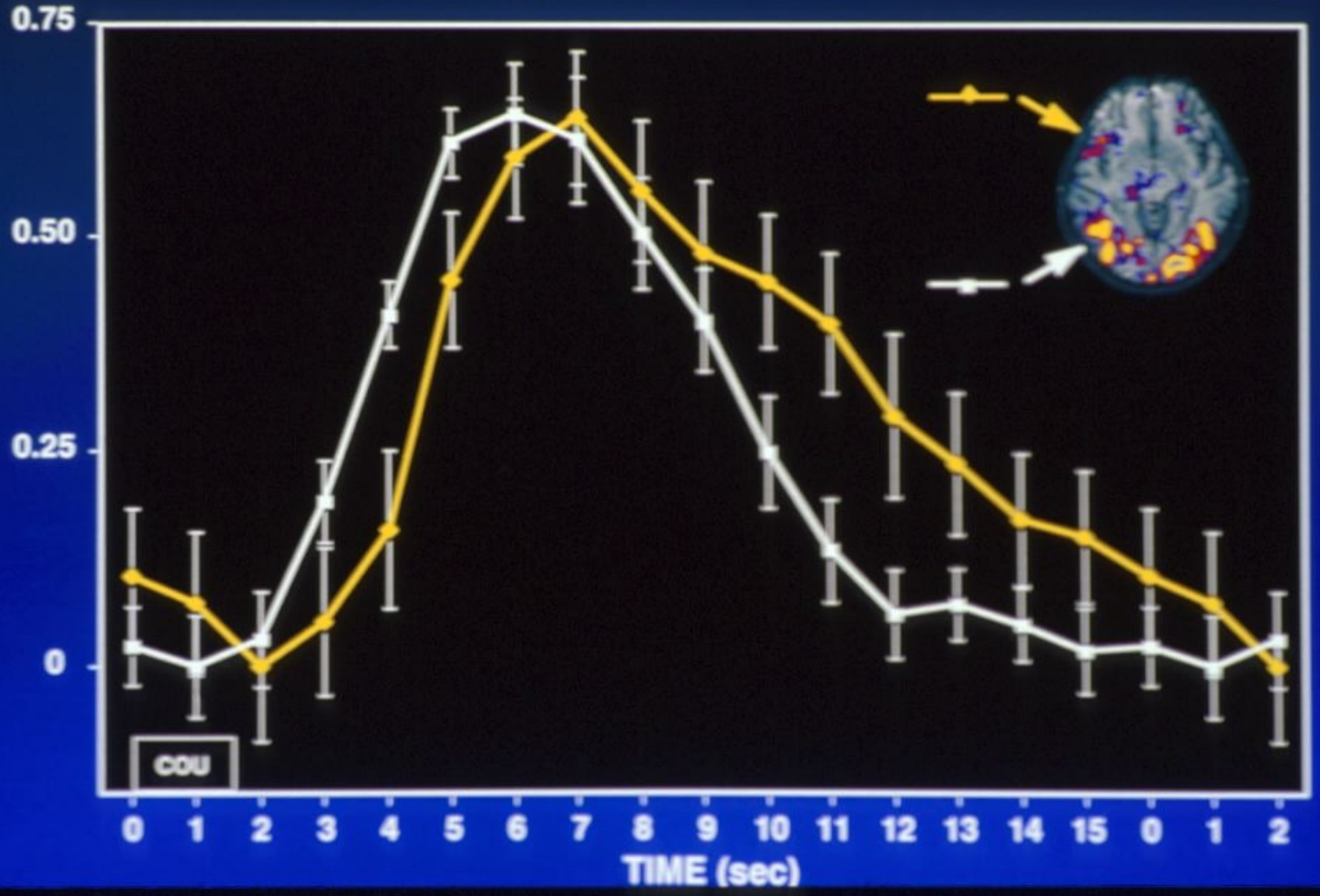

BLOCKED:
SINGLE TRIAL:




385
380
375
370
0 30 60 90 120 150 180 210
TIME (sec)

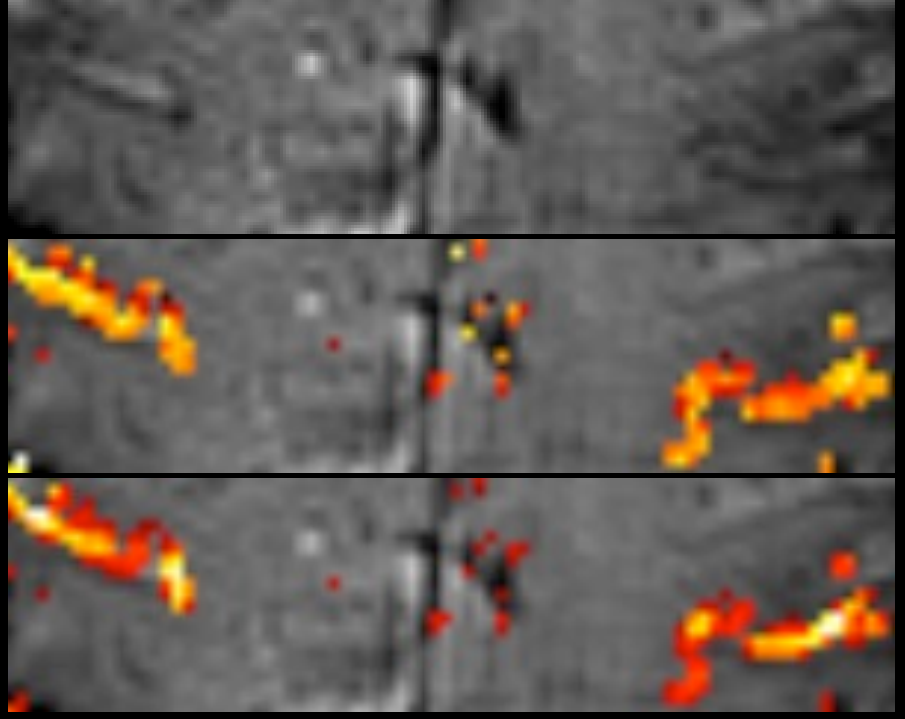

379
378
377
376
375
374
0 2 4 6 8 10 12 14
TIME (sec)

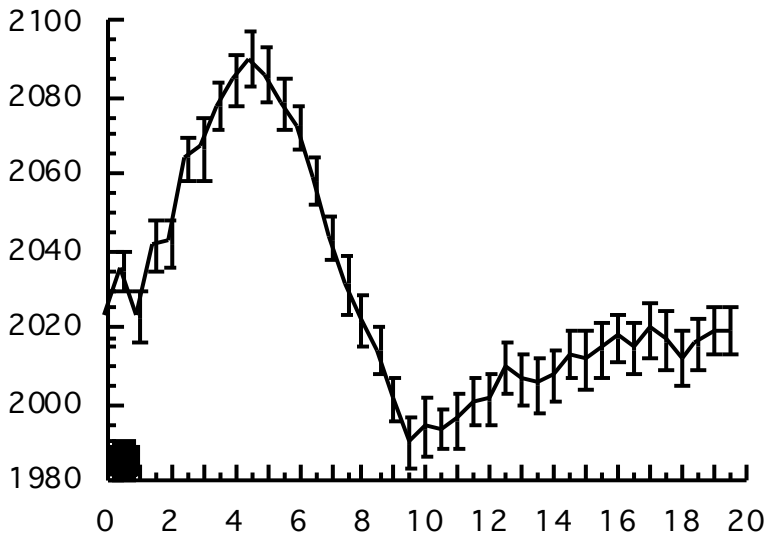
Time Course Comparison Across Brain Regions

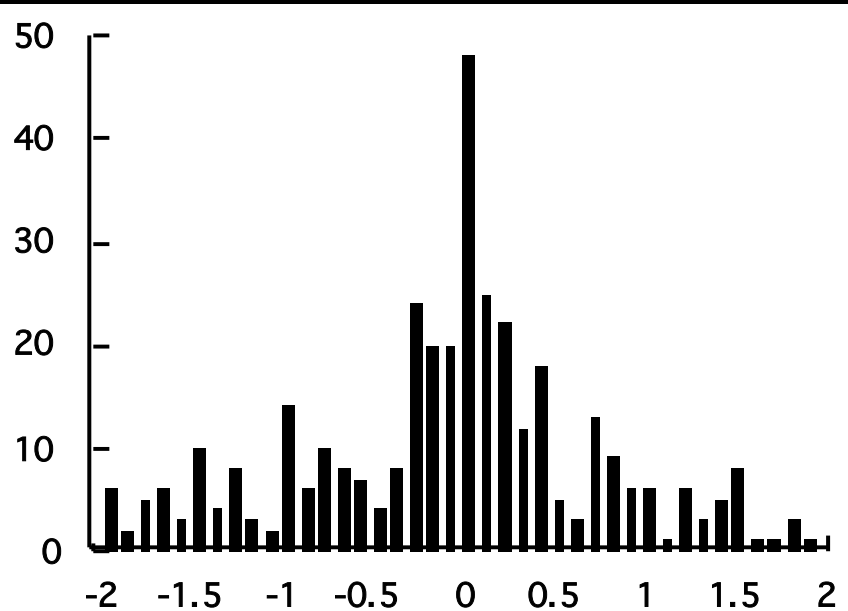


Latency

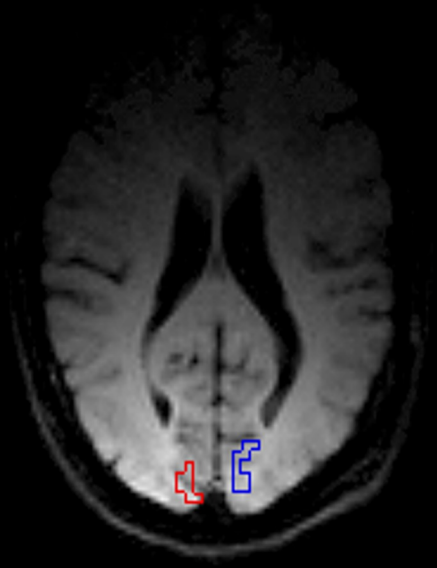
Magnitude





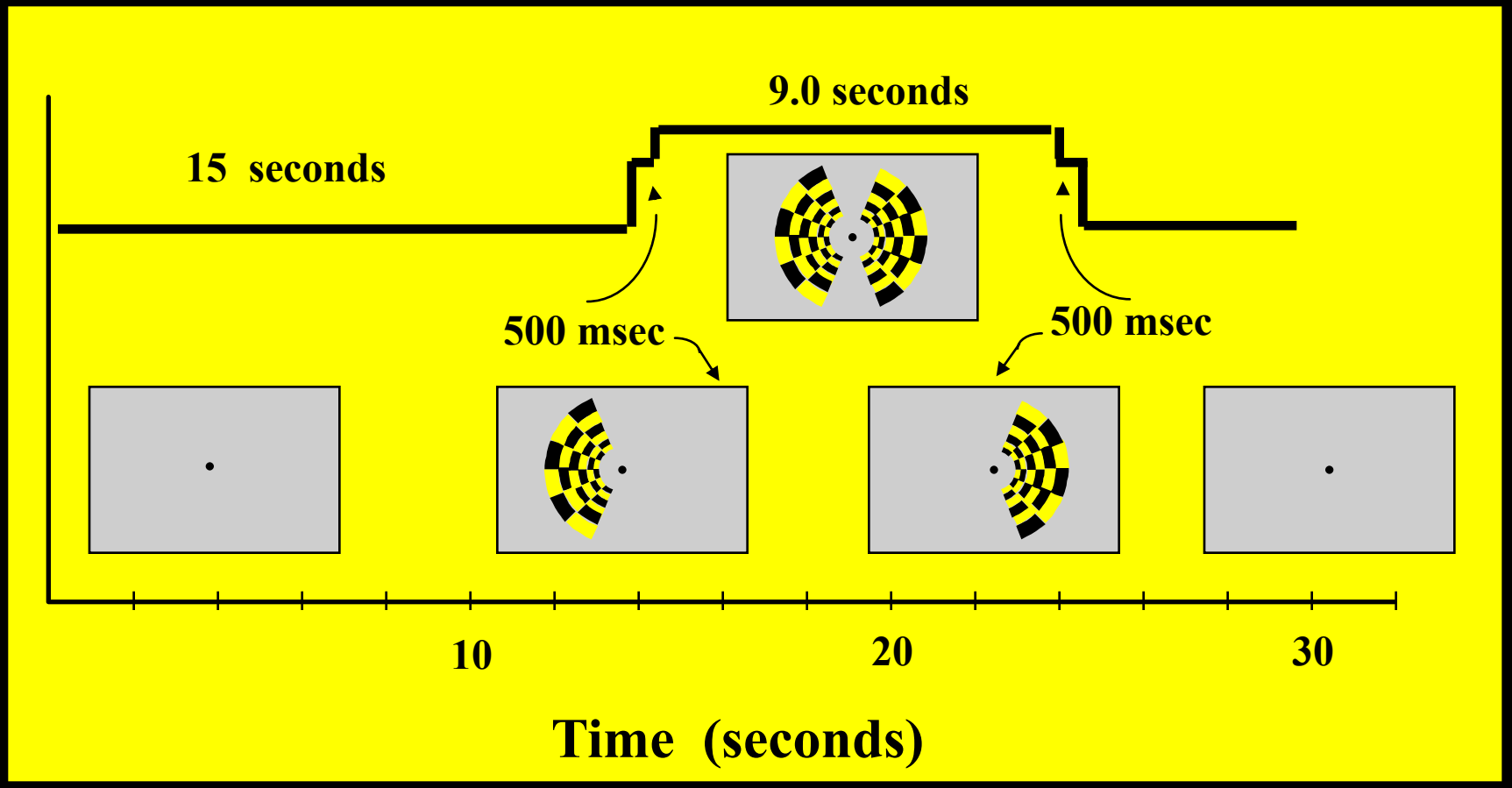


Regions of Interest Used for Hemi-Field Experiment

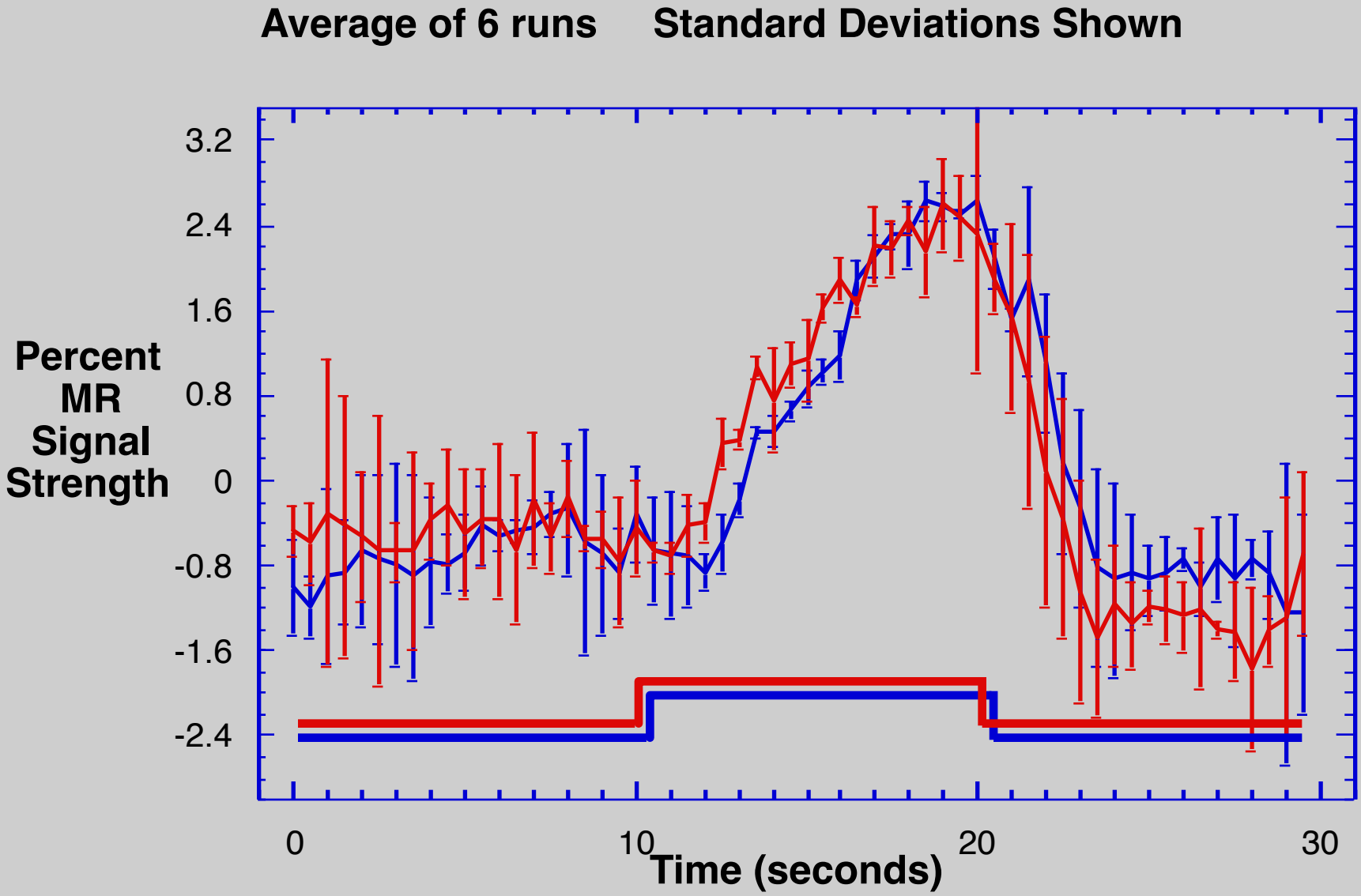


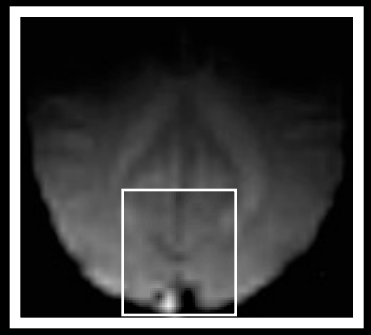
Right Hemisphere

Left Hemisphere


9.0 seconds
15 seconds
500 msec
500 msec
10
20
30
Time (seconds)

Hemi-field with 500 msec asynchrony



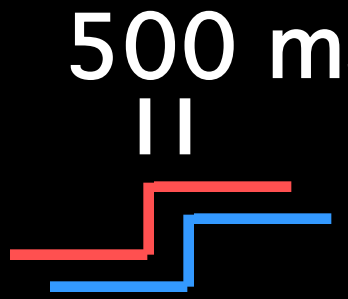


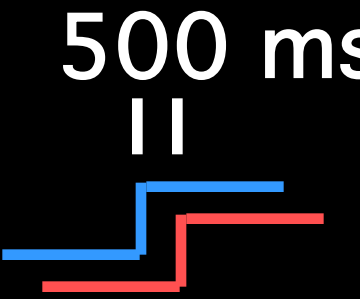
500 ms

500 ms

Right Hemifield

Left Hemifield



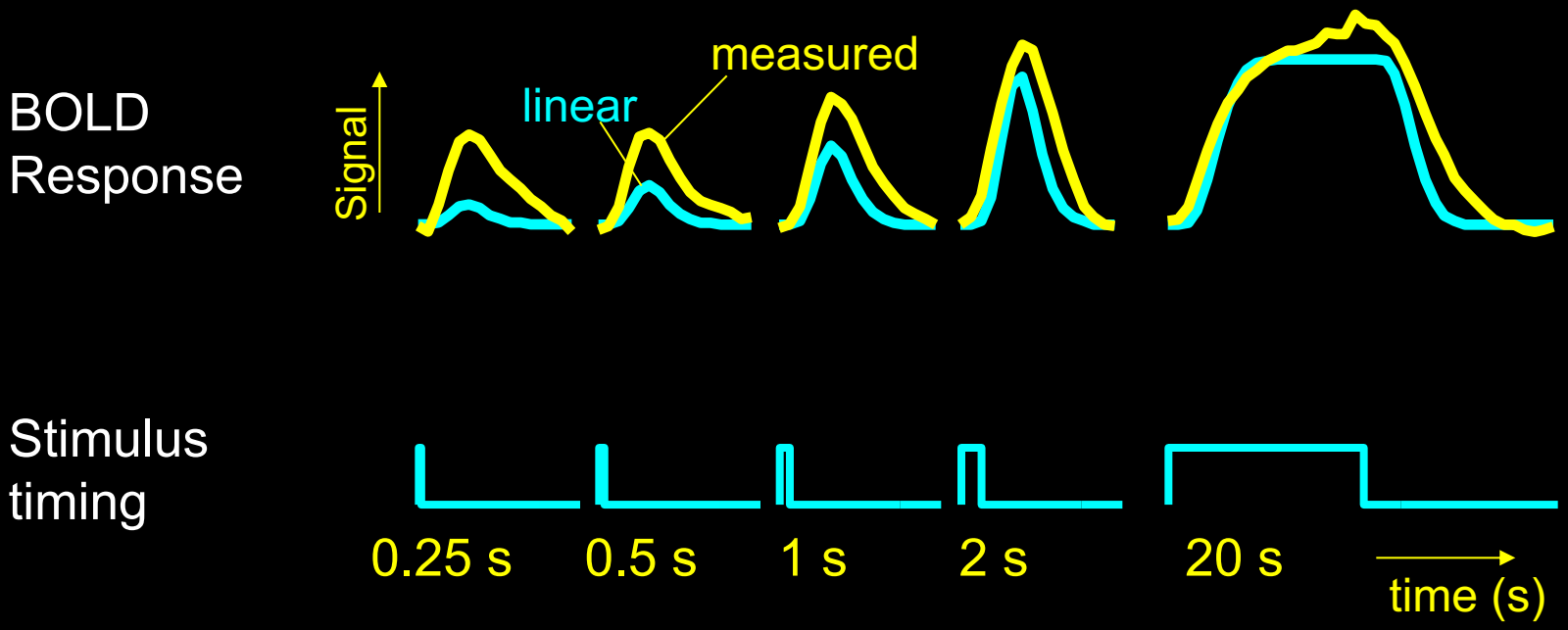


+ 2.5 s

0 s

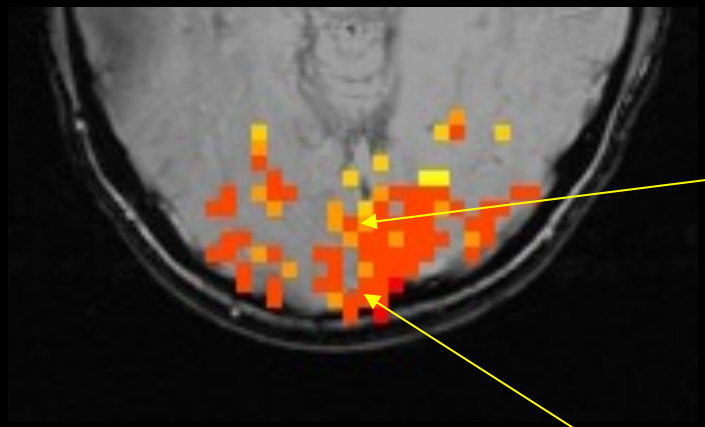
- 2.5 s

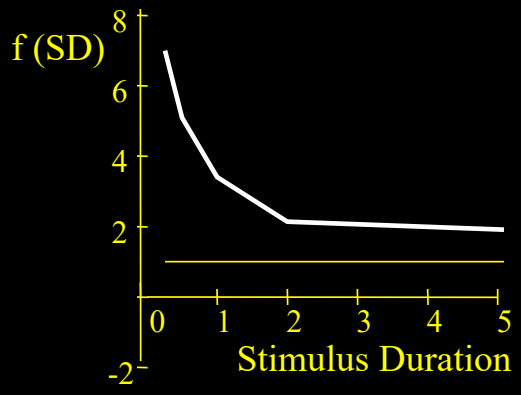
Different stimulus “ON” periods

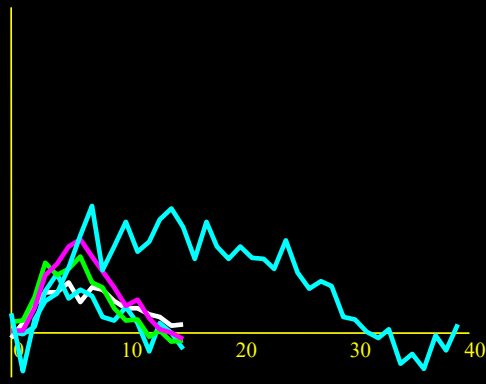


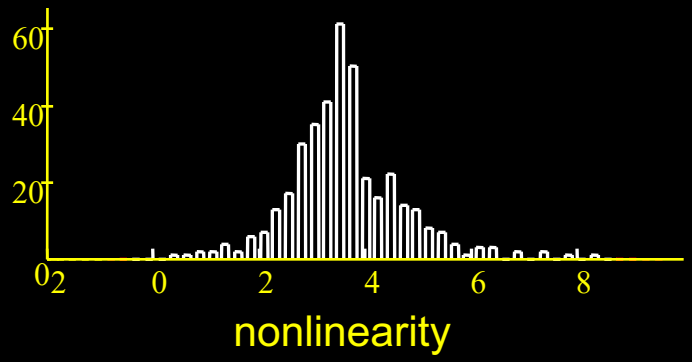
Brief stimuli produce larger responses than expected

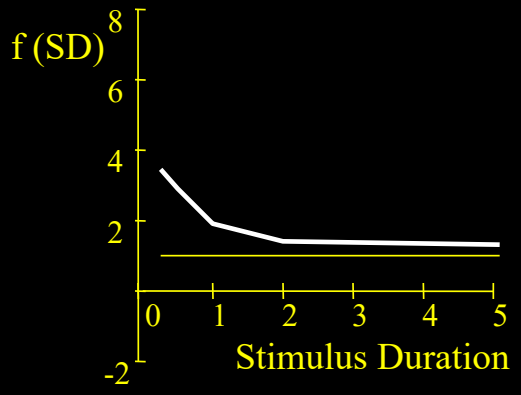
Results – visual task

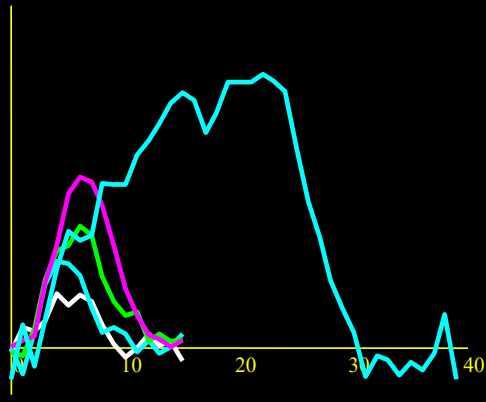










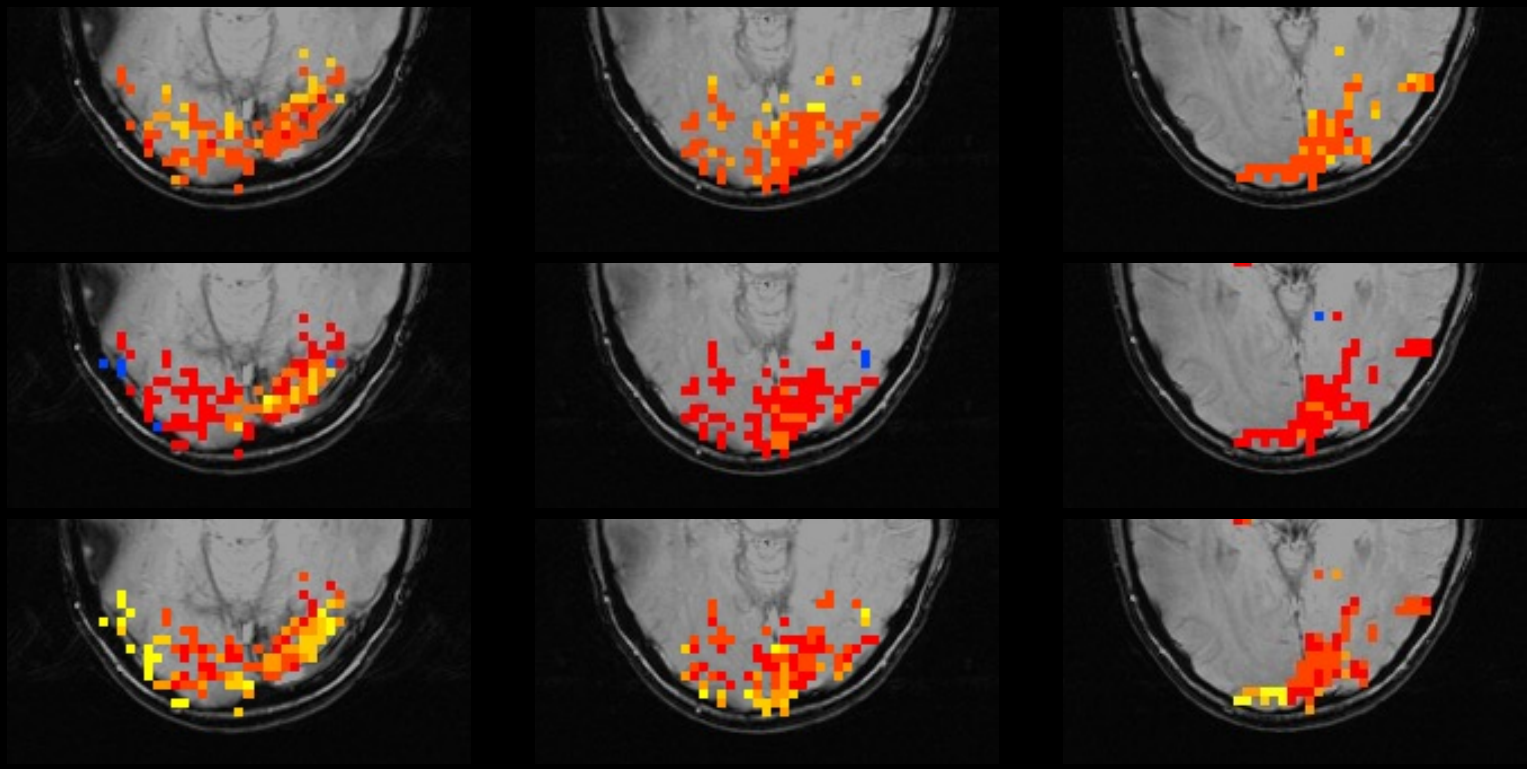


Results – visual task

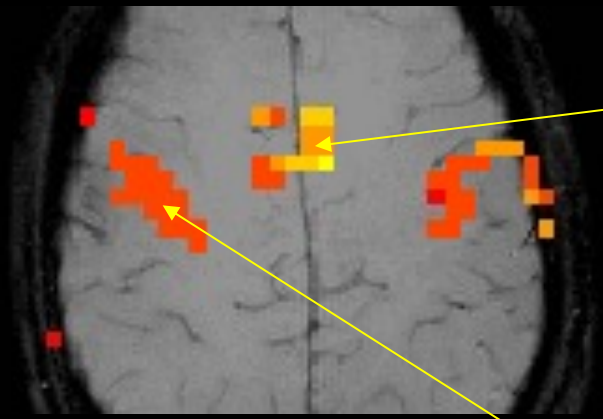
Nonlinearity

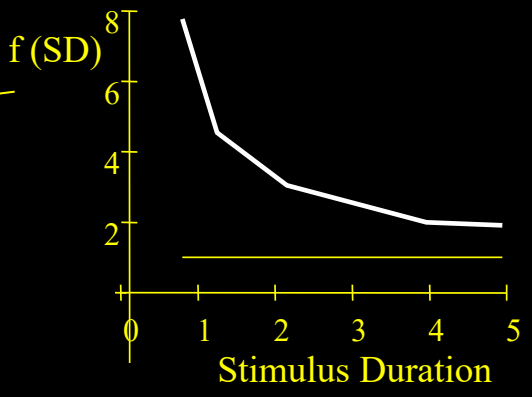
Magnitude

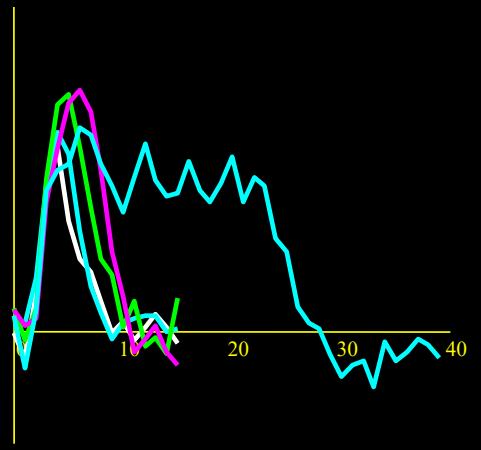
Latency

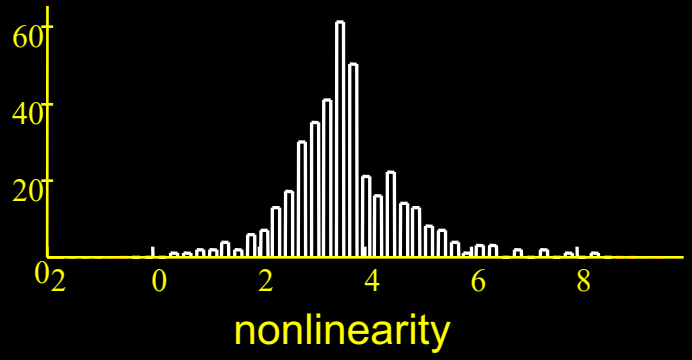


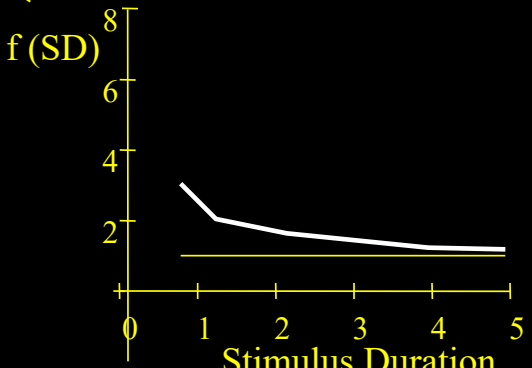
Results – motor task

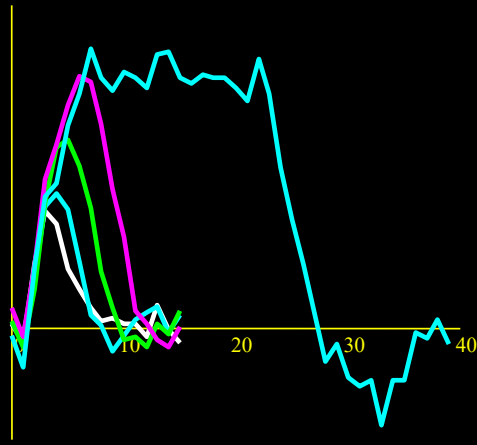










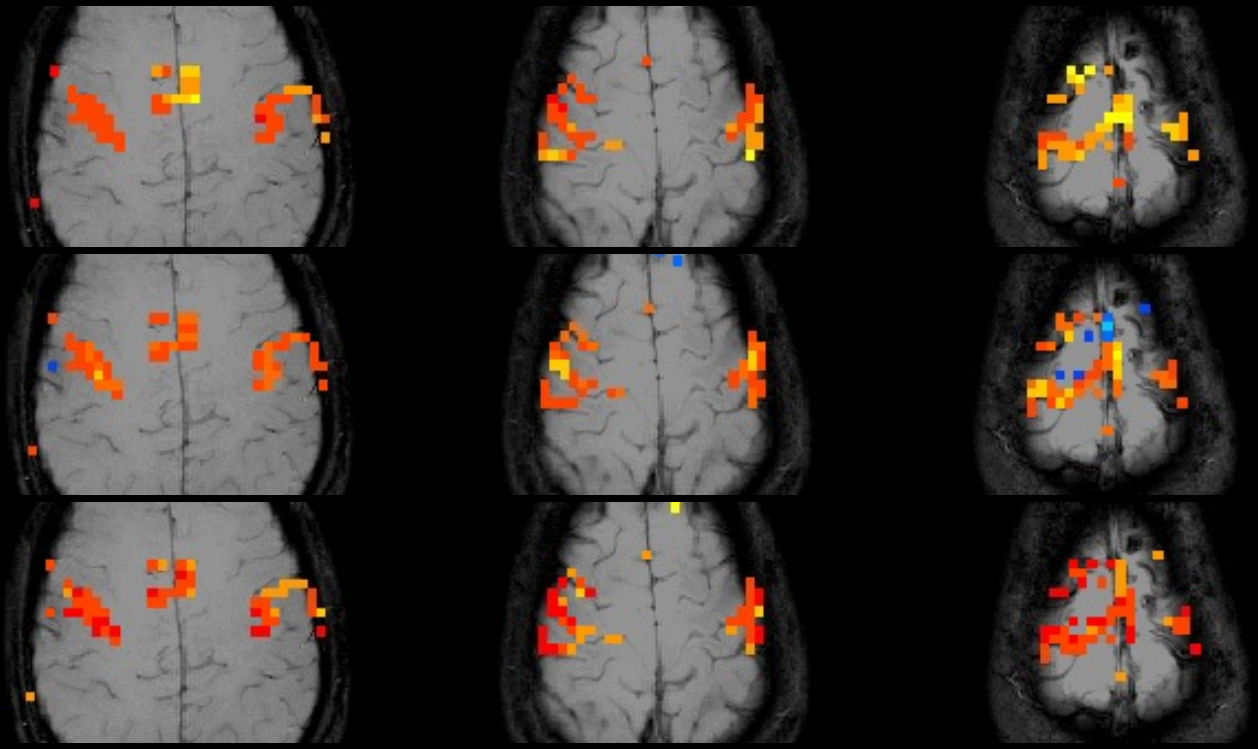


Results – motor task

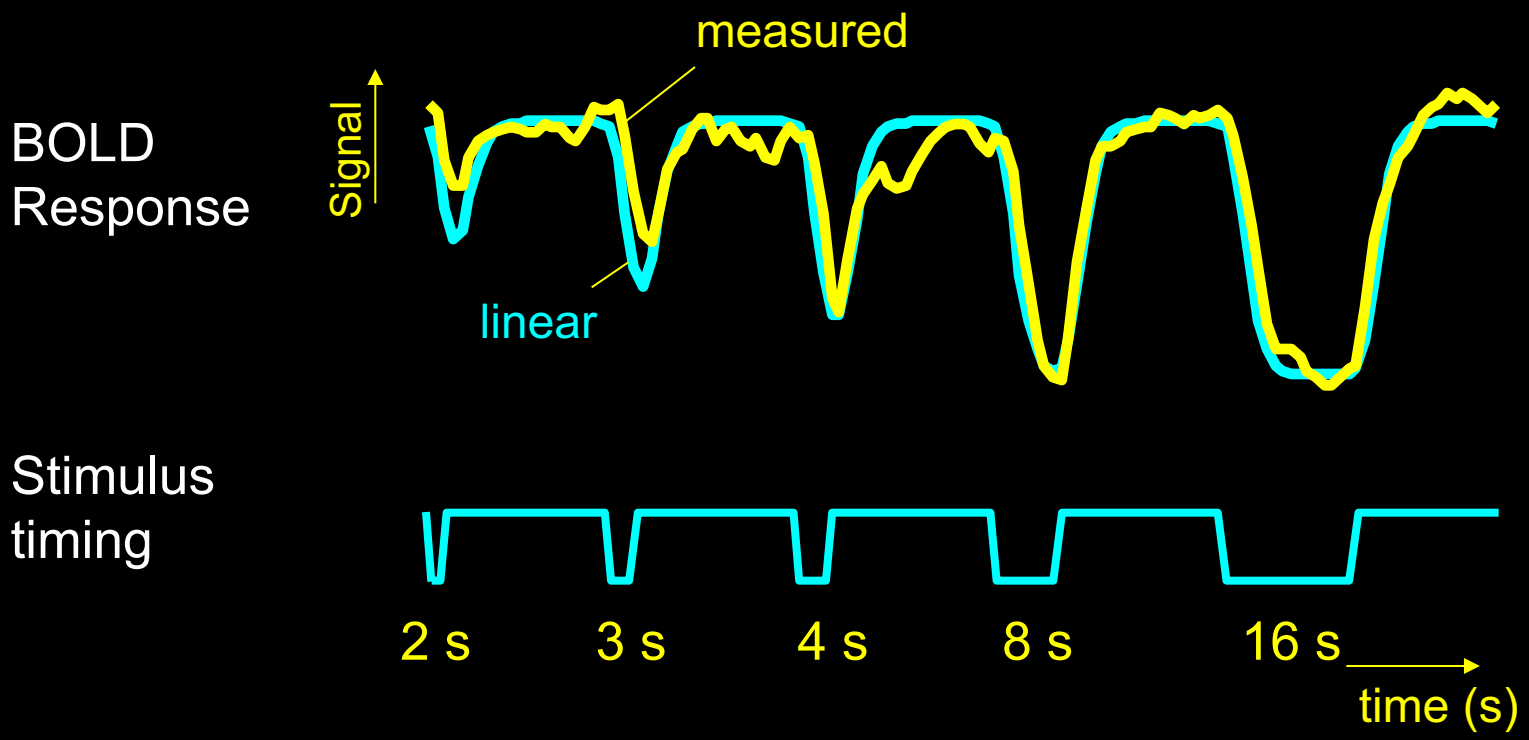
Nonlinearity

Magnitude

Latency



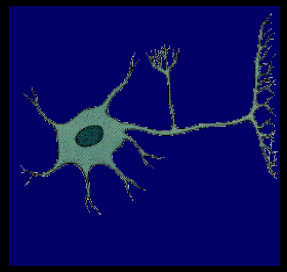
Different stimulus “ON” periods

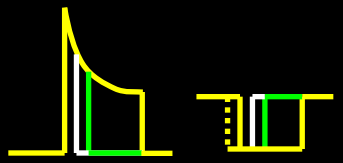


Brief stimulus OFF periods produce smaller decreases than expecte

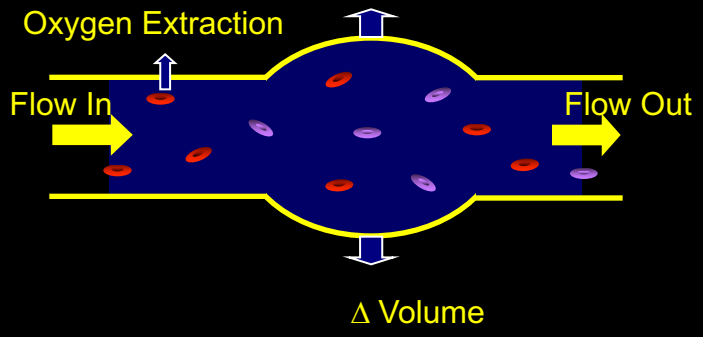
Sources of this Nonlinearity

- Neuronal

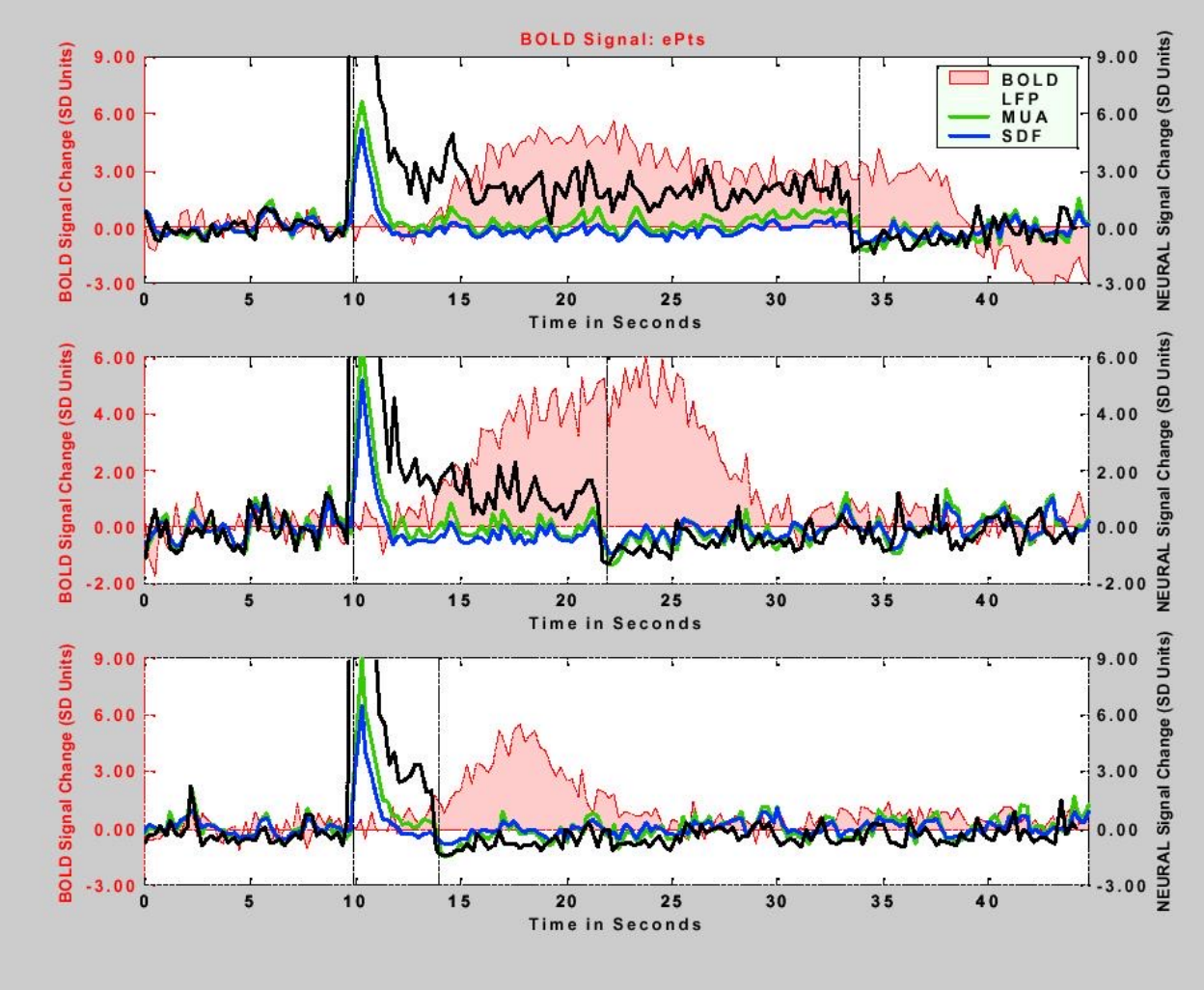




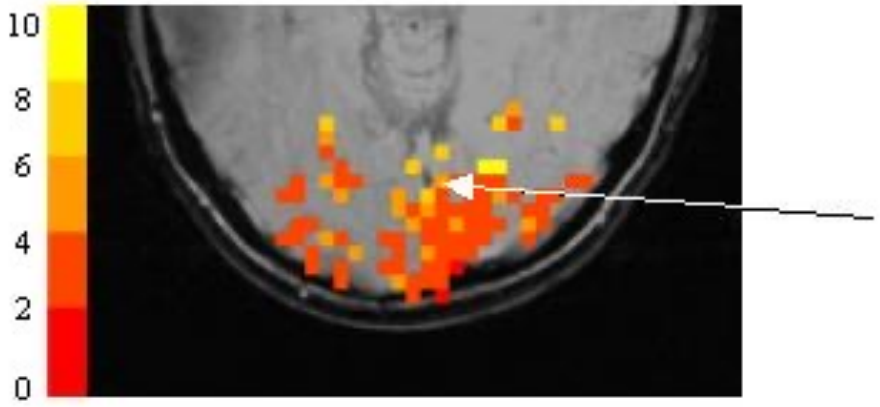
- Hemodynamic
  - Oxygen extraction
  - Blood volume dynamics

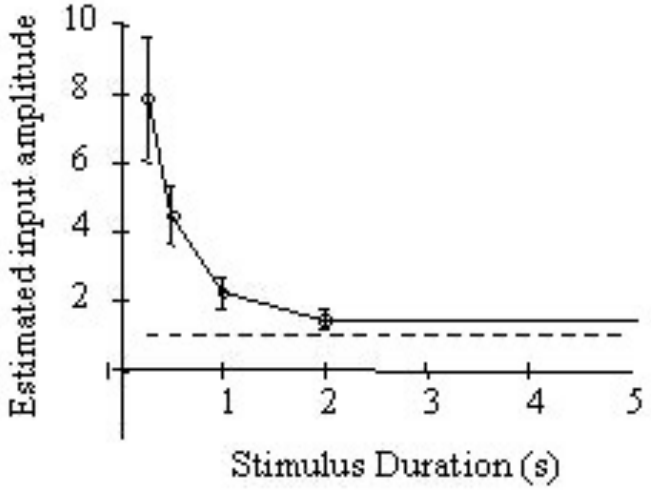


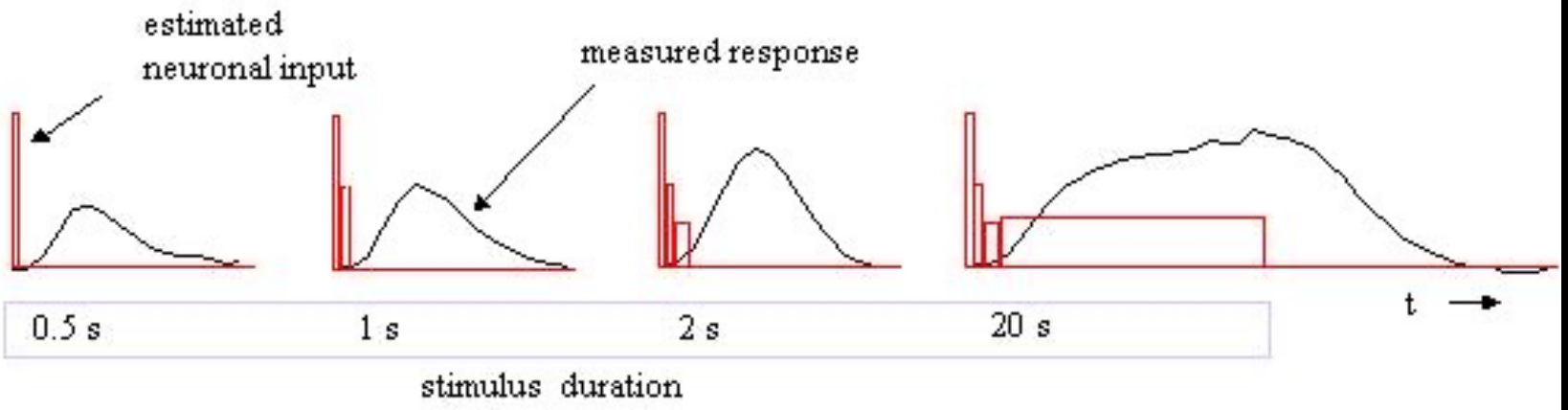
BOLD Correlation with Neuronal Activity

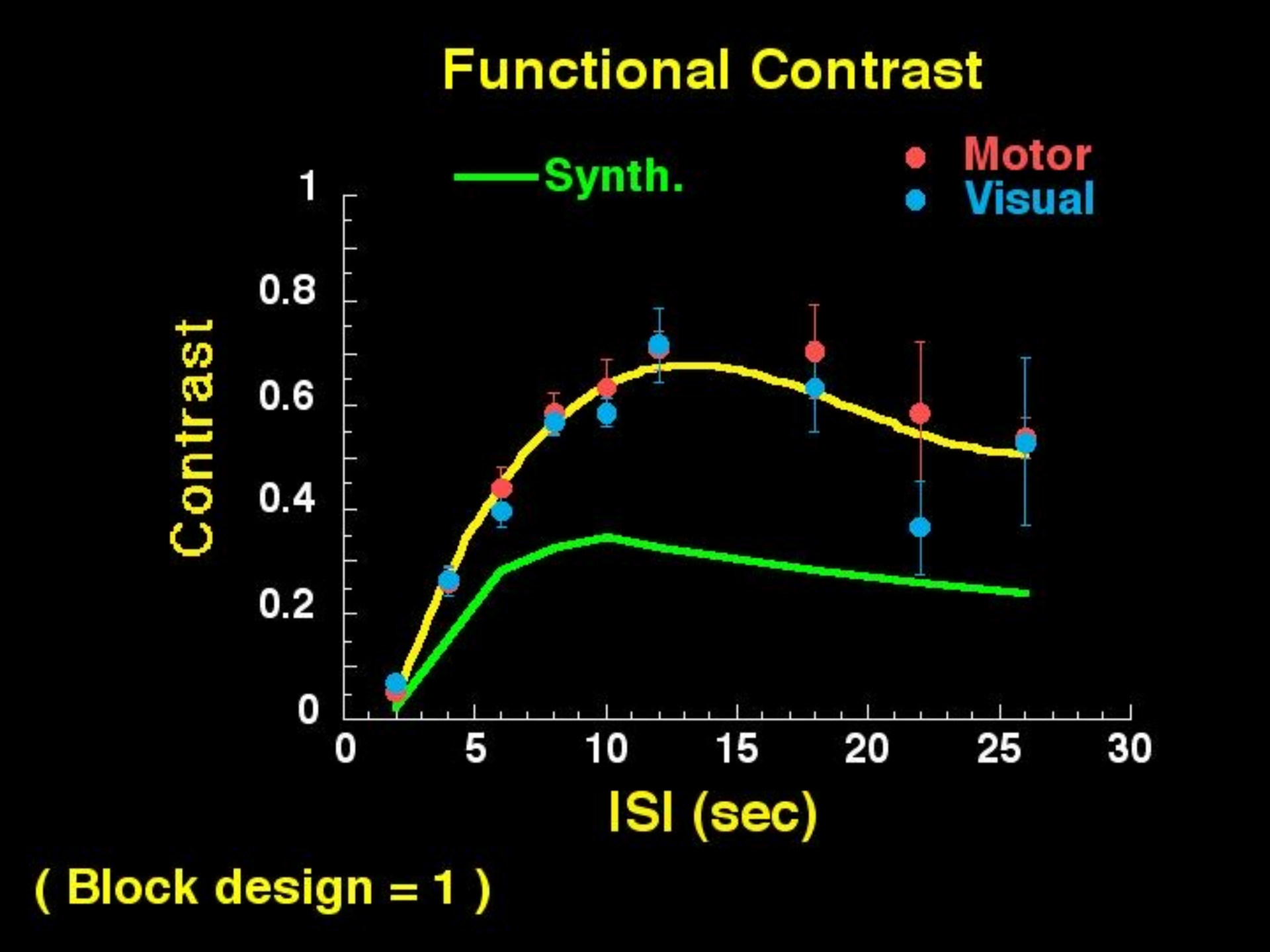


Logothetis et al. Nature, 412, 150-157

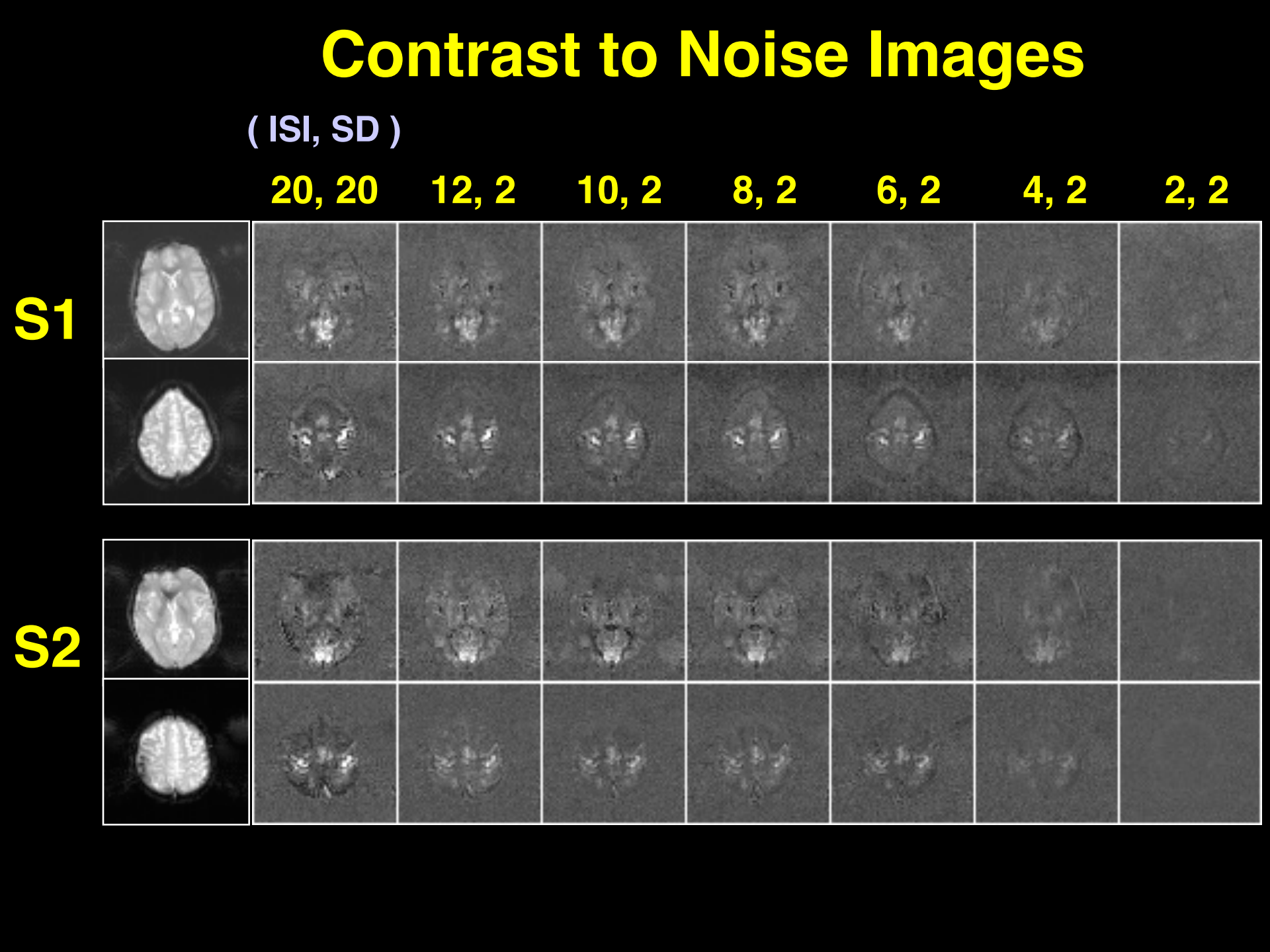

10
8
6
4
2
0


Estimated input amplitude
10
8
6
4
2
1
1
2
3
4
5
Stimulus Duration (s)


estimated
neuronal input
measured response
t
0.5 s
1 s
2 s
20 s
stimulus duration


Functional Contrast
Synth.
Motor
Visual
Contrast
1
0.8
0.6
0.4
0.2
0
0
5
10
15
20
25
30
ISI (sec)
(Block design = 1)

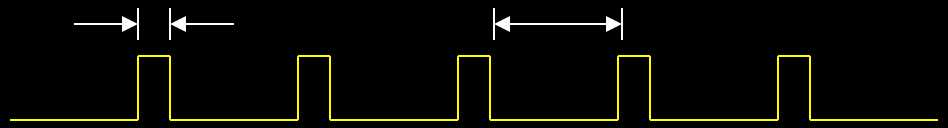
Contrast to Noise Images

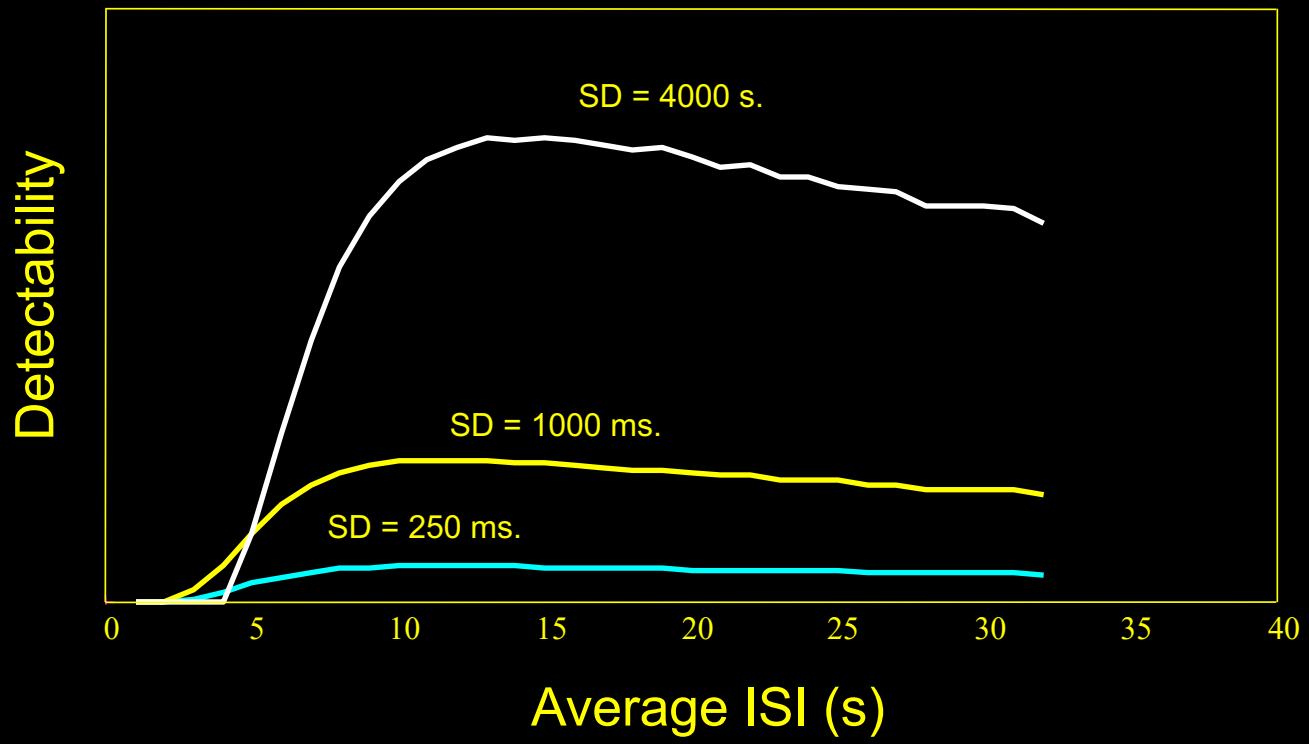


Detectability – constant ISI

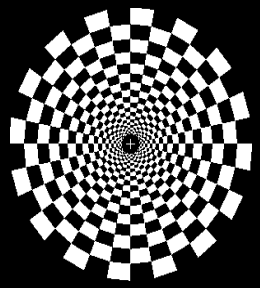
SD – stimulus duration

ISI – inter-stimulus interval

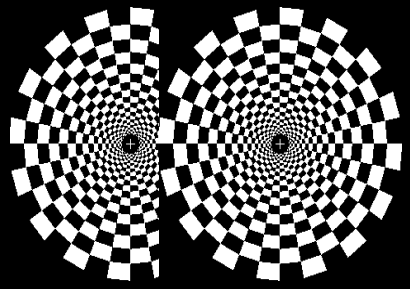




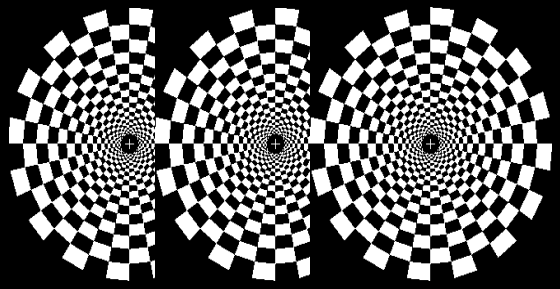
Visual Activation Paradigm: 1 , 2, & 3 Trials



0 sec 20 sec



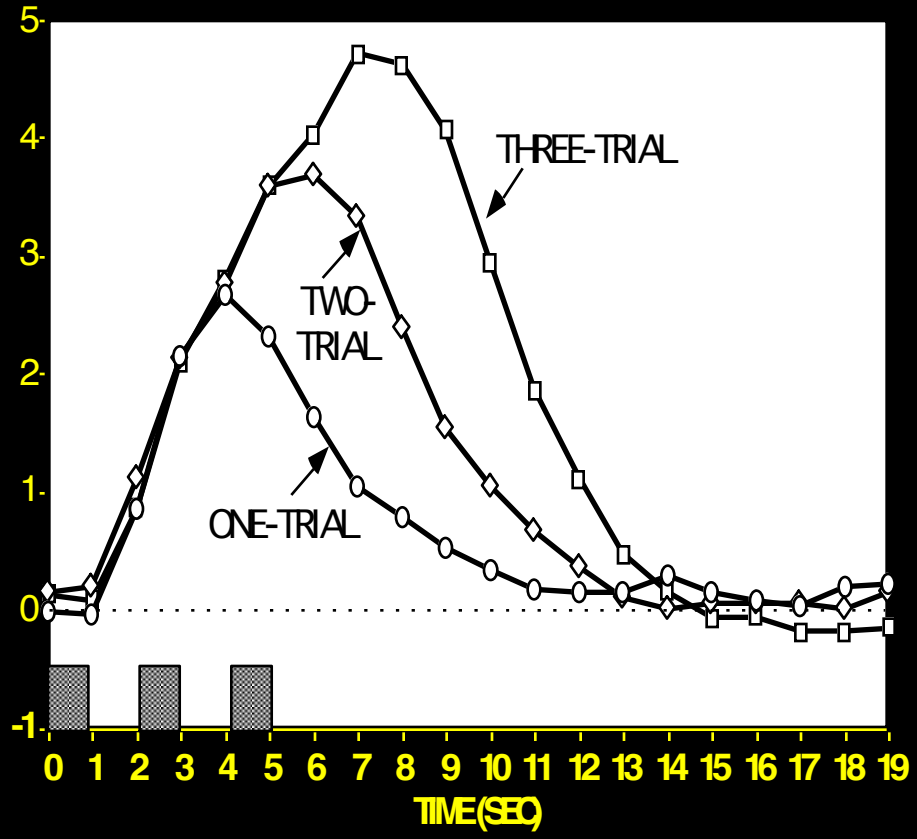
0 sec2 sec 20 sec



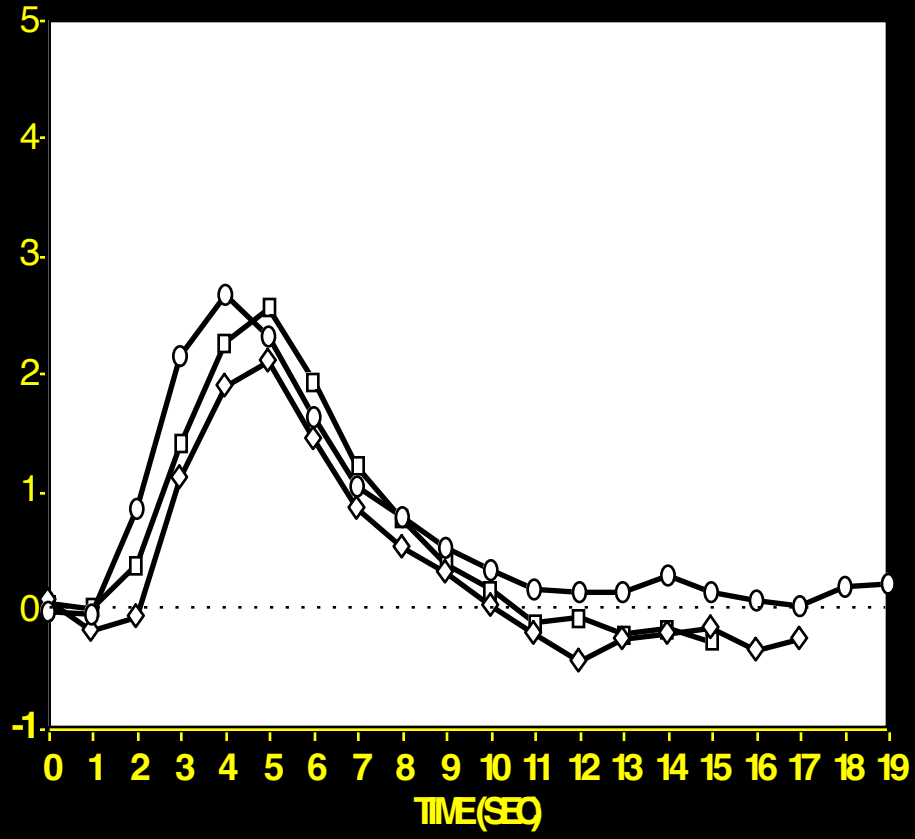
0 sec2 sec4 sec 20 sec

Response to Multiple Trials: Subject RW

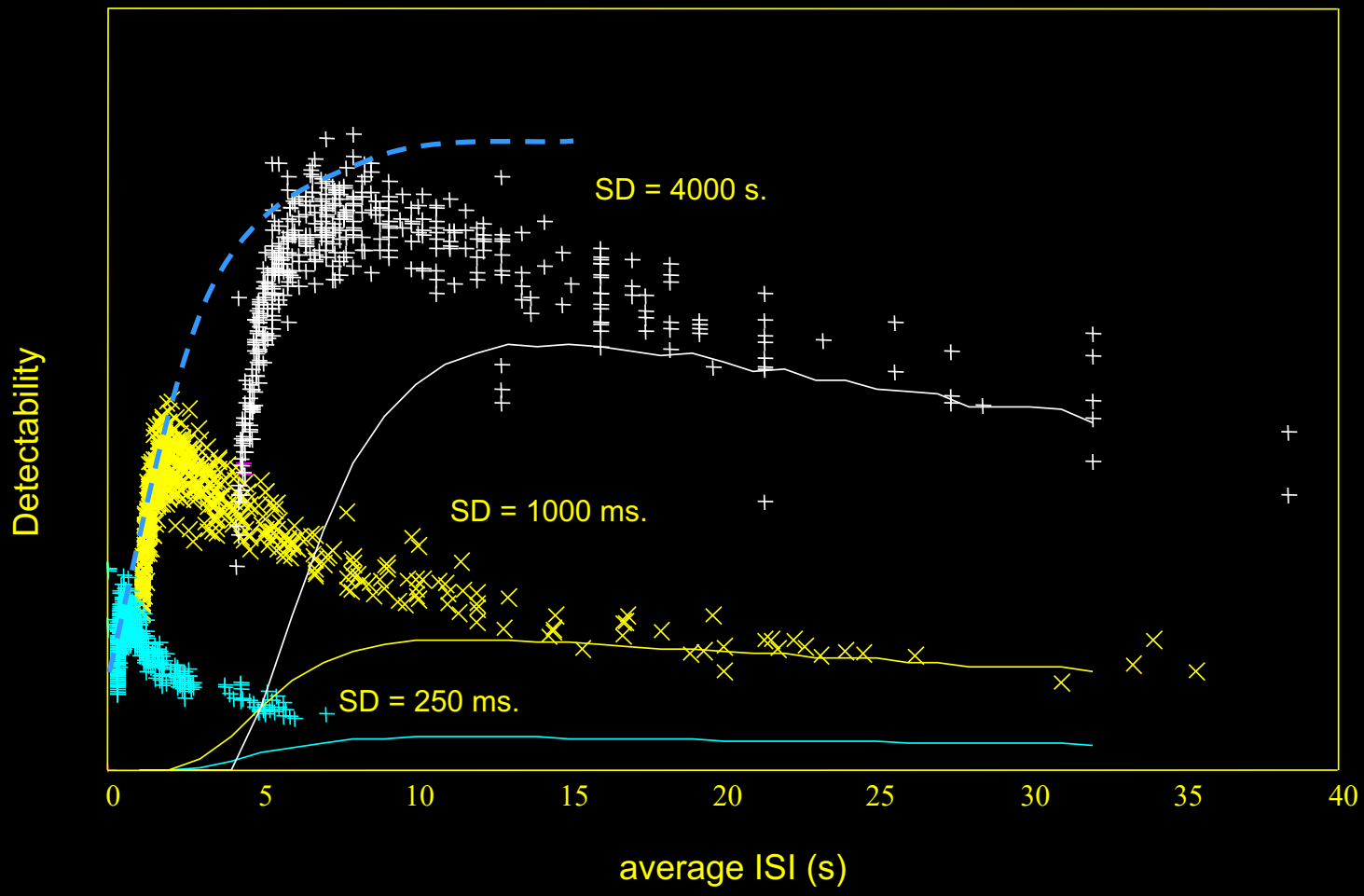
RAW DATA



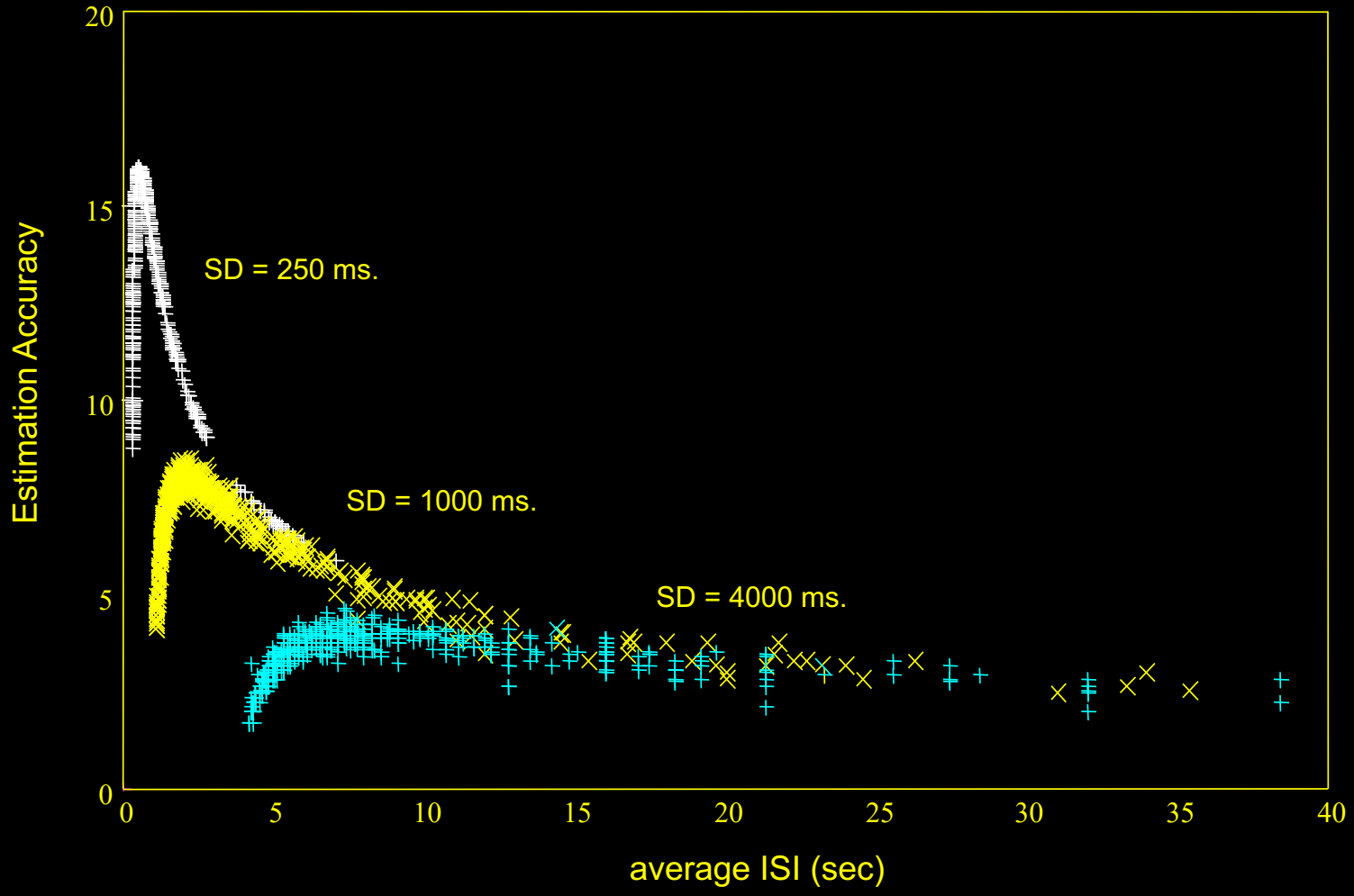
ESTIMATED RESPONSES



Detectability vs. Average ISI



Estimation accuracy vs. average ISI



Motion

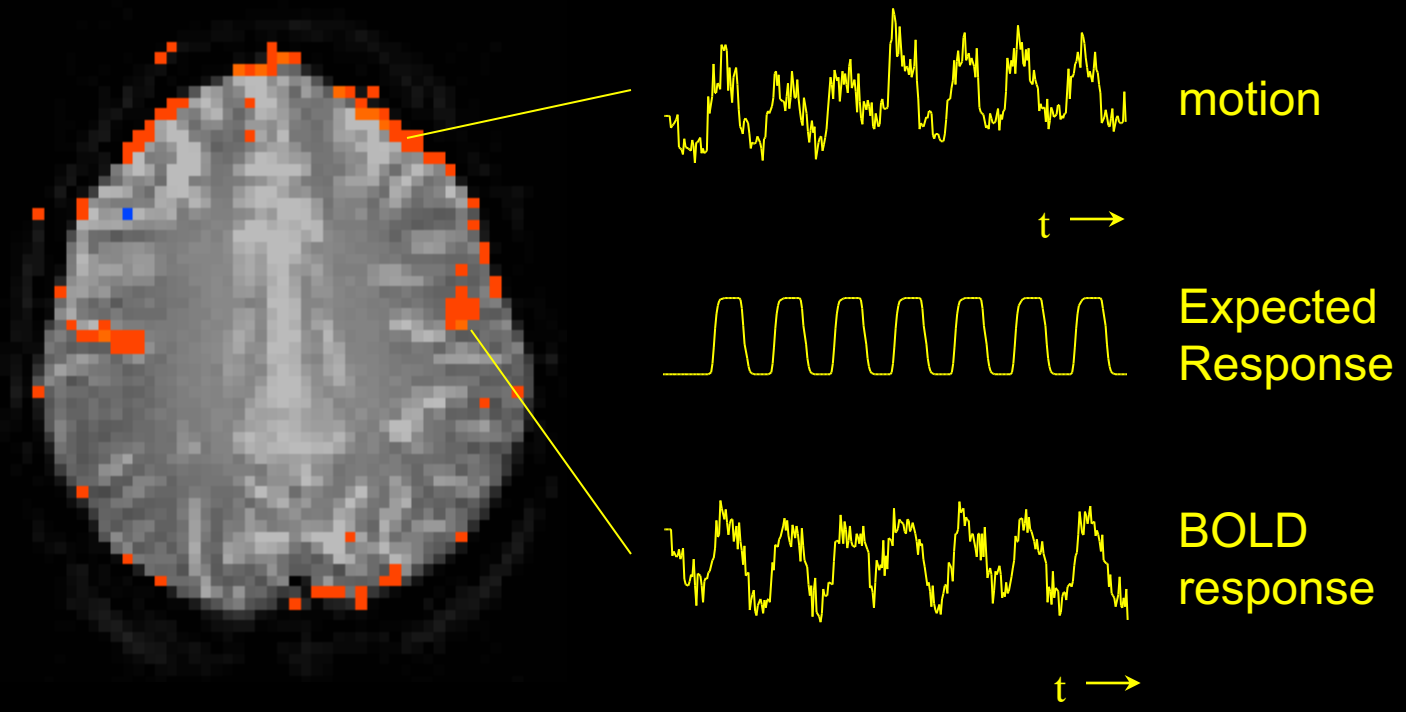
Recognize?
- Edge effects
- Shorter signal change latencies
- Unusually high signal changes
- External measuring devices

Correct?
- Image registration algorithms
- Orthogonalize to motion-related function *(cardiac, respiration, movement)*
- Navigator echo for k-space alignment *(for multishot techniques)*
- Re-do scan

Bypass?
- Paradigm timing strategies..
- Gating (with T1-correction)

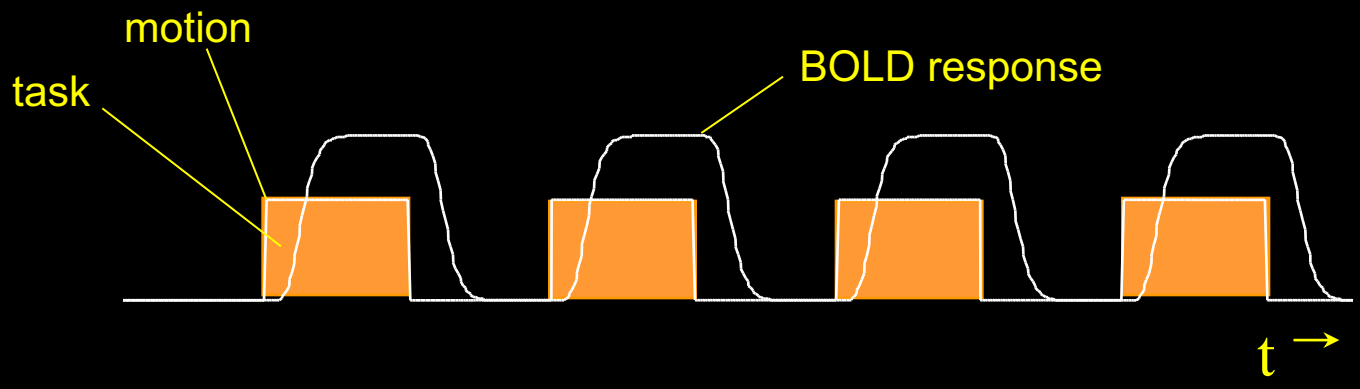
Suppress?
- Flatten image contrast
- Physical restraint
- Averaging, smoothing

Speaking - Blocked Trial

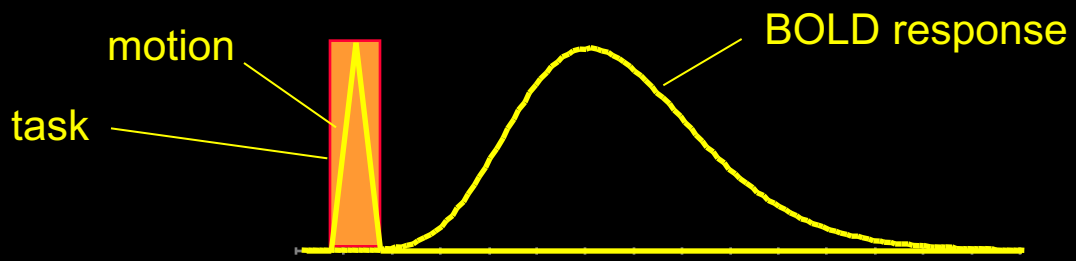


fMRI during tasks that involve brief motion

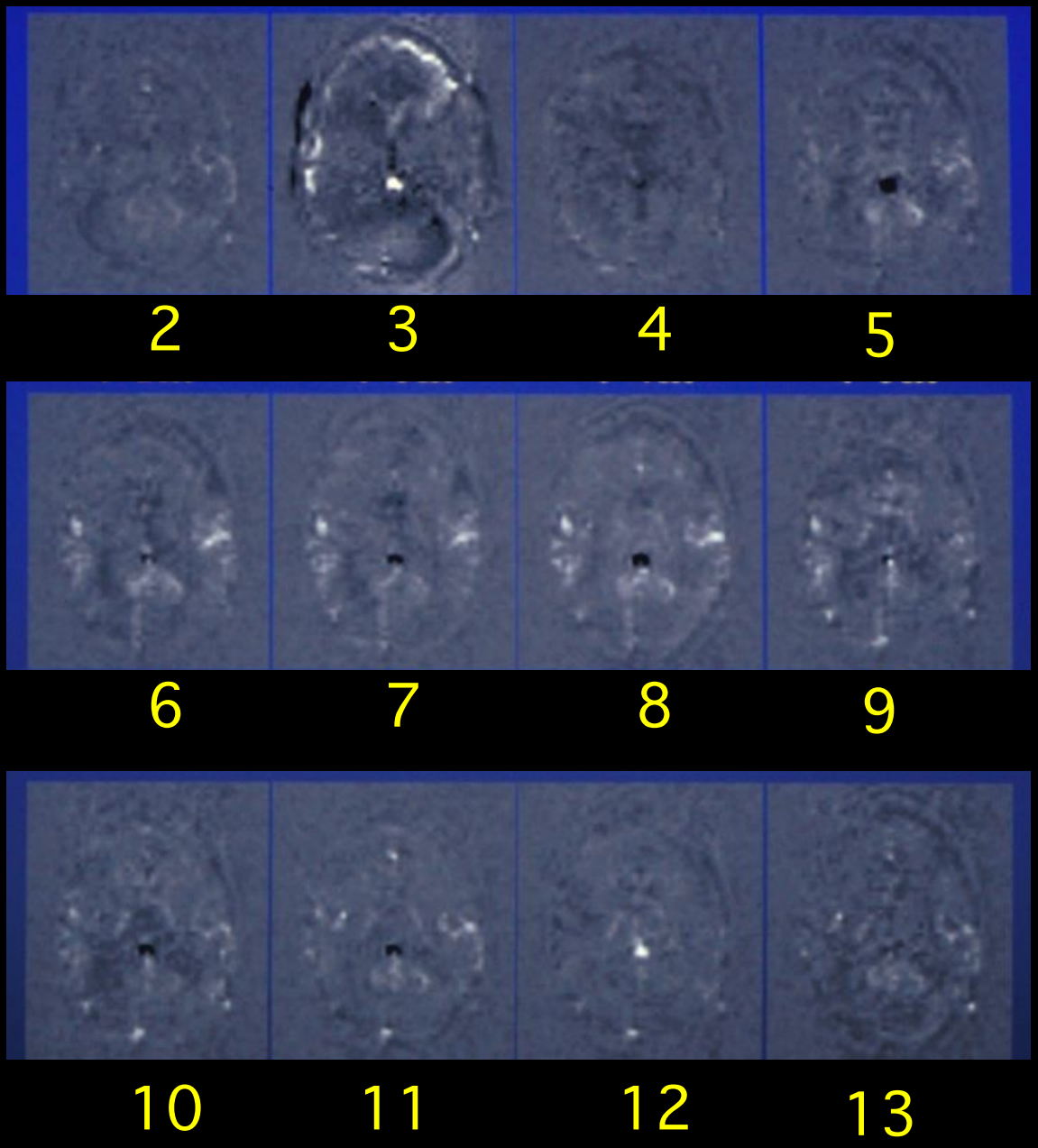
Blocked Design



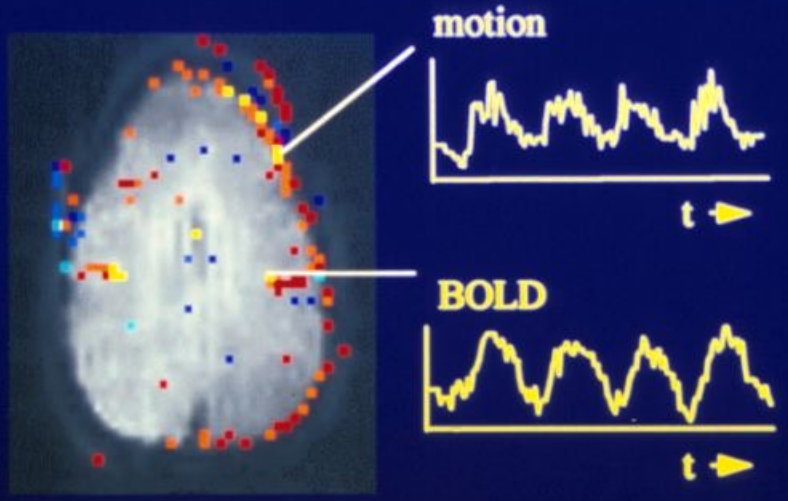
Event-Related Design

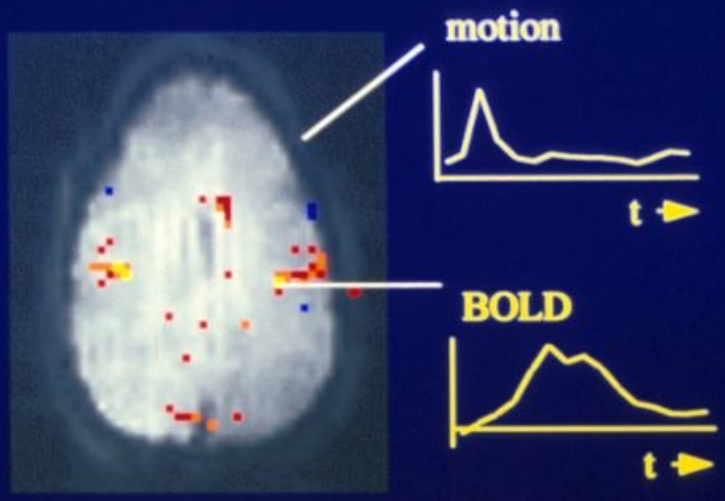


Overt Word Production



Motion-Decoupled fMRI:
Functional MRI during of overt word production





"block-trial" paradigm

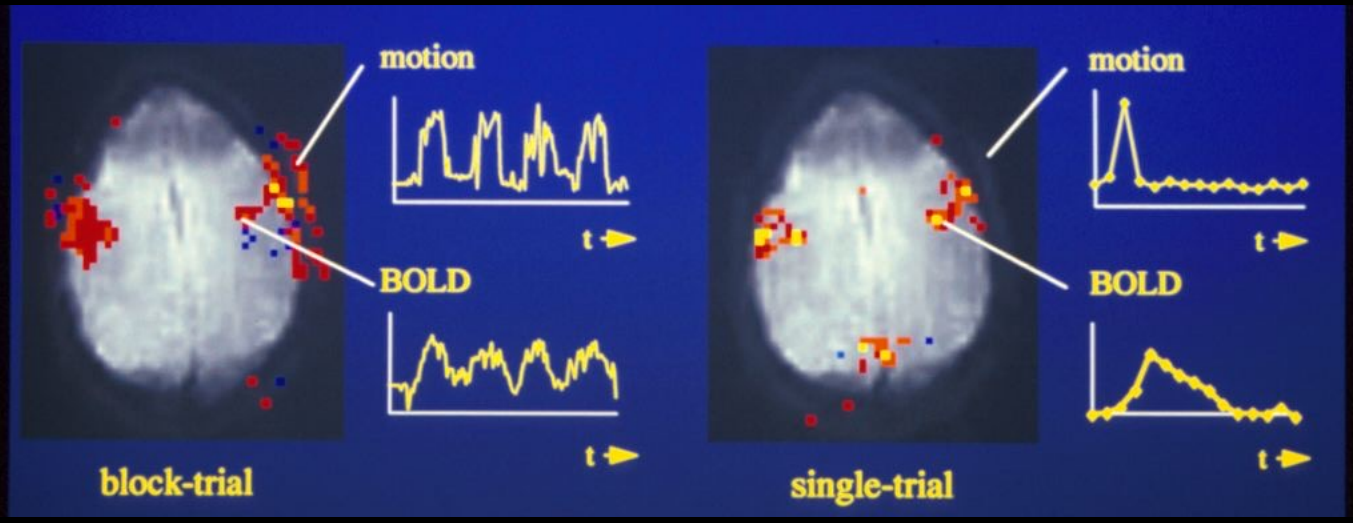
Motion induced signal changes resemble functional (BOLD) signal changes

"single-trial" paradigm

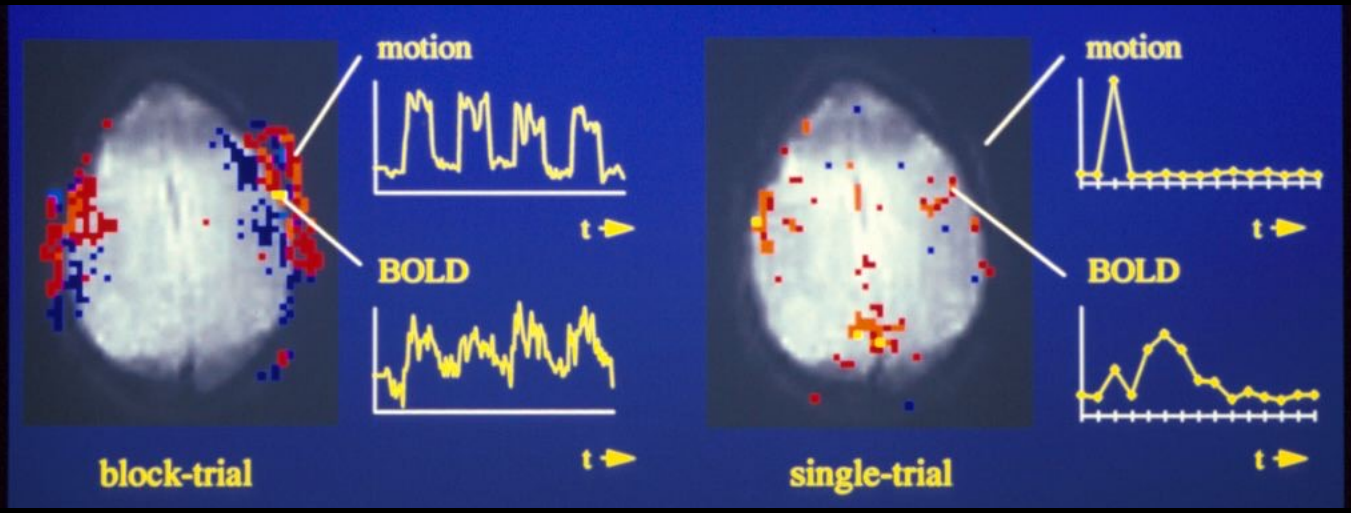
Motion induced and BOLD signal changes are separated in time

R.M. Birn, et al.

Tongue Movement

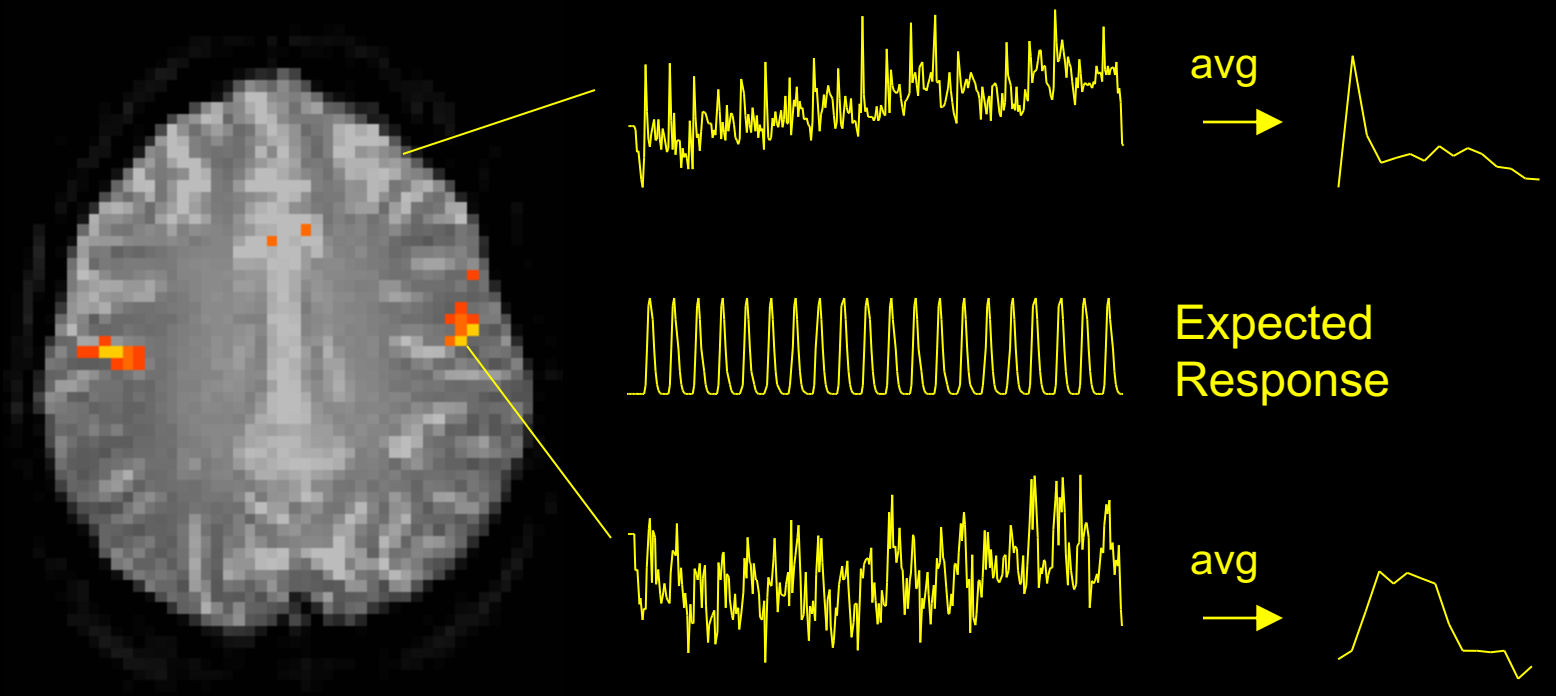


Jaw Clenching

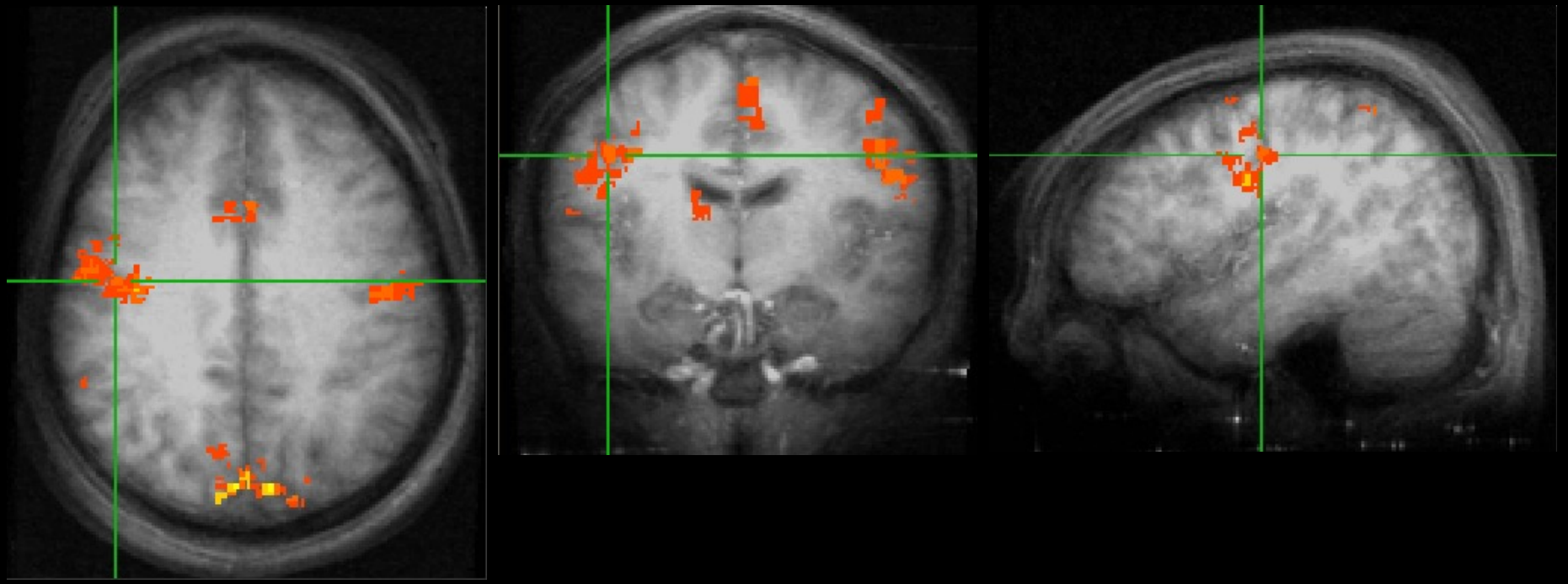


Constant ISI

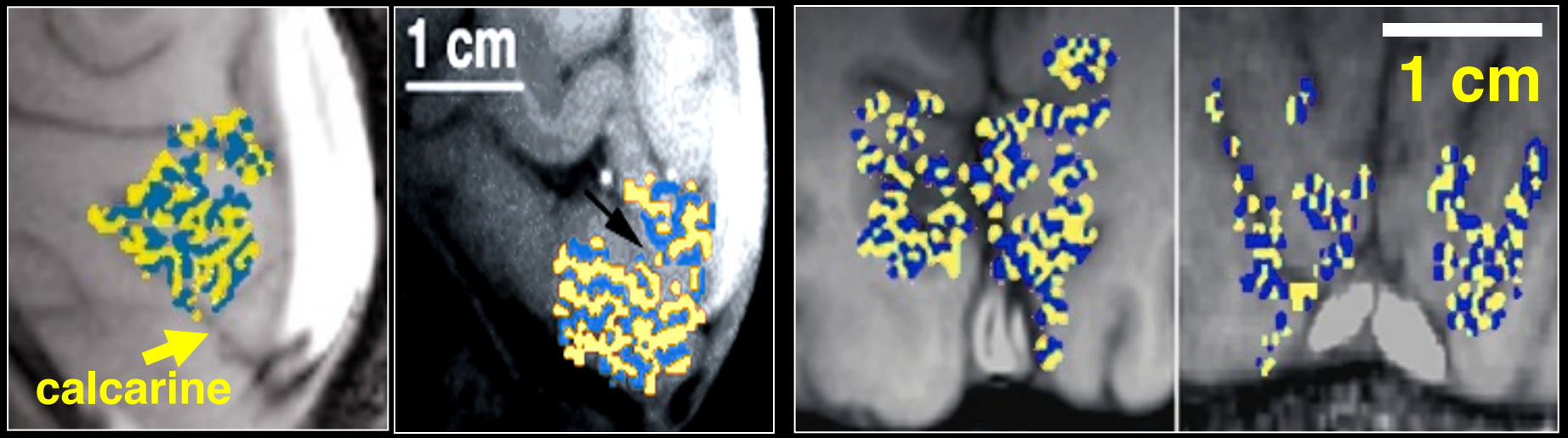
Speaking - ER-fMRI



Swallowing - Event-Related



ODC Maps using fMRI

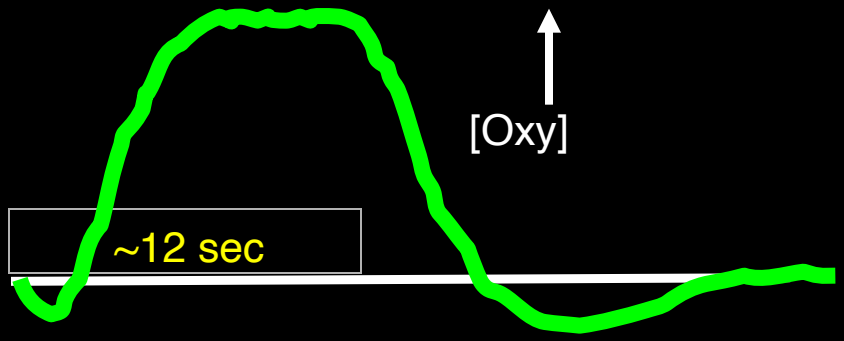


- Identical in size, orientation, and appearance to those obtained by optical imaging[1] and histology[3,4].

[1]Malonek D, Grinvald A. *Science* 272, 551-4 (1996).
[3]Horton JC, Hocking DR. *J Neurosci* 16, 7228-39 (1996).
[4]Horton JC, et al. *Arch Ophthalmol* 108, 1025-31 (1990).

Why short is better than long

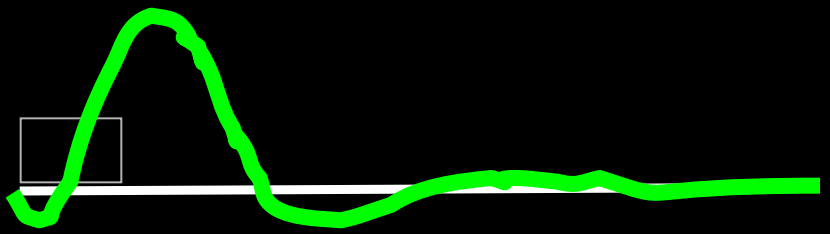
The vascular response to prolonged neural stimulation



It is argued that fMRI cannot achieve submillimeter functional resolution because a saturated hyperoxic vascular response to neural activity spreads over many millimeters[1,2].

However, optical imaging has demonstrated that the hyperoxic response can yield well-localized maps when using short duration stimuli (<5 sec)[1].

The vascular response to brief neural stimulation

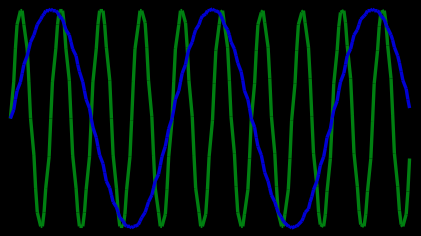


[1]Malonek D, Grinvald A. Science 272, 551-4 (1996).
[2]Kim D-S, Duong T, Kim S-G. Nat Neurosci 3, 164-9 (2000).

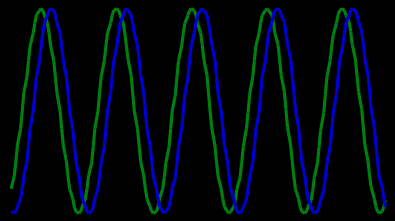
Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

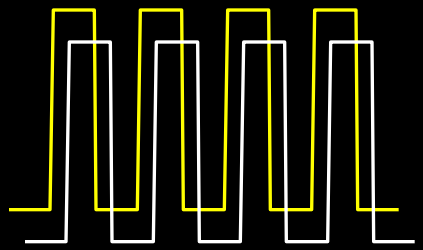


3. Phase Encoding



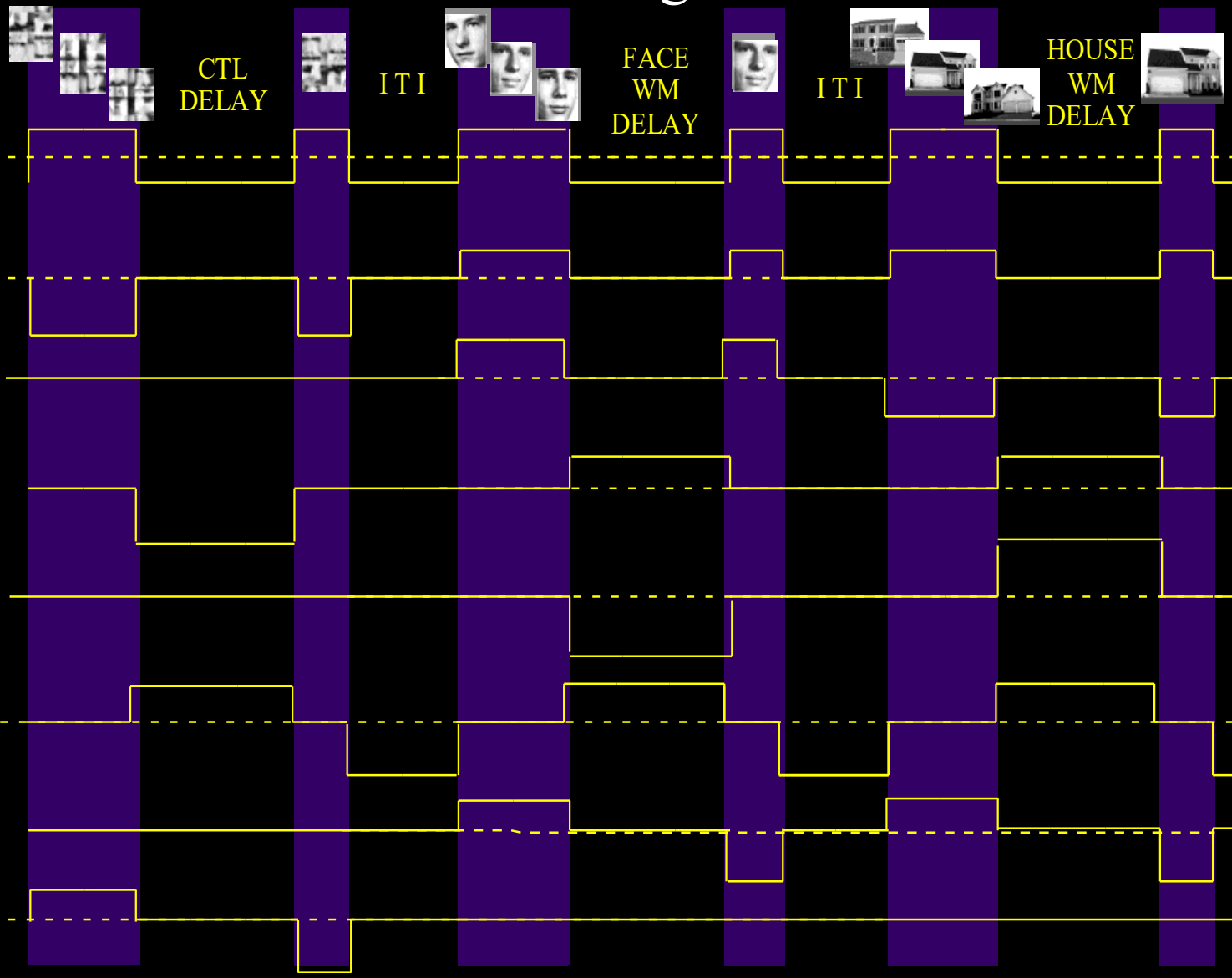
4. Single Event

5. Orthogonal Block Design



6. Free Behavior Design.

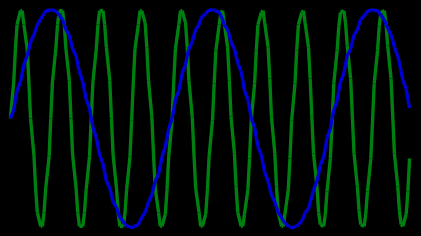
Example of a Set of Orthogonal Contrasts for Multiple Regression



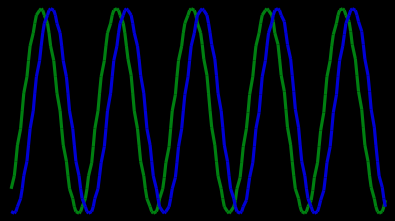
Neuronal Activation Input Strategies

1. Block Design

2. Frequency Encoding

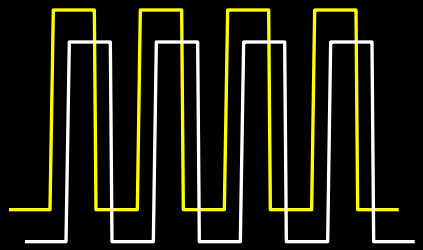


3. Phase Encoding



4. Single Event

5. Orthogonal Block Design



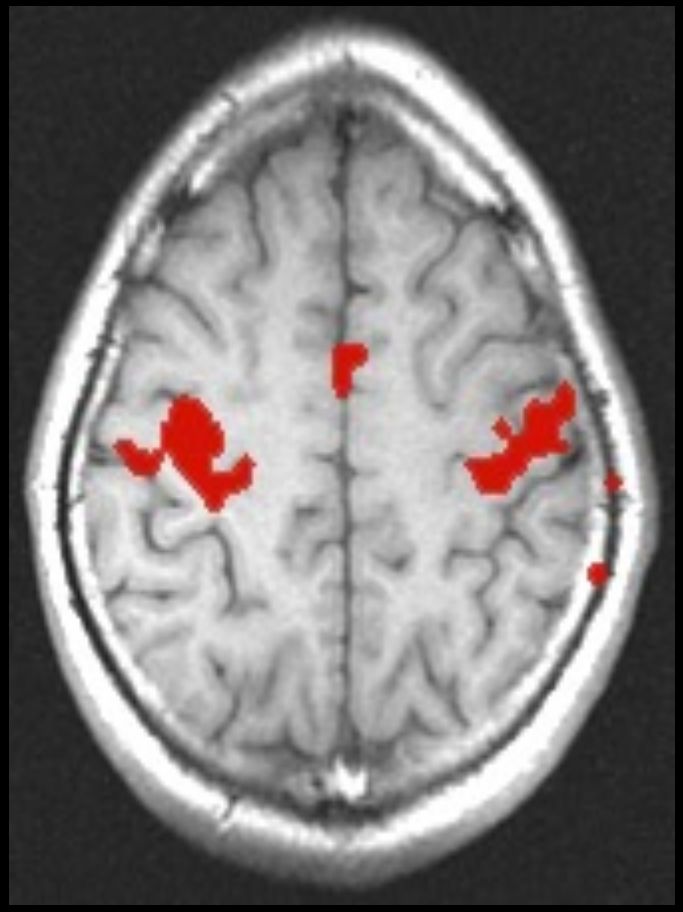
6. Free Behavior Design.

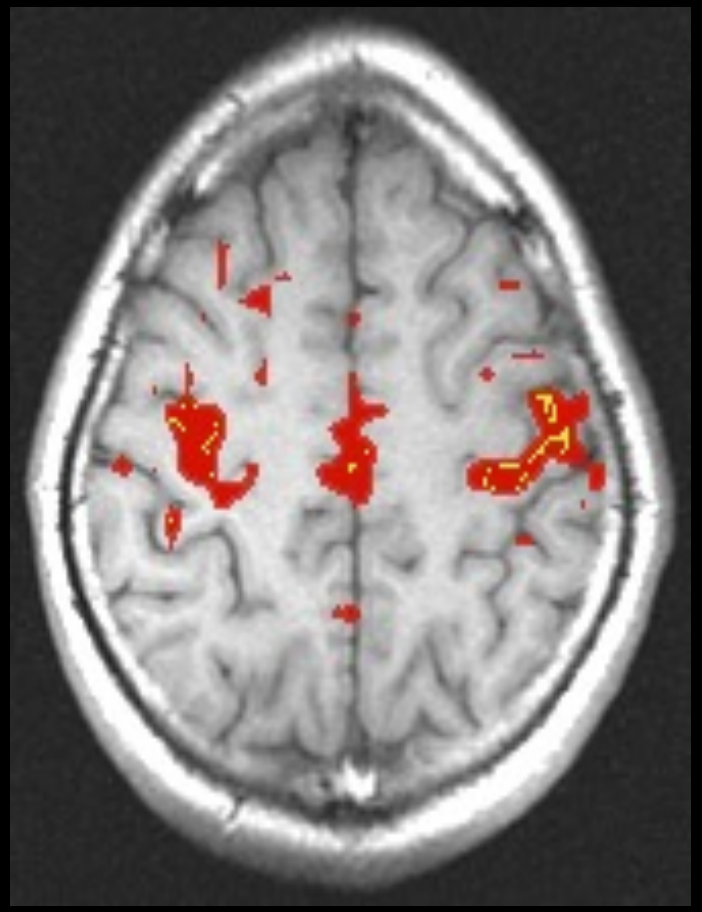
Free Behavior Design

Use a continuous measure as a reference function:

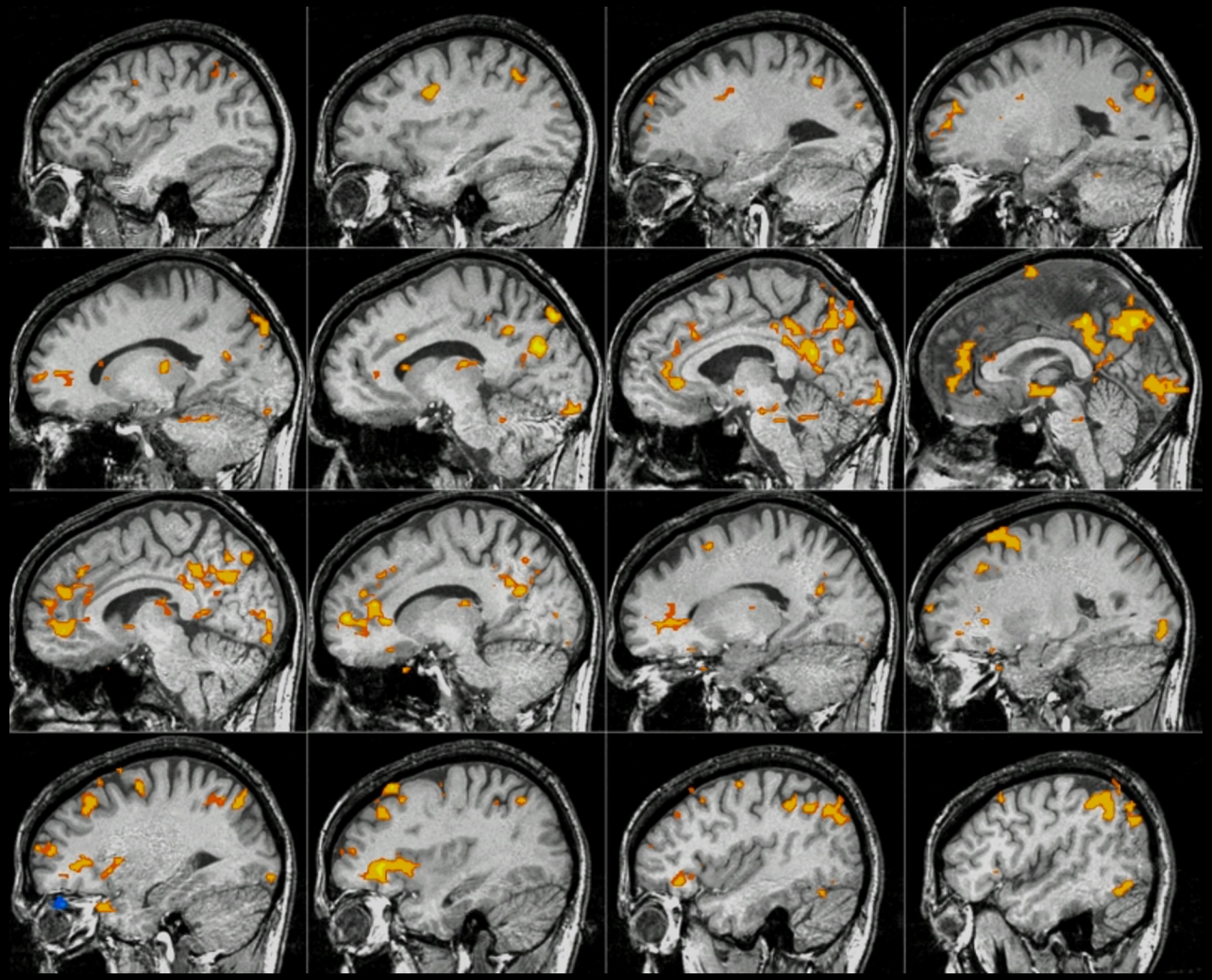
- Task performance
- Skin Conductance
- Heart, respiration rate..
- Eye position
- EEG

Resting Hemodynamic Autocorrelations

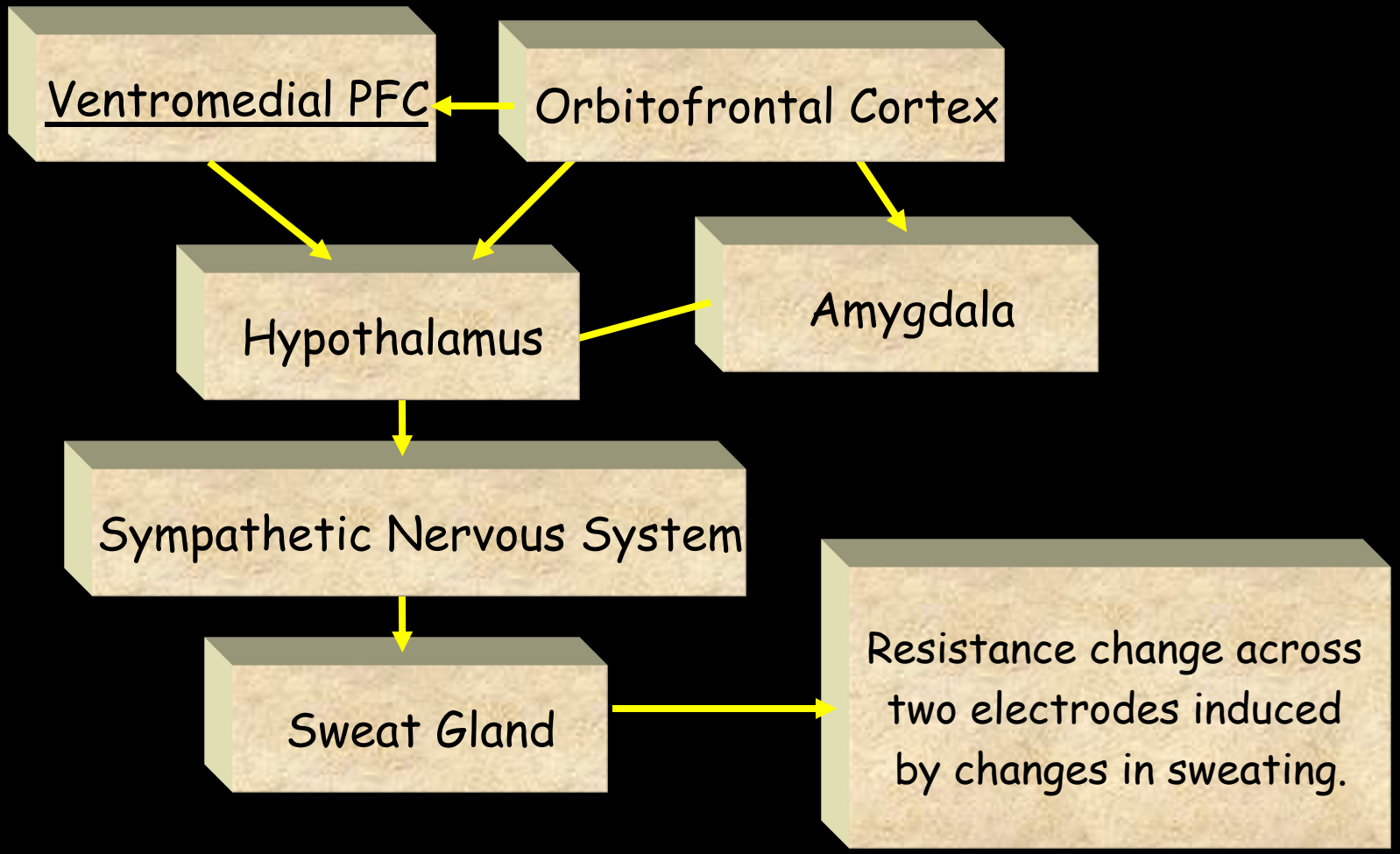




Brain activity correlated with SCR during “Rest”



The Skin Conductance Response (SCR)



Skin Conductance Dynamics

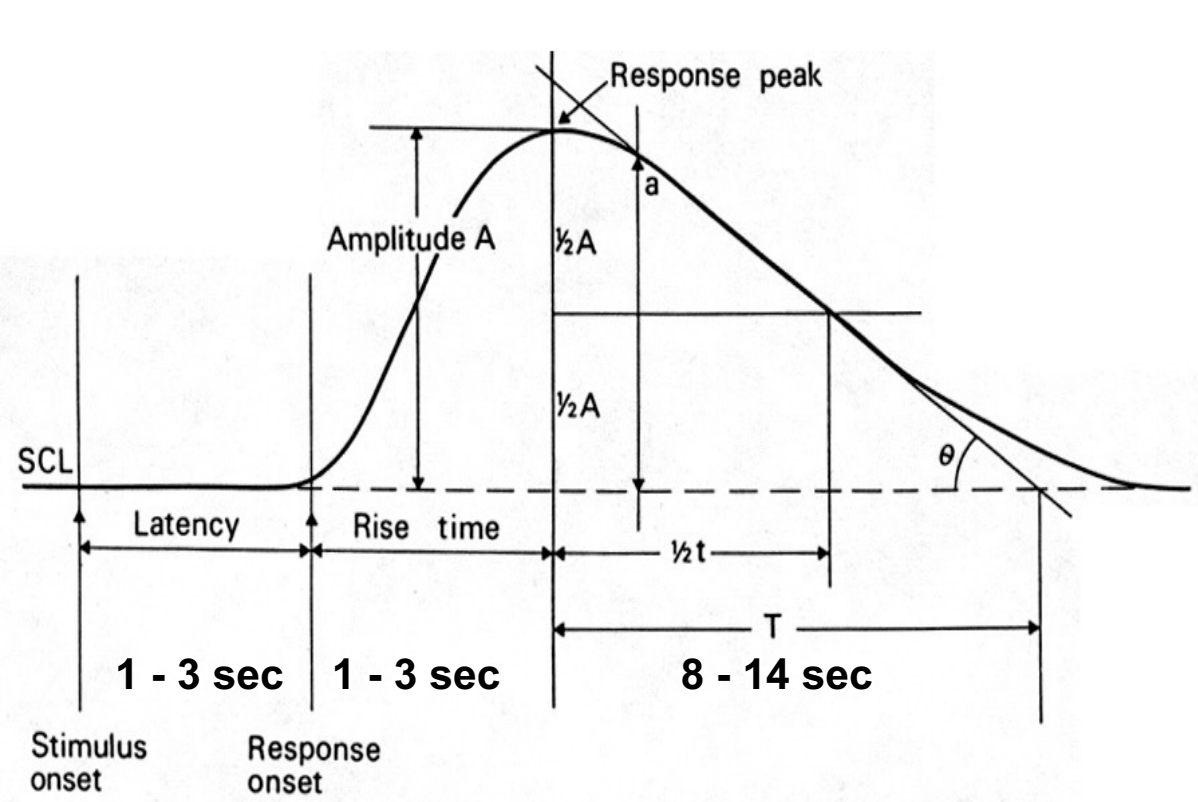


FIGURE 1. Diagrammatic skin conductance response.

•Boucsein, Wolfram (1992). Electrodermal Activity. Plenum Press, NY

•Venables, Peter, (1991). Autonomic Activity ANYAS 620:191-207.

Functional Imaging Methods / 3T Group

Staff Scientists:

Sean Marrett

Jerzy Bodurka

Post Docs:

Rasmus Birn

Patrick Bellgowan

Ziad Saad

Graduate Student:

Natalia Petridou

Summer Student:

Dan Kelley

Program Assistant:

Kay Kuhns

August, 2000

Additional Thanks To...

Eric Wong, UCSD
Robert Savoy, MGH
Peter Jezzard, Oxford
Robert Cox, NIH
Richard Hoge, MGH
Randy Buckner, Wash. U.
Ted DeYoe, MCW
Sue Courtney, Johns Hopkins
Mark Cohen, UCLA